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**Dreyfuss et al.**

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(54) **SUTURE ANCHOR WITH INSERT-MOLDED RIGID MEMBER**

(75) Inventors: **Peter J. Dreyfuss**, Naples, FL (US);  
**William C. Benavitz**, Naples, FL (US)

(73) Assignee: **Arthrex, Inc.**, Naples, FL (US)

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CPC ..... **A61B 17/0401** (2013.01); **A61B 17/8645** (2013.01); **A61B 2017/0427** (2013.01); **A61B 2017/0414** (2013.01); **A61B 2017/044** (2013.01); **A61B 2017/0412** (2013.01)  
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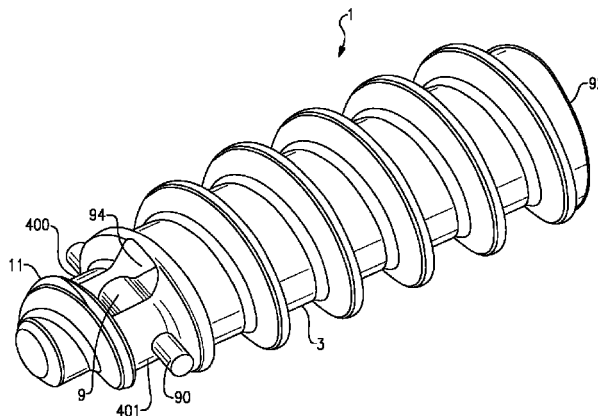
*Primary Examiner* — Dianne Dornbusch

(74) *Attorney, Agent, or Firm* — Carlson, Gaskey & Olds, P.C.

(57) **ABSTRACT**

A threaded suture anchor with an eyelet shield transversely molded at a distal end of the anchor body, over which one or more strands of suture is looped. The anchor body is threaded and has a tapered distal portion. The proximal end portion of the suture anchor body has a polygonally shaped opening to accept a polygonal drive head, preferably hexagonal or square. The peripheral surface defining polygonally shaped opening is rounded and smooth to prevent abrading sutures placed in contact therewith. In another embodiment, a push-in anchor is provided with an eyelet shield at the proximal end of the anchor.

**11 Claims, 8 Drawing Sheets**



S&N Exhibit 1001  
Smith & Nephew v. Arthrex

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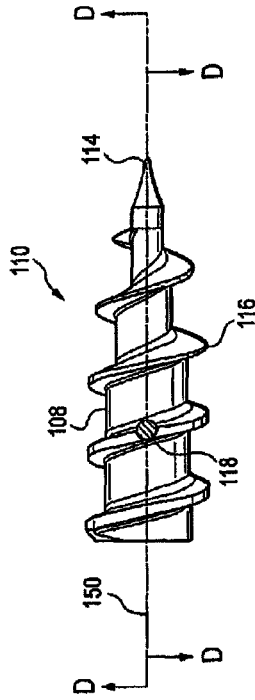


FIG. 1

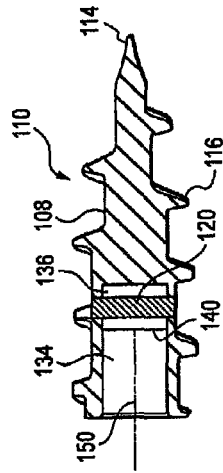


FIG. 2

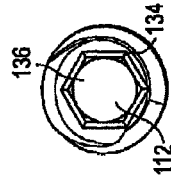


FIG. 3

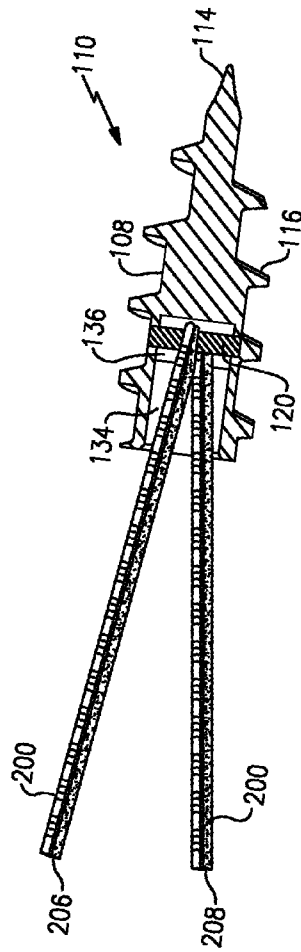
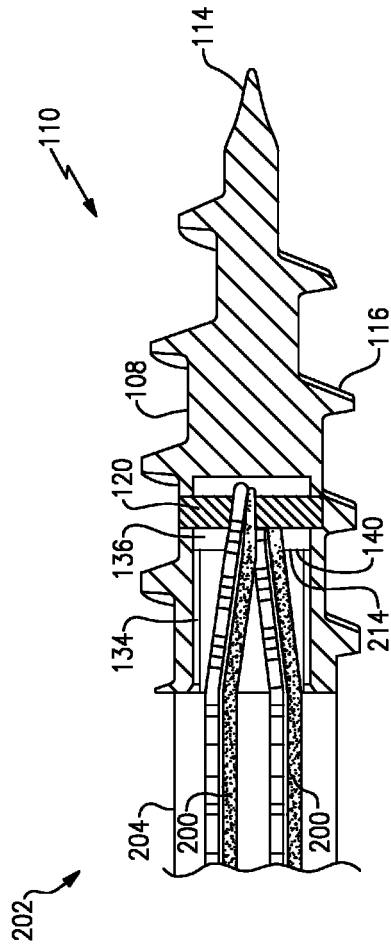
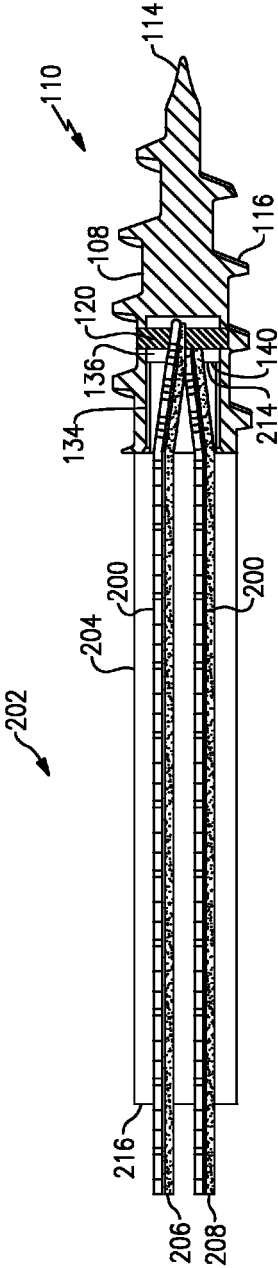


FIG. 4g

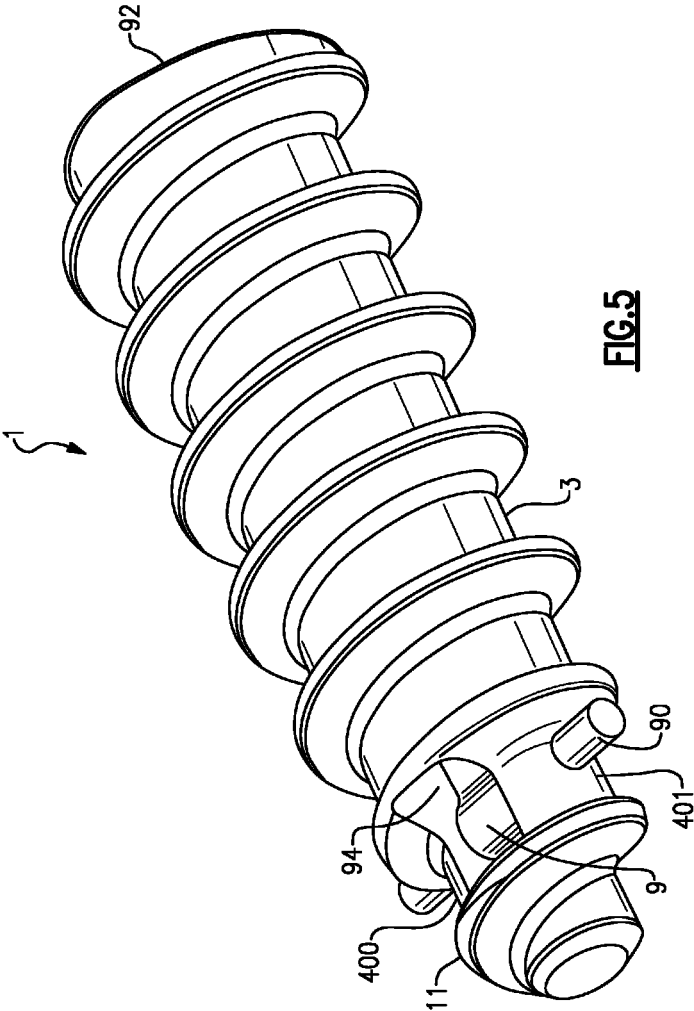


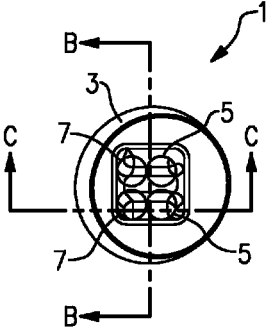
**FIG. 4b**



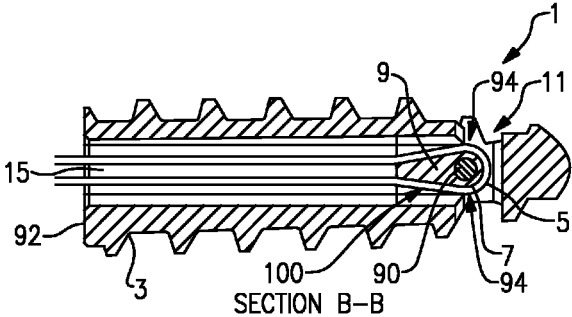
**FIG. 4c**



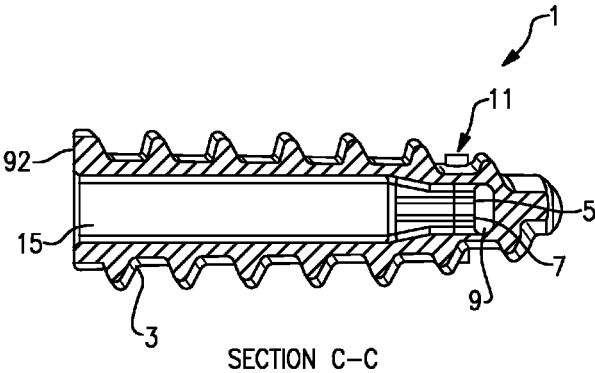




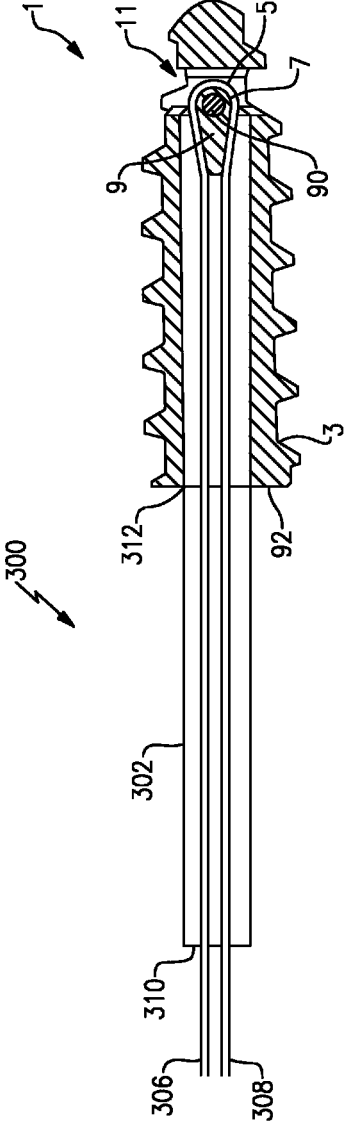
**FIG. 6**



**FIG. 7a**



**FIG. 8**



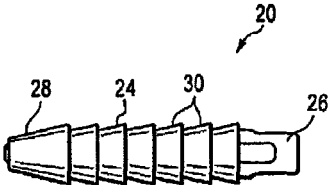


FIG. 9

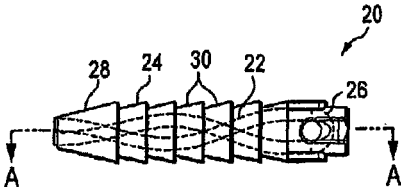
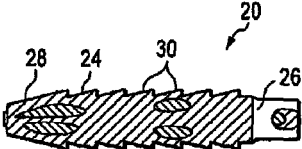


FIG. 10



FIG. 11



SECTION A-A  
FIG. 12

## SUTURE ANCHOR WITH INSERT-MOLDED RIGID MEMBER

This application is a continuation-in-part of U.S. application Ser. No. 11/097,172, filed on Apr. 4, 2005, now U.S. Pat. No. 8,343,186. This application is also a continuation-in-part of U.S. application Ser. No. 10/083,568, filed on Feb. 27, 2002, now U.S. Pat. No. 7,226,469, which claims priority to U.S. Provisional Application No. 60/271,414, filed on Feb. 27, 2001, and which is a continuation-in-part of U.S. application Ser. No. 09/495,816, filed on Feb. 2, 2000, now U.S. Pat. No. 6,517,564, which claims priority to U.S. Provisional Application No. 60/118,228, filed on Feb. 2, 1999 and U.S. Provisional Application No. 60/125,781, filed on Mar. 23, 1999. This application is also a continuation-in-part of U.S. application Ser. No. 11/224,060, filed on Sep. 13, 2005. This application also claims priority to U.S. Provisional Application No. 60/715,614, filed on Sep. 12, 2005. The disclosures of all of the above-cited applications are incorporated by reference in their entirety.

### FIELD OF THE INVENTION

The present invention relates to an apparatus for anchoring surgical suture to bone, and more particularly, to an apparatus using a suture anchor having a transverse anchor pin or an insert-molded eyelet shield.

### BACKGROUND OF THE INVENTION

When soft tissue tears away from bone, reattachment becomes necessary. Various devices, including sutures alone, screws, staples, wedges, and plugs have been used in the prior art to secure soft tissue to bone.

Recently, various types of threaded suture anchors have been developed for this purpose. Some threaded suture anchors are designed to be inserted into a pre-drilled hole. Other suture anchors are self-tapping.

U.S. Pat. No. 4,632,100 discloses a cylindrical threaded suture anchor. The suture anchor of the '100 patent includes a drill bit at a leading end for boring a hole in a bone, followed by a flight of threads spaced from the drill bit for securing the anchor into the hole created by the drill bit.

U.S. Pat. No. 5,370,662 discloses a suture anchor having threads which extend to the tip of the anchor. U.S. Pat. No. 5,156,616 discloses a similar suture anchor having an axial opening for holding a knotted piece of suture.

All of the above-noted suture anchors include a structure for attaching the suture to the anchor. U.S. Pat. No. 4,632,100, for example, discloses a press-fitted disc and knot structure which secures the suture to the anchor. In other suture anchors, such as those disclosed in U.S. Pat. No. 5,370,662, the suture is passed through an eyelet located on the proximal end of the anchor. In the case of a bioabsorbable suture anchor, the suture may be insert molded into the anchor, as disclosed in U.S. Pat. No. 5,964,783.

Problems can arise if the structure for attaching the suture fails, allowing the suture to become detached from the anchor. Also, the suture often is exposed to abrasion or cutting by sharp or rough areas along the walls of the bone canal into which the anchor is inserted.

Moreover, the eyelet or, in the case of U.S. Pat. No. 4,632,100, the axial opening for receiving the disc to which the suture is knotted, is formed as part of the drive head of the known suture anchors. Combining these two functions in one structure often tends to weaken the drive head.

In addition, various other modifications to the drive head often are employed in connection with suture attachment. For example, recessed grooves may be formed on opposite sides of the drive head to receive and protect the suture from abrasive areas of the suture anchor tunnel or to facilitate mating between the anchor to the driver. In such cases, the drive head often must be made of a larger diameter to recover the mechanical strength lost from the removal of material relating to the suture-attachment or suture-protection modifications.

Further, the prior art suture anchors having eyelets extending from the proximal ends require countersinking of the eyelet below the bone surface to avoid having the patient's tissue abrade against the exposed eyelet. As a result, suture attached to the eyelet is vulnerable to abrasion by the bony rim of the countersunk hole into which the suture anchor is installed. In addition, in biodegradable suture anchors, the suture eyelet can degrade rapidly, causing the suture to become detached from the anchor prematurely.

Accordingly, there is a need for a threaded suture anchor to which suture is secured effectively so as to prevent detachment of the suture. It is further desirable for such suture anchors to have eyelets that will not abrade tissue and which do not require countersinking.

Further, there is a need for a suture eyelet shield within a biodegradable suture anchor with a bearing surface that will resist suture cut-through of the bioabsorbable material.

### SUMMARY OF THE INVENTION

The suture anchor of the present invention overcomes the disadvantages of the prior art discussed above by providing, in one embodiment, a fully threaded suture anchor with an eyelet shield that is molded into the distal part of the biodegradable suture anchor. The eyelet shield of the present invention provides the strength necessary to secure the suture and also prevents suture cut-through.

The eyelet formed at the distal end is formed of a piece of suture or other material transversely insert-molded into the anchor so as to provide an eyelet shield. The shield provides a bearing surface that will resist suture cut-through.

In accordance with another embodiment of the invention, a ribbed suture anchor is provided with an eyelet shield at the proximal end. The eyelet shield is formed of a loop of suture material which is inserted molded within the suture anchor during the manufacturing process.

Other features and advantages of the present invention will become apparent from the following description of the invention, which refers to the accompanying drawings.

### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a side elevational view of the suture anchor according to an embodiment of the invention.

FIG. 2 is a longitudinal sectional view of the suture anchor shown in FIG. 1 through the plane D-D indicated therein.

FIG. 3 is a proximal end view of the suture anchor of FIG. 1.

FIG. 4A is a cross sectional view of the suture anchor of FIG. 1 showing a suture looped over the transverse anchor pin.

FIG. 4B is a cross sectional view of the suture anchor of FIG. 1 showing a portion of a polygonal driver inserted into a polygonally shaped bore of the suture anchor.

FIG. 4C is a cross sectional view of the suture anchor of FIG. 1 showing the polygonal driver inserted into a polygonally shaped bore of the suture anchor.

FIG. 5 is a perspective representation of the suture anchor according to another embodiment of the invention.

FIG. 6 is an end view of the suture anchor shown in FIG. 5.

FIG. 7A is an elevational cross-section of the suture anchor of FIG. 6 through the plane B-B indicated therein.

FIG. 7B is an elevational cross-section of the suture anchor of FIG. 6 through the plane B-B indicated therein showing a portion of a driver inserted into a bore of a suture anchor.

FIG. 8 is a cross-section in plan view of the suture anchor of FIG. 6 through the plane C-C indicated therein.

FIG. 9 is a plan view of the push-in suture anchor according to another embodiment of the invention.

FIG. 10 is a plan view of the push-in suture anchor of FIG. 9 showing a suture insert-molded within the suture anchor.

FIG. 11 is a proximal end view of the suture anchor of FIG. 9.

FIG. 12 is a longitudinal sectional view of the suture anchor shown in FIG. 9 through the plane A-A, indicated therein.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

In the following detailed description, reference is made to various specific embodiments in which the invention may be practiced. These embodiments are described with sufficient detail to enable those skilled in the art to practice the invention, and it is to be understood that other embodiments may be employed, and that structural and logical changes may be made without departing from the spirit or scope of the present invention.

FIG. 1 illustrates a suture anchor according to a first preferred embodiment of the present invention, indicated generally by reference numeral **110**. In the preferred embodiment, body **108** of anchor **110** generally tapers to a narrow point **114** at the distal end thereof. In particular, the major diameter of the anchor body is generally constant along about two-thirds of the length of the body, whereupon the diameter of the anchor then tapers to a relatively sharp point, e.g., approximately 16°. The relatively sharp distal tip of anchor **110** enables the anchor to be installed without having to first drill a hole in the bone where the anchor **110** is to be installed.

Although such tapering is preferred, suture anchor **110** may be formed to have a less tapered shape, or even cylindrical shape, to accommodate different preferences of the surgeon and/or the application of the suture anchor. For example, the tapered distal end of the anchor may be formed to be more blunt, in which case it is necessary to provide a pre-formed hole in the bone prior to insertion of the suture anchor.

A continuous thread **116** wraps around the body **108** in a clockwise direction, as shown. Anchor **110** has about five flights of thread, with the angle of the threads and other configurations of the anchor being similar to the suture anchor of U.S. Pat. No. 6,511,499, the disclosure of which is hereby incorporated by reference in its entirety.

As can be seen more clearly with reference to FIG. 3, the proximal end portion of the anchor has a polygonally shaped bore **134**, preferably hexagonal or square, having an opening **112** at the proximal end **92** of anchor body **108** and extending into the anchor body approximately one-third of the length thereof. Prior art anchors have sharp edges around the drive opening, which is problematic in that sutures passing through the central opening at the proximal end **92** of the anchor can be abraded by the sharp edges, thereby compromising the strength of the sutures. In the suture anchor of the present invention, the peripheral edges defining polygonally shaped opening **112** is smooth and rounded outwardly with no sharp edges. Preferably, the opening **112** forms a slight lip curving

around the diameter of the bore **134**. Thus, sutures threaded through the anchor **110**, as will be discussed below, will not become frayed upon being pressed or rubbed against the anchor at the proximal opening **112**.

As shown in FIG. 2, a cylindrical bore **136** having a diameter corresponding to that of the polygonally shaped bore **134** extends from the distal end of the polygonally shaped bore **134** to a position roughly halfway along the length of anchor body **108**. The transition between polygonally shaped bore **134** and cylindrical bore **136** forms an annular shoulder **140**, against which the distal end of a polygonal driver **202**, preferably hexagonal or square, abuts when inserted into the polygonally shaped bore **134** to drive the anchor into bone.

Two longitudinal, diametrically opposite apertures **118** are formed in anchor body **108**, the apertures **118** supporting a metal transverse anchor pin **120** which extends across cylindrical bore **136**.

As illustrated in FIGS. 1, 2 and 4a, apertures **118** extend through and interrupt the threads **116** around anchor body **108** at approximately one-third of the length of the anchor body from the proximal end **92** thereof. One or more sutures **200** are secured to the anchor by looping the suture(s) around metal anchor pin **120** as shown in FIG. 4a. Although the metal anchor pin **120** is illustrated in FIGS. 2 and 4a as oriented transversal to longitudinal axis **150** of the anchor body **108**, the metal anchor pin **120** may form any angle with the longitudinal axis **150** and, thus, the invention is not limited to metal anchor pin **120** forming an angle of about ninety degrees with the longitudinal axis **150** of the anchor body **108**.

Preferably, suture anchor **110** is formed of a hard biocompatible metal, such as a titanium alloy, but can be made of biocompatible materials other than metal. The suture secured to the anchor may be FiberWire suture, sold by Arthrex, Inc. of Naples, Fla.

The suture anchor according to the present invention need not be formed as a threaded device, but can also be formed as a tap-in type anchor. Also, the measurements, angles and ratios between the dimensions of the suture anchor may be varied from those described above so as to be suitable for the conditions and applications in which the suture anchor is to be used.

In manufacturing the suture anchor **110** in accordance with the present invention, the anchor body **108** is cast in a die, with the bores, passageways and apertures described above either being formed during the casting process or formed afterwards. If necessary, the distal tip **114** of the anchor **110** is trimmed to the desired length and the surfaces of the anchor are polished to the desired finish.

As mentioned above, the suture anchor **110** of the present invention may be installed in the bone without the need to pre-drill a hole in the bone. The suture anchor **110** is installed using a driver **202** having a shaft having a polygonal cross-section for at least a length equal to the length of the polygonal bore **134** from proximal opening **112** to the shoulder **140** inside the anchor **110**. The driver **202** has a cannula **204** extending through the entire length thereof, with openings **216** and **214** at the proximal end and the distal end, respectively, thereof. Of course, the outer diameter of the polygonal shaft is sized to fit inside the polygonal bore in the anchor so as to be enabled to drive the same.

As shown in FIGS. 4b and 4c, with the desired number of suture strands **200** threaded around the anchor pin **120** in the suture anchor **110**, the ends **206** and **208** of the suture strands **200** are threaded through the cannula **204** in the polygonal driver **202** from the distal end thereof and extend from the proximal opening **216** thereof. The distal end of the polygonal driver **202** is inserted into the proximal end **92** of the anchor

110. With the distal end of the driver **202** abutting the shoulder **140** and the anchor **110** positioned at the location at which it is to be installed, the polygonal driver **202** is rotated to drive the anchor **110** into the bone until the proximal surface of the anchor **110** is flush with the surface of the bone.

Since it is not necessary for the proximal end **92** of the anchor to be countersunk below the bone surface to prevent tissue abrasion by an exposed suture loop, as is required with prior art devices, the suture anchor of the present invention does not need to be inserted as far as the prior art anchors, while also avoiding abrasion of the sutures by the rim of the bone.

The suture anchor of the present invention provides greater pull-out strength of the suture loop than prior suture anchors. In addition, the suture loop of the present invention, being disposed inside the suture anchor, is protected from abrasion and degradation.

Referring to FIG. 5, a suture anchor **1** is shown in perspective in accordance with another embodiment of the invention. In this embodiment, the suture anchor **1** has a fully-threaded body **3**. The suture anchor **1** may be comprised of any material. Preferably, the suture anchor **1** is formed of a bioabsorbable material. Rather than having an anchor pin as discussed in the embodiment above, the suture anchor **1** has an eyelet shield **9** molded transversely into a distal part **11** of the threaded body **3** of the suture anchor **1**. Eyelet shield **9** is shown as a bar, however, any appropriate type of material may be used, including bioabsorbable material or a length of suture, for example. The eyelet shield **9** can include of a length of suture **90** molded transversely into distal part **11** of threaded body **3**. Although the shield **9** is illustrated as being transverse to the longitudinal axis of suture anchor **1**, the shield **9** may also be formed at any angle with respect to the longitudinal axis and, thus, the invention is not limited to shield **9** formed at angle of about ninety degrees with the longitudinal axis of the suture anchor **1**.

As illustrated in FIGS. 6-8, two strands of tie-down sutures **5, 7** are threaded around the eyelet shield **9** of the distal end **11** of the suture anchor **1** and threaded into a suture passage **94**. In one example, there is a suture passage **94** on opposing sides of the shield **9**. The shield **9** provides a bearing surface around which sutures **5, 7** are threaded and disposed. The sutures **5, 7** are threaded through a bore **15** and disposed about the shield **9** and have ends **306** and **308** that extend out of the proximal end **92** of the anchor **1**. The bore **15** extends from the proximal end **92** of the suture anchor **1** to a location roughly halfway along the anchor body **1**. As discussed above, the bore **15** has an opening at the proximal end **92** of the suture anchor and is shaped to accommodate a driver head for driving the suture anchor.

The eyelet shield **9** resists suture cut-. Further, the shield **9** provides the strength necessary to secure the sutures **5, 7**. In addition, because the eyelet shield is molded transversely into the distal end of the suture anchor, this provides greater security to prevent pull-out of the suture from within the suture anchor or from an anchor pin, which could loosen. The eyelet shield also prevents the suture from fraying.

Although a fully-threaded suture anchor **1** with threaded body **3** is shown, the anchor does not necessarily have to be fully threaded. As discussed above, the suture anchor also need not be a threaded device, but can also be formed as a tap-in type anchor. In addition, sutures **5, 7** can be insert-molded into the anchor to prevent saw-through.

The suture anchor **1** is installed using a driver **300**. The driver **300** has a cannula **302** with openings at the proximal and distal ends thereof. As shown in FIGS. 7A and 7B, with the desired number of sutures **5** and **7** threaded around the

shield **9** in the suture anchor **1**, ends **306** and **308** of the sutures **5** and **7** are threaded through the cannula **302** in the driver **300** from a distal end **310** thereof and extend from the proximal opening **312** thereof. The distal end of the driver **300** is inserted into the proximal end **92** of the anchor **1**, and the driver **300** is rotated to drive the anchor **1** into the bone until the proximal surface of the anchor **1** is flush with the surface of the bone.

In another embodiment, as illustrated in FIGS. 9-12, a push-in suture anchor **20** is shown having suture **22** that is insert-molded longitudinally into the suture anchor body **24** during the manufacturing process.

The suture anchor body **24** preferably is formed of a bioabsorbable material, poly(l-lactide-co-d, l-lactide) 70:30 (PLDLA) being most preferred. Suture **22** can be any known type of suture selected according to the size of the anchor and the anticipated application. The suture **22** preferably is No. 2 polyester braided suture.

At least one length of the insert-molded suture **22** extends from the proximal end **92** of the suture anchor body **24**. Preferably, the suture **22** extends from the suture anchor body **24** in the form of a loop. The suture **22** is insert-molded into the suture anchor body **24** and also into the loop or eyelet **26**. Various devices provide a suture anchor with a loop formed of a suture material, as disclosed in U.S. Publication No. 2002/0087190 and U.S. application Ser. No. 11/224,060, the entire disclosures of which are incorporated by reference herein. However, the suture loops disclosed in these applications are not encapsulated—this results in friction between the suture loop and a suture threaded through the loop. In the present invention, the suture **22**, being insert-molded within the loop **26**, eliminates suture against suture friction and provides better support and strength for a suture threaded through the loop.

The distal end **28** of the suture anchor body **24** tapers to a blunt tip. Suture anchor **20** is provided with slotted ribs **30** formed circumferentially at least partially around and partially along the length of body **24**. Ribs **30** have a truncated, conical anchor at an angle of preferably 15° with respect to the longitudinal axis of anchor **20**, and reaching a major diameter of 3.0 mm.

Although PLDLA is the most preferred material for the suture anchor of the present invention, other bioabsorbable materials known in the art can be utilized. As used herein, bioabsorbable is considered to be interchangeable with biodegradable, resorbable, and absorbable to mean that the device can be at least partially absorbed by the body over time. Preferably, the anchor material is selected so as to absorb or degrade substantially completely within 12-16 months of implantation.

Although the present invention has been described in relation to particular embodiments thereof, many other variations and modifications and other uses will become apparent to those skilled in the art. Therefore, the present invention is to be limited not by the specific disclosure herein, but only by the appended claims.

What is claimed as new and desired to be protected by Letters Patent of the United States is:

1. A suture anchor comprising:
  - an anchor body having a longitudinal axis, a proximal end, a distal end, a central passage, a first suture opening, and a second suture opening, wherein the central passage extends along the longitudinal axis, the central passage extends from the first suture opening which is located at the proximal end of the anchor body and through a portion of a length of the anchor body, the first suture

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opening is encircled by a perimeter of the anchor body, and the second suture opening extends through a portion of the anchor body;

a rigid support fixed to the anchor body, wherein the rigid support extends across the central passage and has a first portion and a second portion spaced from the first portion, the first portion branching from a first wall portion of the anchor body and the second portion branching from a second wall portion of the anchor body, the rigid support spaced axially away from the first suture opening along the longitudinal axis of the anchor body, and the second suture opening is disposed near the rigid support; and

at least one suture strand threaded into the central passage, wherein the at least one suture strand is supported by the rigid support and threaded through the first suture opening and the second suture opening of the anchor body.

2. The suture anchor according to claim 1, wherein the second suture opening is defined in part by the rigid support and a portion of the anchor body.

3. The suture anchor according to claim 2, including a third suture opening extending through the anchor body, wherein the third suture opening is disposed distal of the second suture opening, and the at least one suture strand is disposed in the first suture opening, the second suture opening, and the third suture opening.

4. The suture anchor according to claim 3, wherein the third suture opening forms in part a suture passage that extends across the longitudinal axis of the anchor body.

5. The suture anchor according to claim 3, wherein the at least one suture strand follows a path beginning with a first end of the at least one suture strand outside of the anchor body, through the first suture opening, through the central passage, through the second suture opening, through the third suture opening, around the rigid support, back through the central passage, back through the first suture opening, and ending at a second end of the at least one suture strand outside of the anchor body.

6. The suture anchor according to claim 1, wherein the at least one suture strand follows a path beginning with a first end of the at least one suture strand outside of the anchor body, through the first suture opening, through the central passage, through the second suture opening, around the rigid support, back through the central passage, back through the first suture opening, and ending at a second end of the at least one suture strand outside of the anchor body.

7. The suture anchor according to claim 1, wherein the second suture opening is located in a distal half of the anchor body, and the distal half includes the distal end of the anchor body.

8. The suture anchor according to claim 1, wherein the suture anchor and the rigid support are made of the same material.

9. The suture anchor according to claim 1, wherein the second suture opening forms in part a suture passage that extends along the longitudinal axis of the anchor body to the first suture opening.

10. A suture anchor assembly comprising:

an anchor body including a longitudinal axis, a proximal end, a distal end, and a central passage extending along

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the longitudinal axis from an opening at the proximal end of the anchor body through a portion of a length of the anchor body, wherein the opening is a first suture opening, the anchor body including a second suture opening disposed distal of the first suture opening, and a third suture opening disposed distal of the second suture opening, wherein a helical thread defines a perimeter at least around the proximal end of the anchor body;

a rigid support extending across the central passage, the rigid support having a first portion and a second portion spaced from the first portion, the first portion branching from a first wall portion of the anchor body and the second portion branching from a second wall portion of the anchor body, wherein the third suture opening is disposed distal of the rigid support;

at least one suture strand having a suture length threaded into the central passage, supported by the rigid support, and threaded past the proximal end of the anchor body, wherein at least a portion of the at least one suture strand is disposed in the central passage between the rigid support and the opening at the proximal end, and the at least one suture strand is disposed in the first suture opening, the second suture opening, and the third suture opening; and

a driver including a shaft having a shaft length, wherein the shaft engages the anchor body, and the suture length of the at least one suture strand is greater than the shaft length of the shaft.

11. A suture anchor assembly comprising:

an anchor body including a distal end, a proximal end having, an opening, a central longitudinal axis, a first wall portion, a second wall portion spaced opposite to the first wall portion, and a suture passage beginning at the proximal end of the anchor body, wherein the suture passage extends about the central longitudinal axis, and the suture passage extends from the opening located at the proximal end of the anchor body and at least partially along a length of the anchor body, wherein the opening is a first suture opening that is encircled by a perimeter of the anchor body, a second suture opening extends through a portion of the anchor body, and a third suture opening extends through the anchor body, wherein the third suture opening is disposed distal of the second suture opening;

a rigid support integral with the anchor body to define a single-piece component, wherein the rigid support extends across the suture passage and has a first portion and a second portion spaced from the first portion, the first portion branching from the first wall portion of the anchor body and the second portion branching from the second wall portion of the anchor body, and the rigid support is spaced axially away from the opening at the proximal end along the central longitudinal axis; and

at least one suture strand threaded into the suture passage, supported by the rigid support, and having ends that extend past the proximal end of the anchor body, and the at least one suture strand is disposed in the first suture opening, the second suture opening, and the third suture opening.

\* \* \* \* \*



UNITED STATES PATENT AND TRADEMARK OFFICE  
**CERTIFICATE OF CORRECTION**

PATENT NO. : 8,821,541 B2  
APPLICATION NO. : 11/518872  
DATED : September 2, 2014  
INVENTOR(S) : Peter J. Dreyfuss et al.

Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

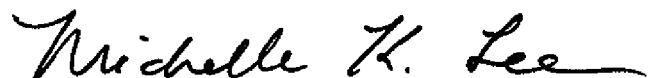
IN THE CLAIMS:

In claim 2, column 7, line 20; delete “a” and replace with --the--

In claim 10, column 8, line 16; delete “hayng” and replace with --having--

In claim 11, column 8, line 31; after “having” delete “,”

Signed and Sealed this  
Ninth Day of December, 2014



Michelle K. Lee  
*Deputy Director of the United States Patent and Trademark Office*