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(12) **United States Patent
McBride**

(10) **Patent No.: US 10,463,563 B2**
(45) **Date of Patent: Nov. 5, 2019**

(54) **METHODS AND APPARATUS FOR BODY
WEIGHT SUPPORT SYSTEM**

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(71) Applicant: **Bioness Inc.**, Valencia, CA (US)

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(72) Inventor: **Keith McBride**, Ventura, CA (US)

(73) Assignee: **Bioness Inc.**, Valencia, CA (US)

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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 490 days.

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(21) Appl. No.: **14/613,140**

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(65) **Prior Publication Data**

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Primary Examiner — Megan Anderson

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(57)

ABSTRACT

An apparatus includes a drive mechanism, a patient support mechanism, and an electronic system. The drive mechanism is included in a trolley and is configured to suspend the trolley from a support track. The drive mechanism includes a first sensor configured to sense an operating condition of the drive mechanism. The patient support mechanism couples to the trolley and includes a tether and a second sensor. The tether can be operatively coupled to a patient such that the patient support mechanism supports the patient. The second sensor is configured to sense an operating condition of the patient support mechanism. The electronic system is included in the trolley and has at least a processor and a memory. The processor is configured to define a gait characteristic of the patient based at least in part on a signal received from the first sensor and a signal received from the second sensor.

Related U.S. Application Data

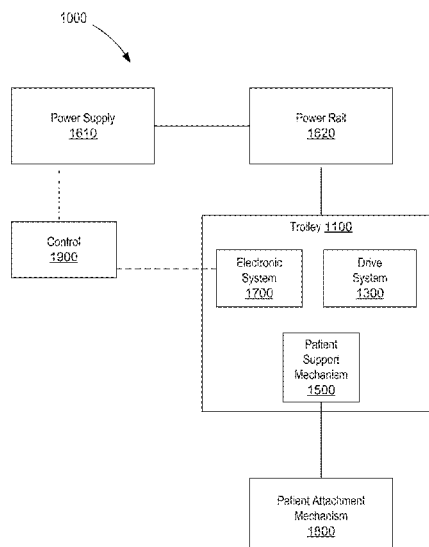
(63) Continuation-in-part of application No. 14/226,021, filed on Mar. 26, 2014, which is a
(Continued)

(51) **Int. Cl.**
A61H 3/00 (2006.01)
A61G 7/10 (2006.01)

(52) **U.S. Cl.**
CPC **A61H 3/008** (2013.01); **A61G 7/1001**
(2013.01); **A61G 7/1015** (2013.01);
(Continued)

(58) **Field of Classification Search**
CPC A61H 2201/0188; A61H 2201/5007; A61H
2201/5084; A61H 2201/5079;
(Continued)

20 Claims, 53 Drawing Sheets



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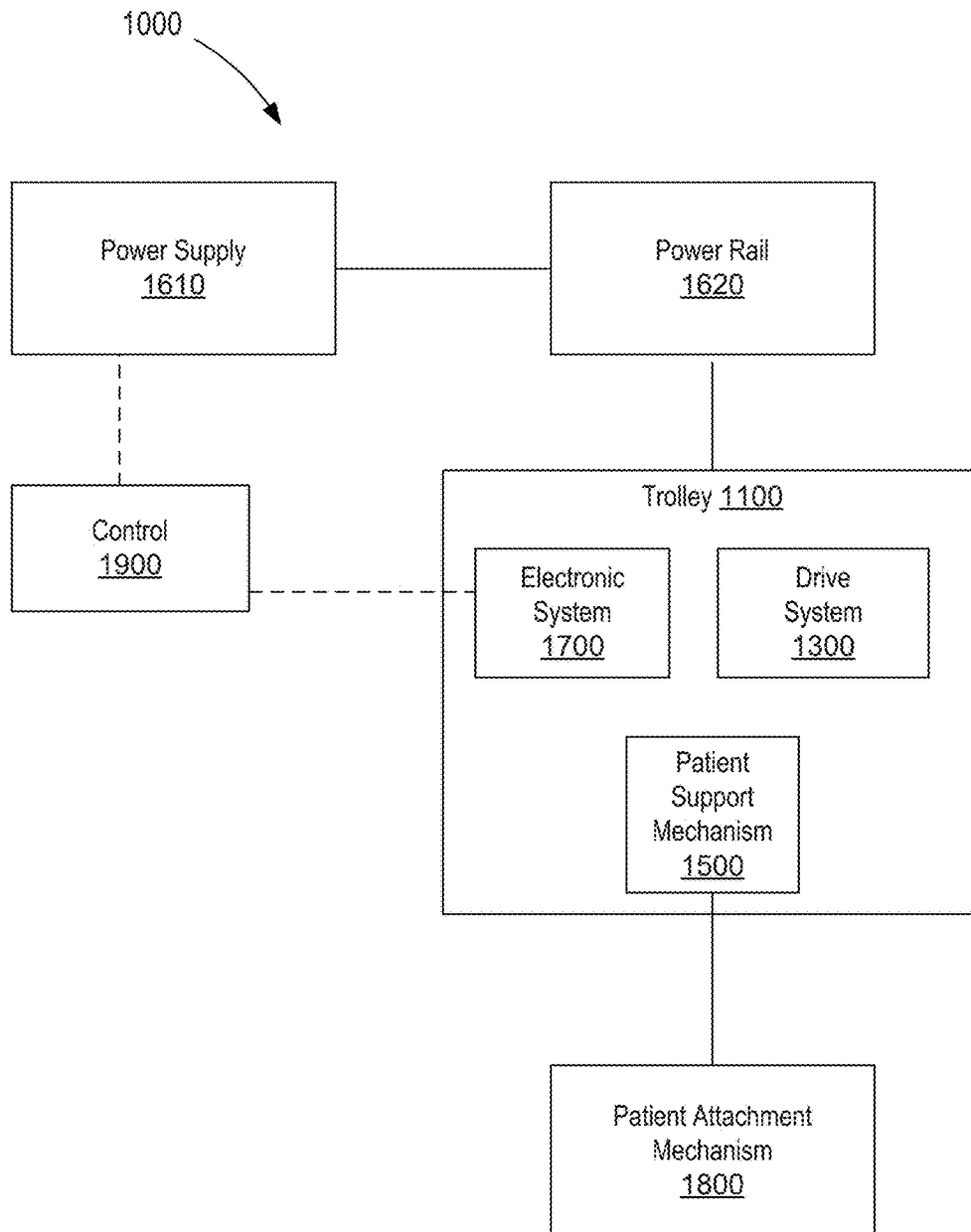


FIG. 1

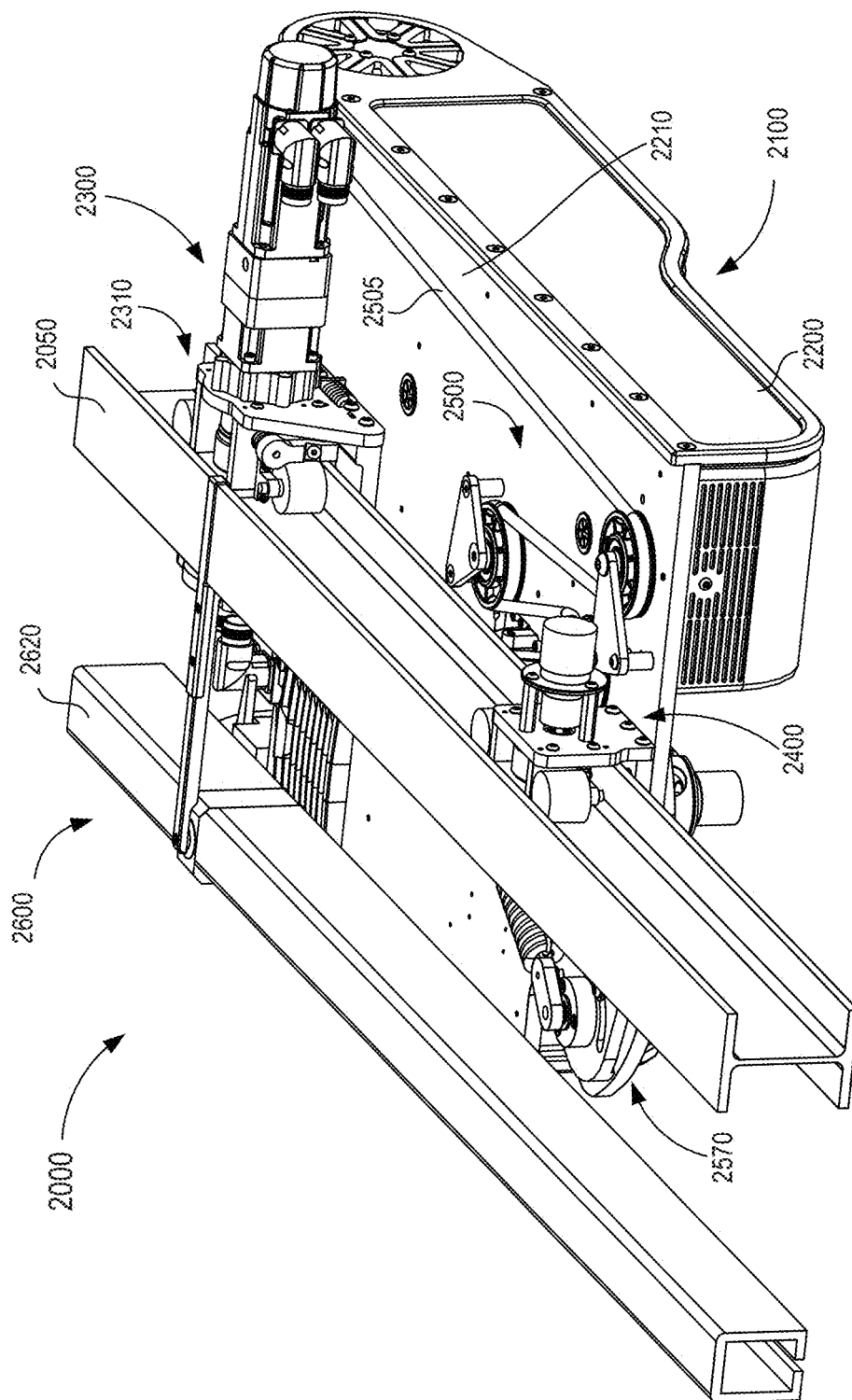
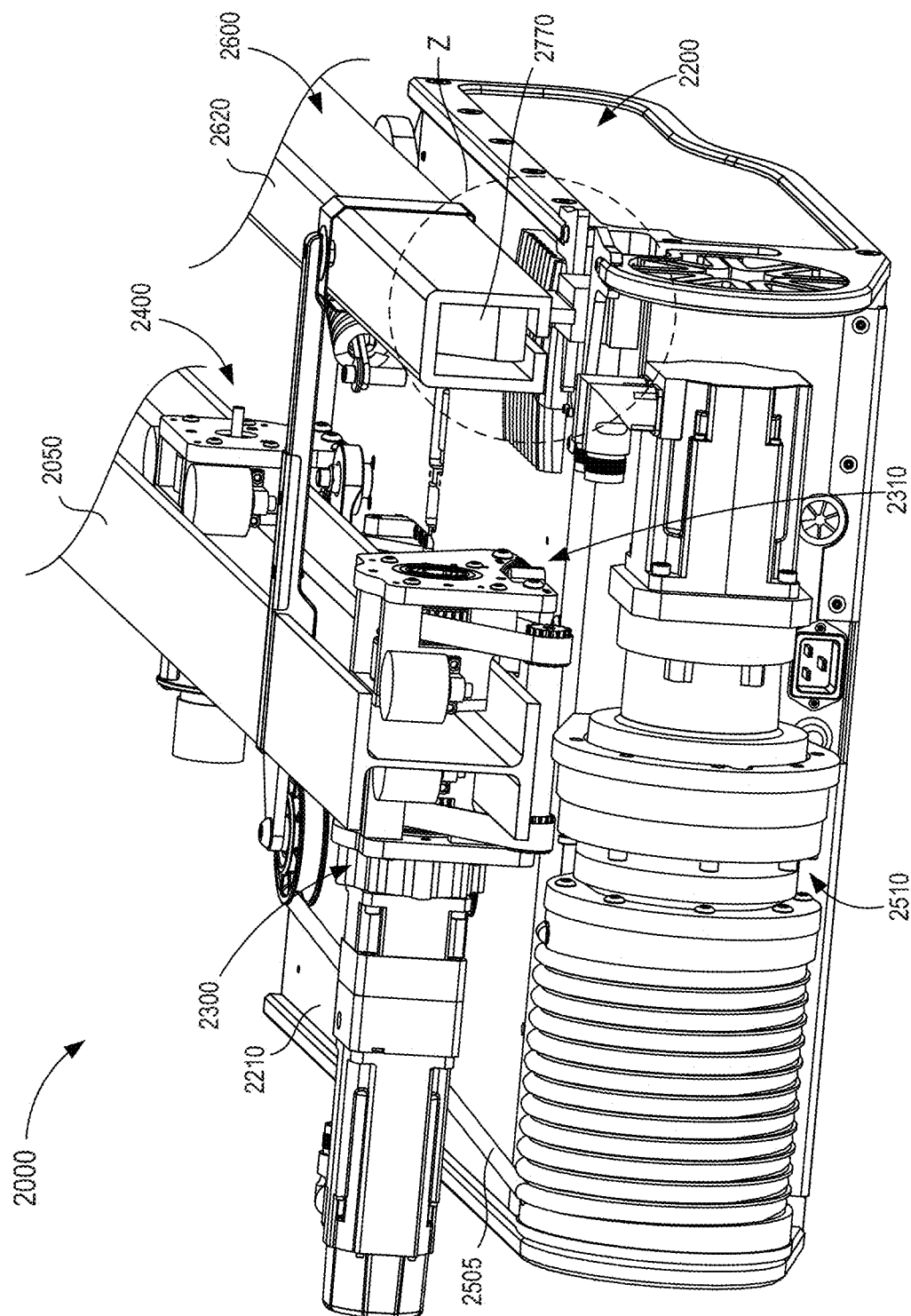


FIG. 2



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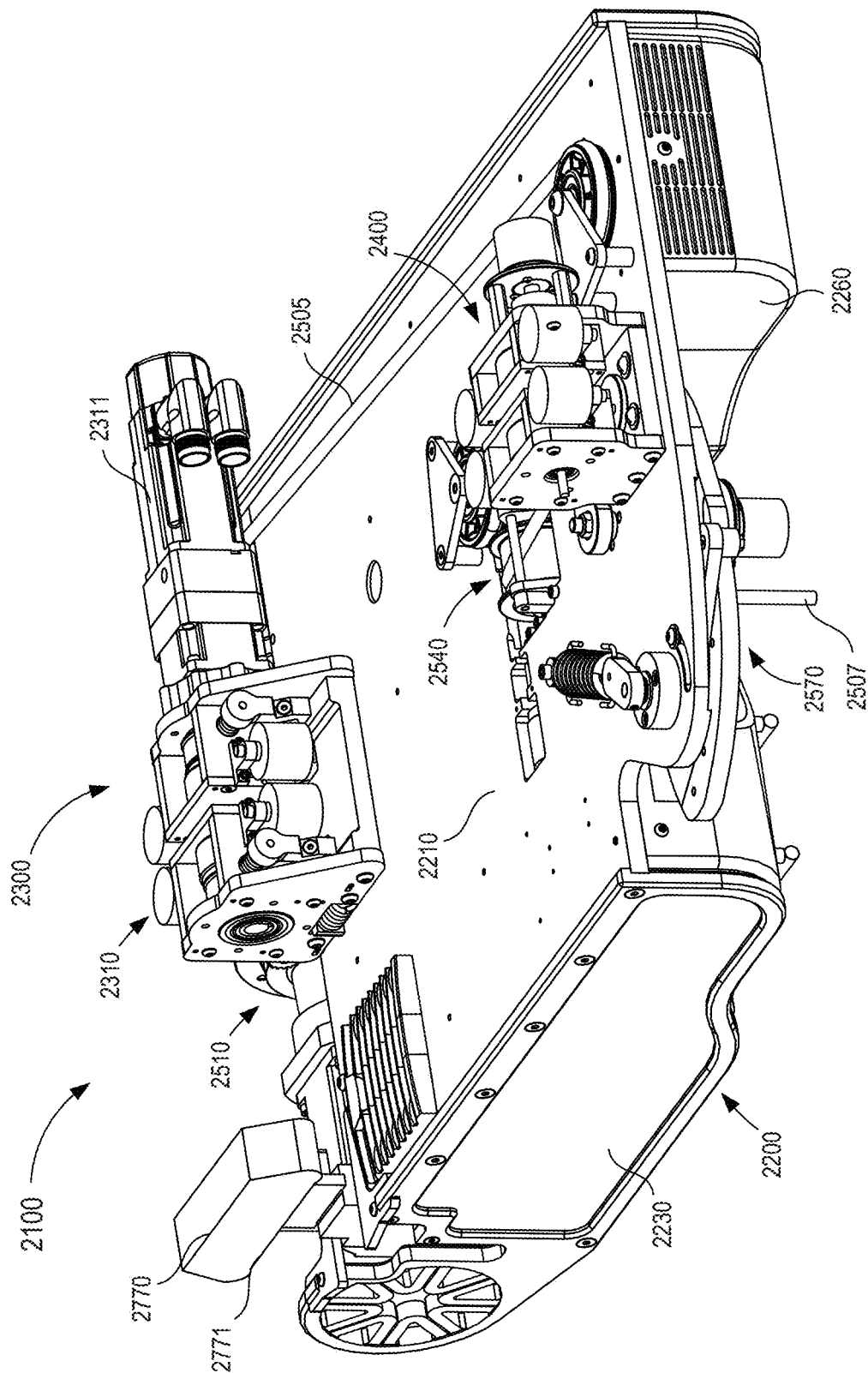


FIG. 4

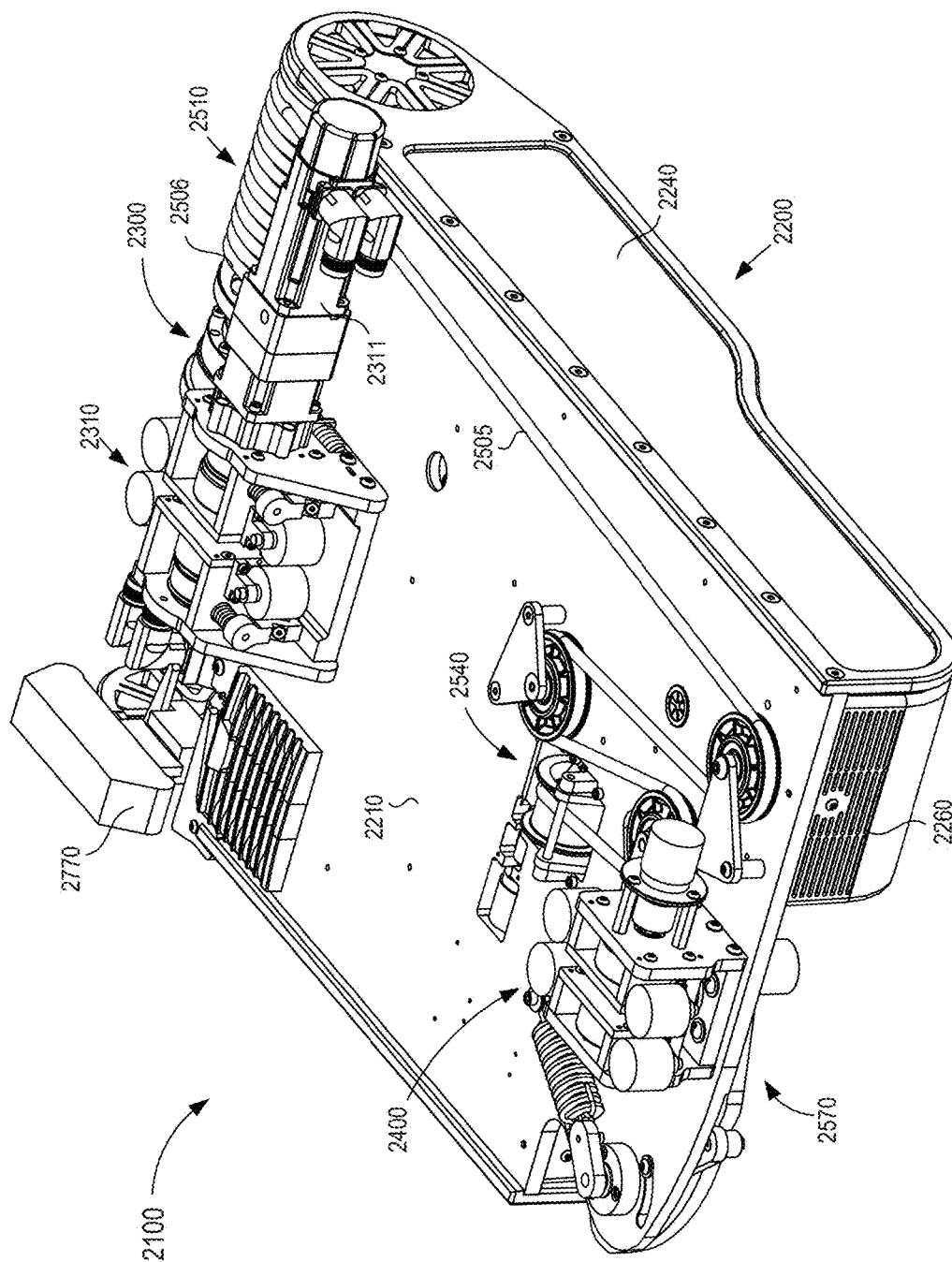


FIG. 5

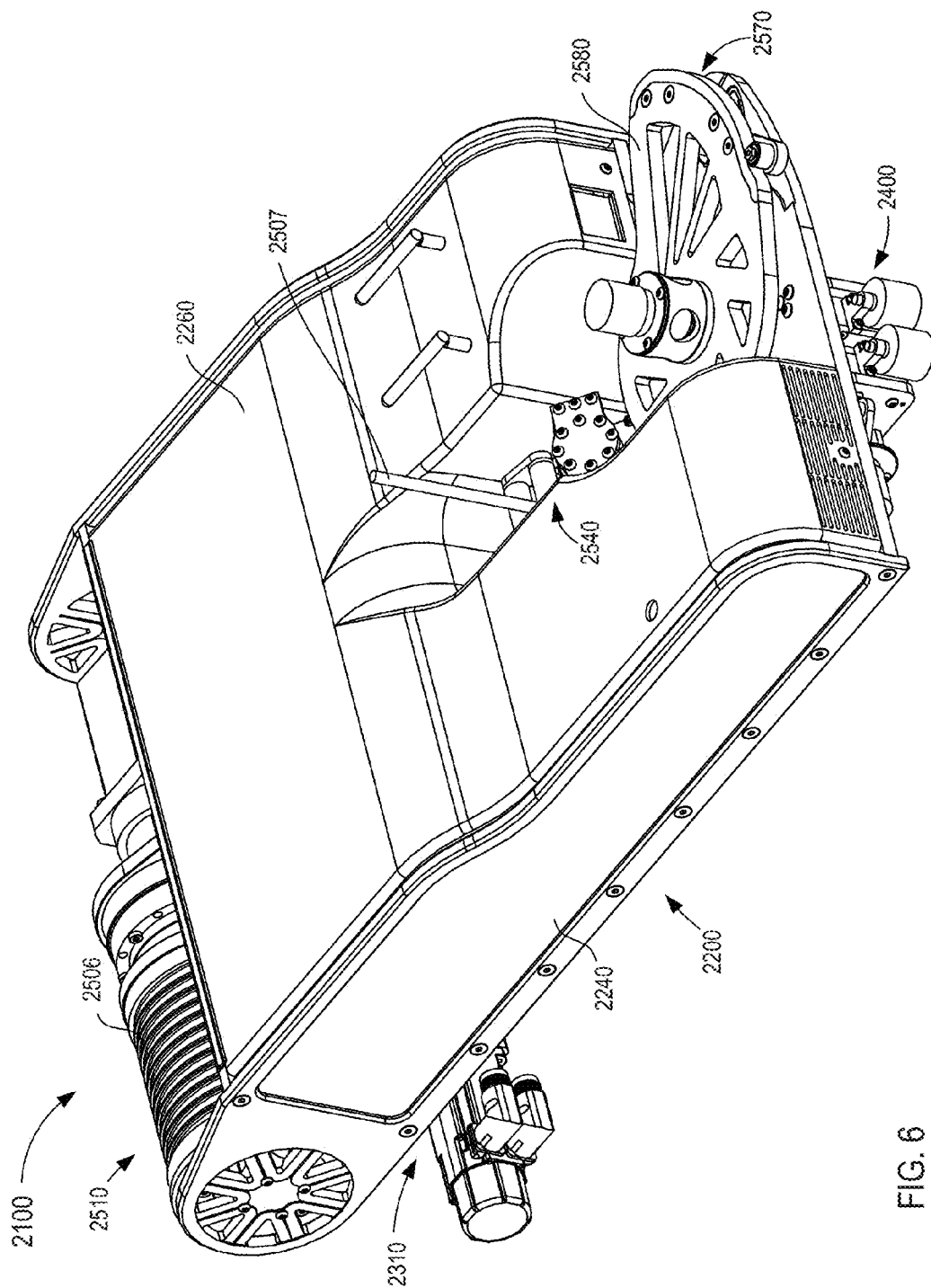


FIG. 6

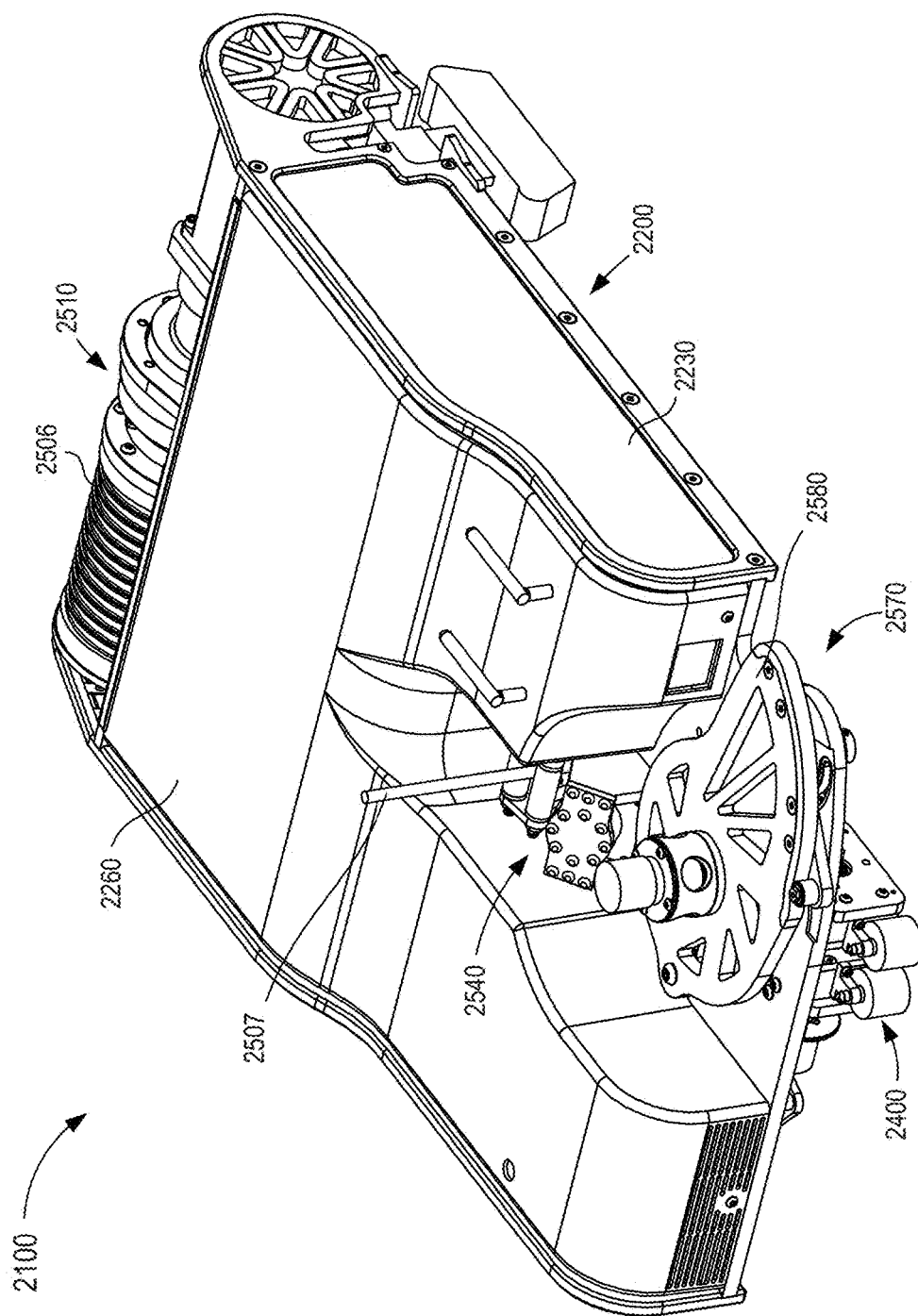


FIG. 7

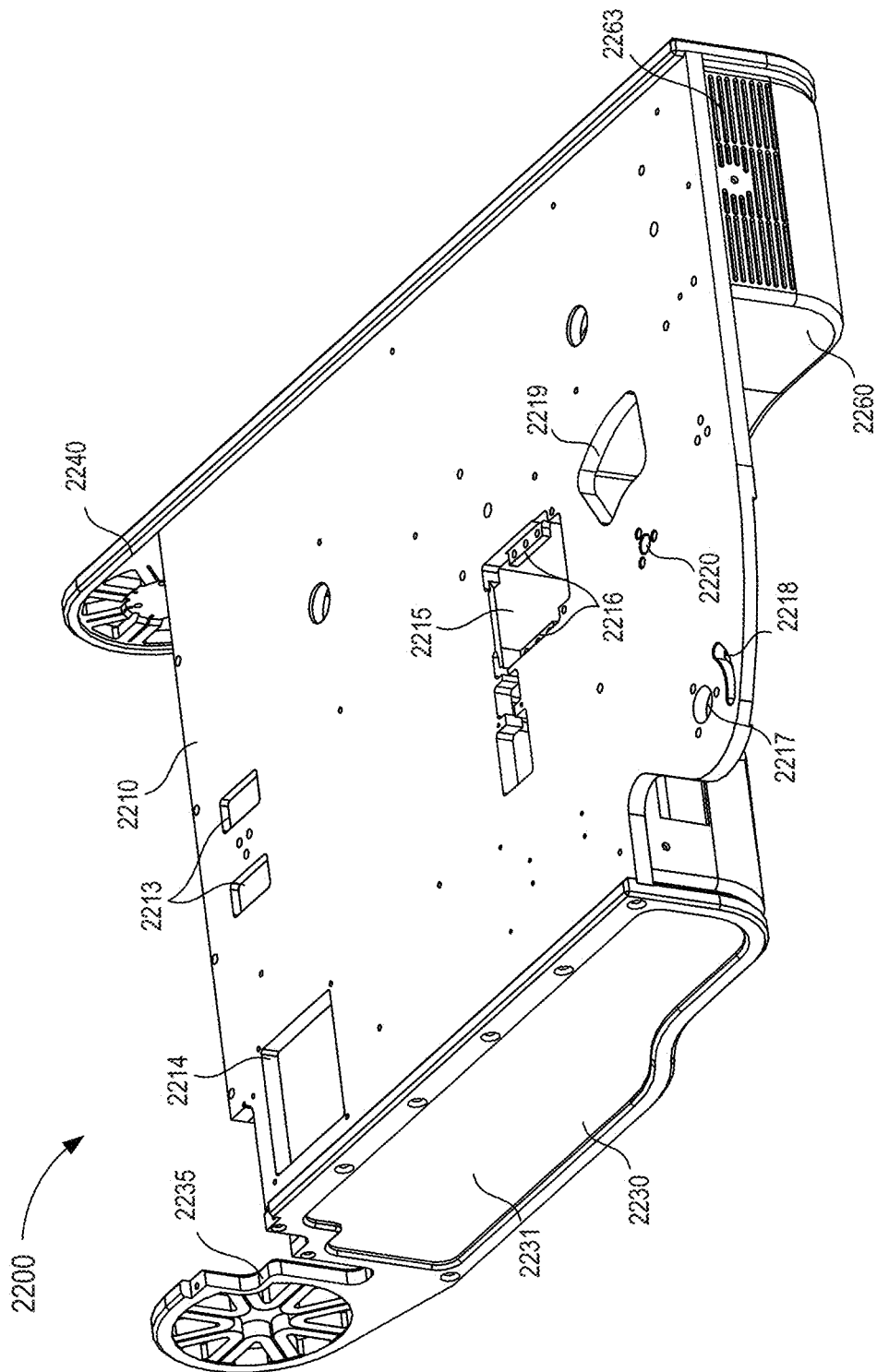


FIG. 8

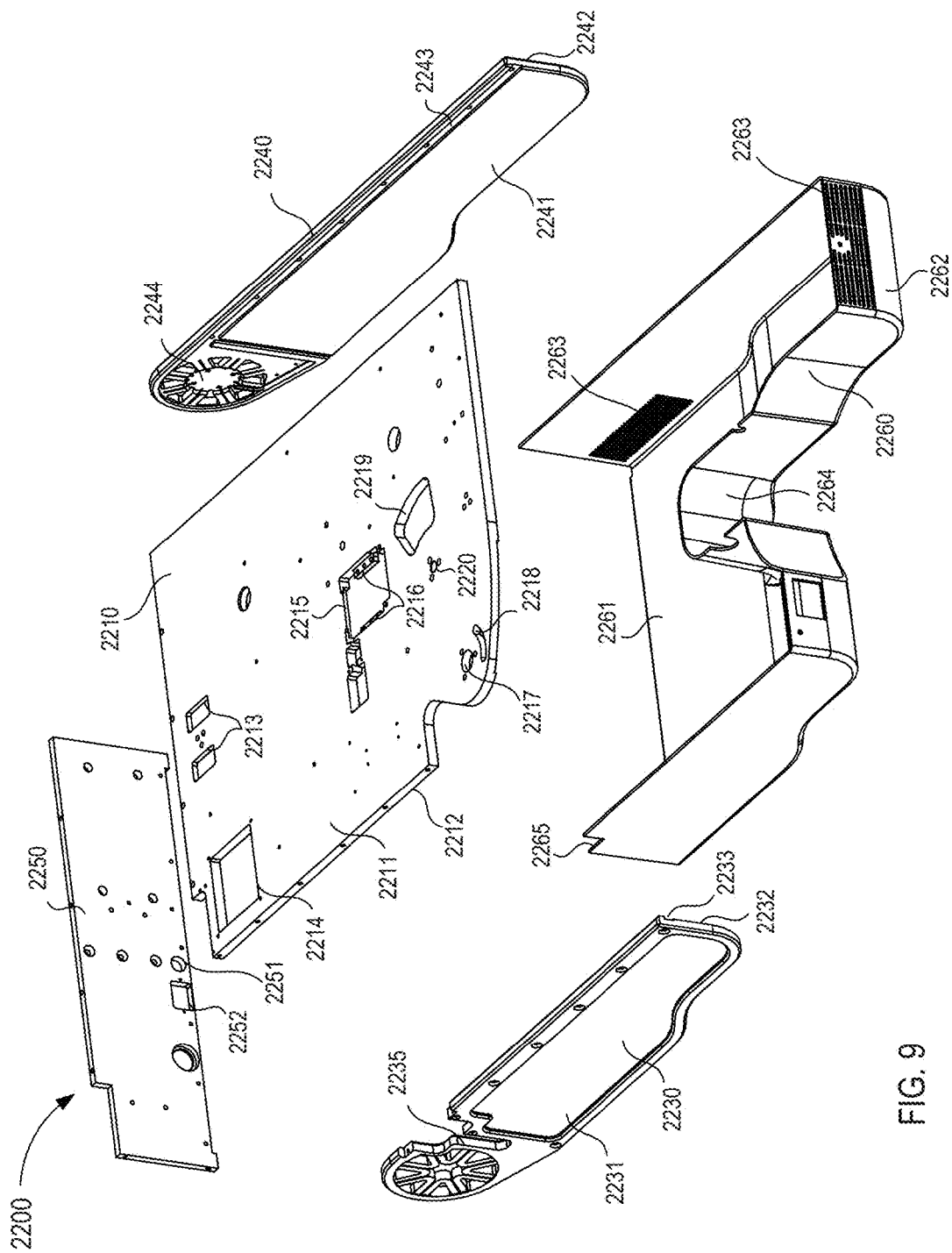


FIG. 9

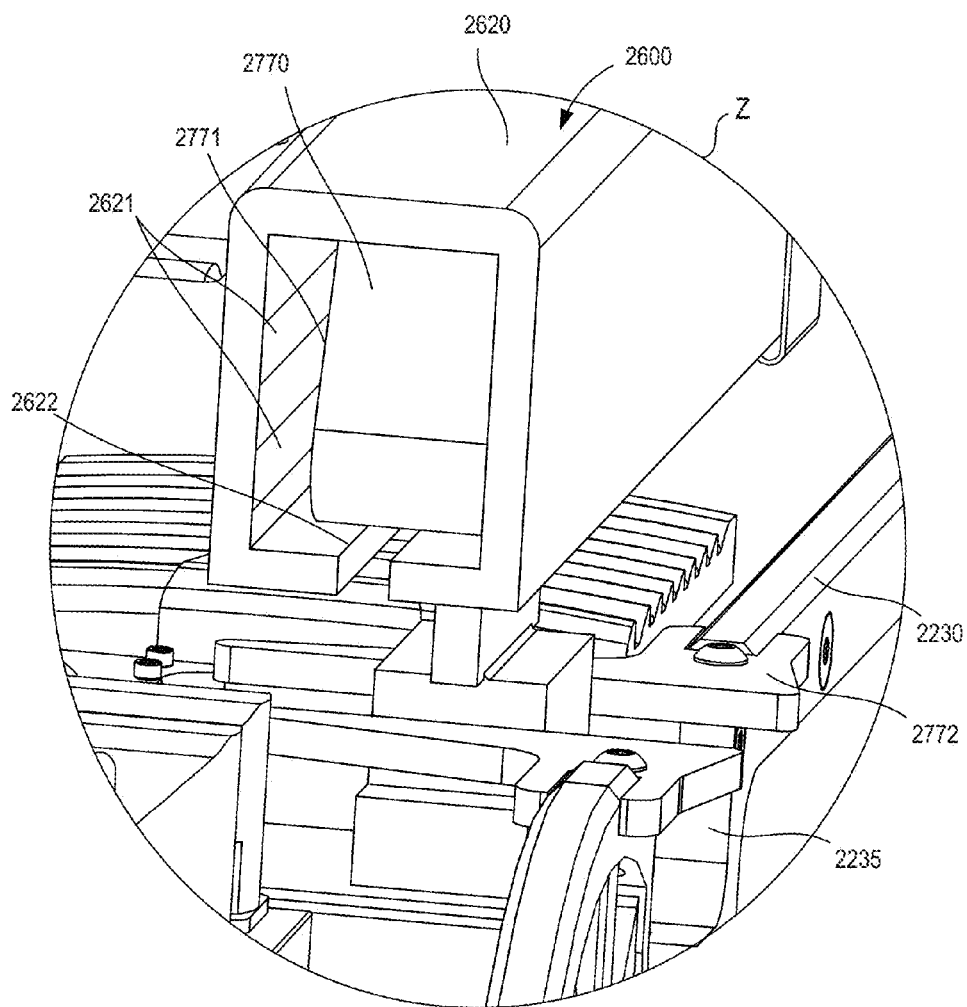
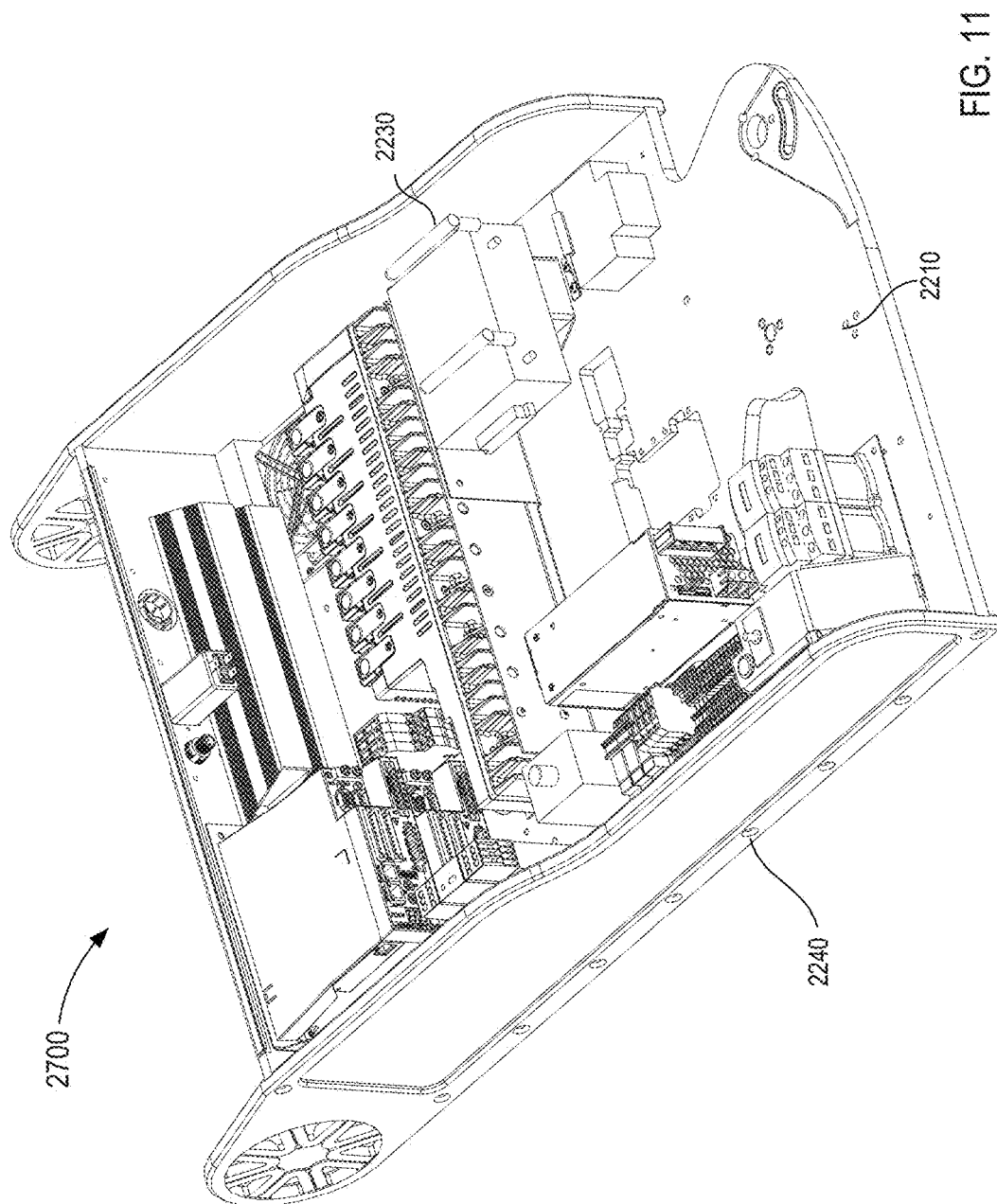


FIG. 10



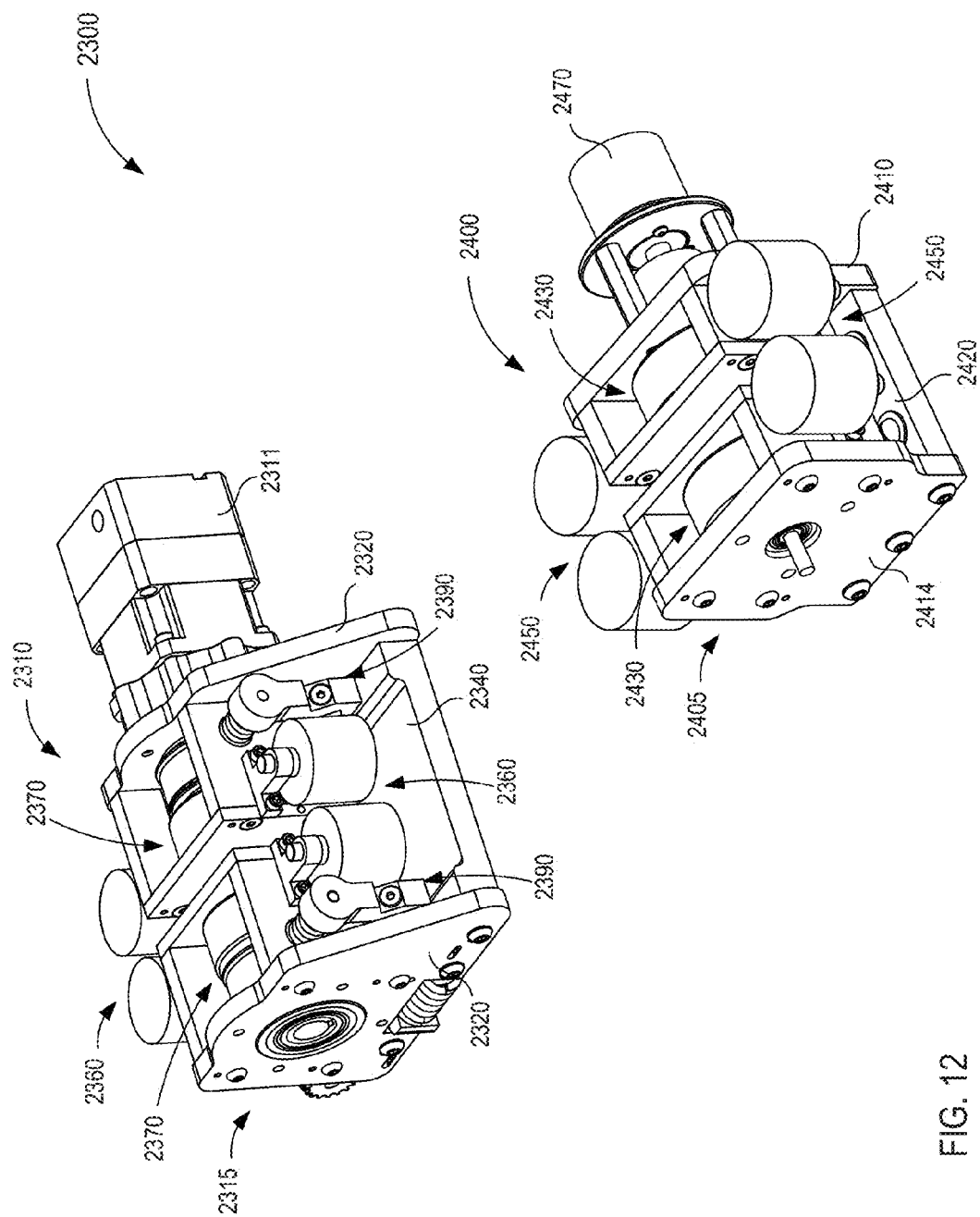


FIG. 12

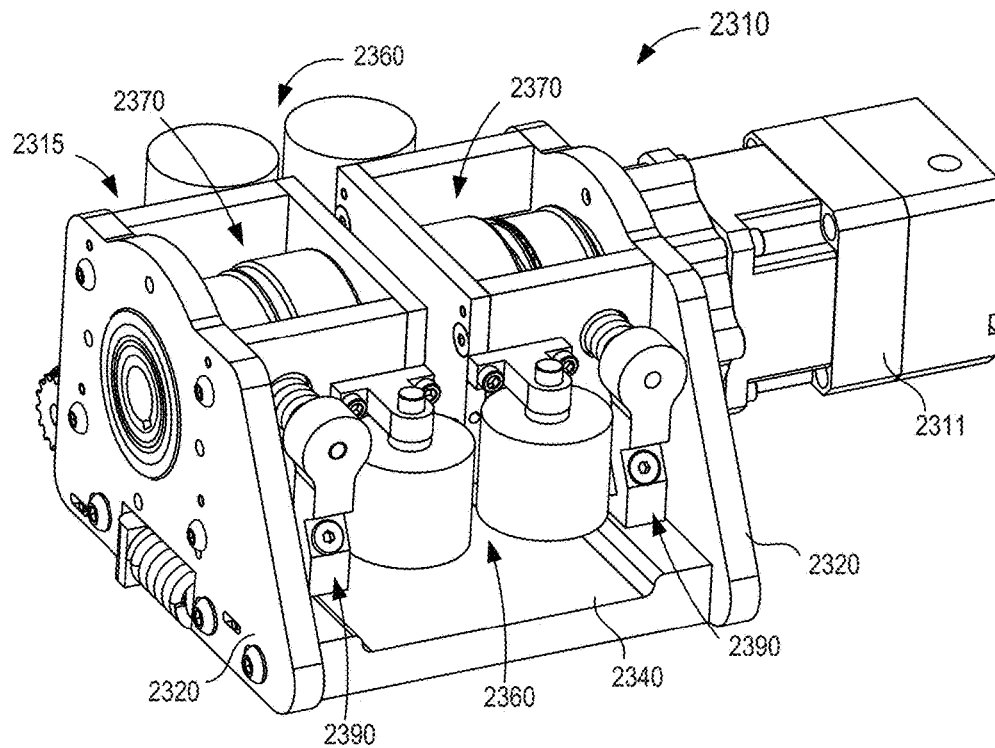


FIG. 13

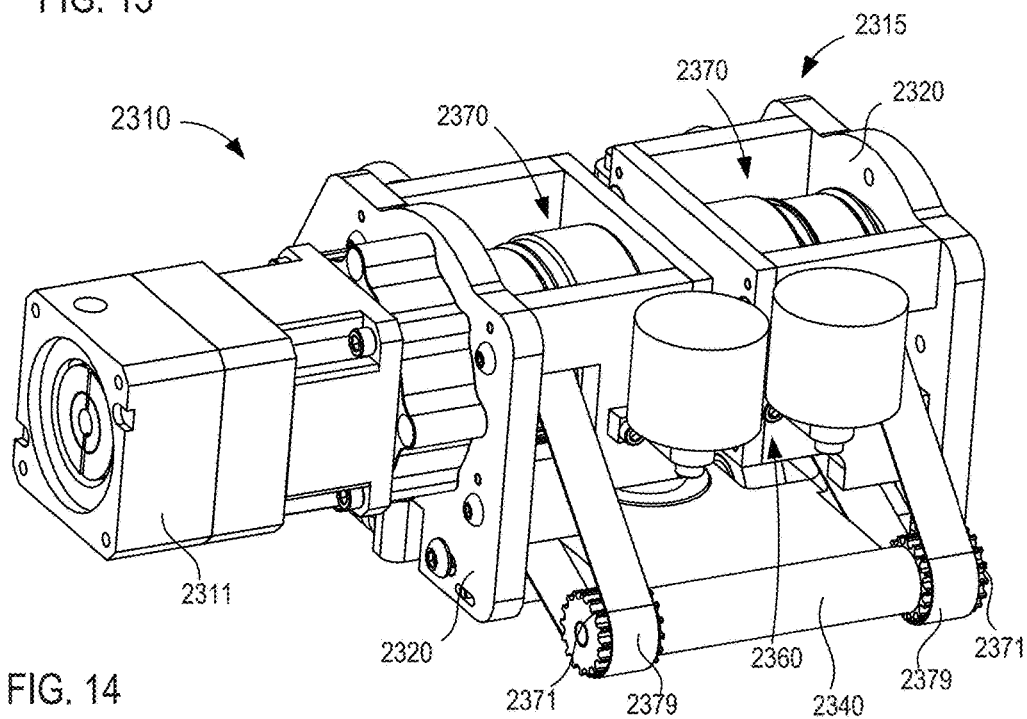
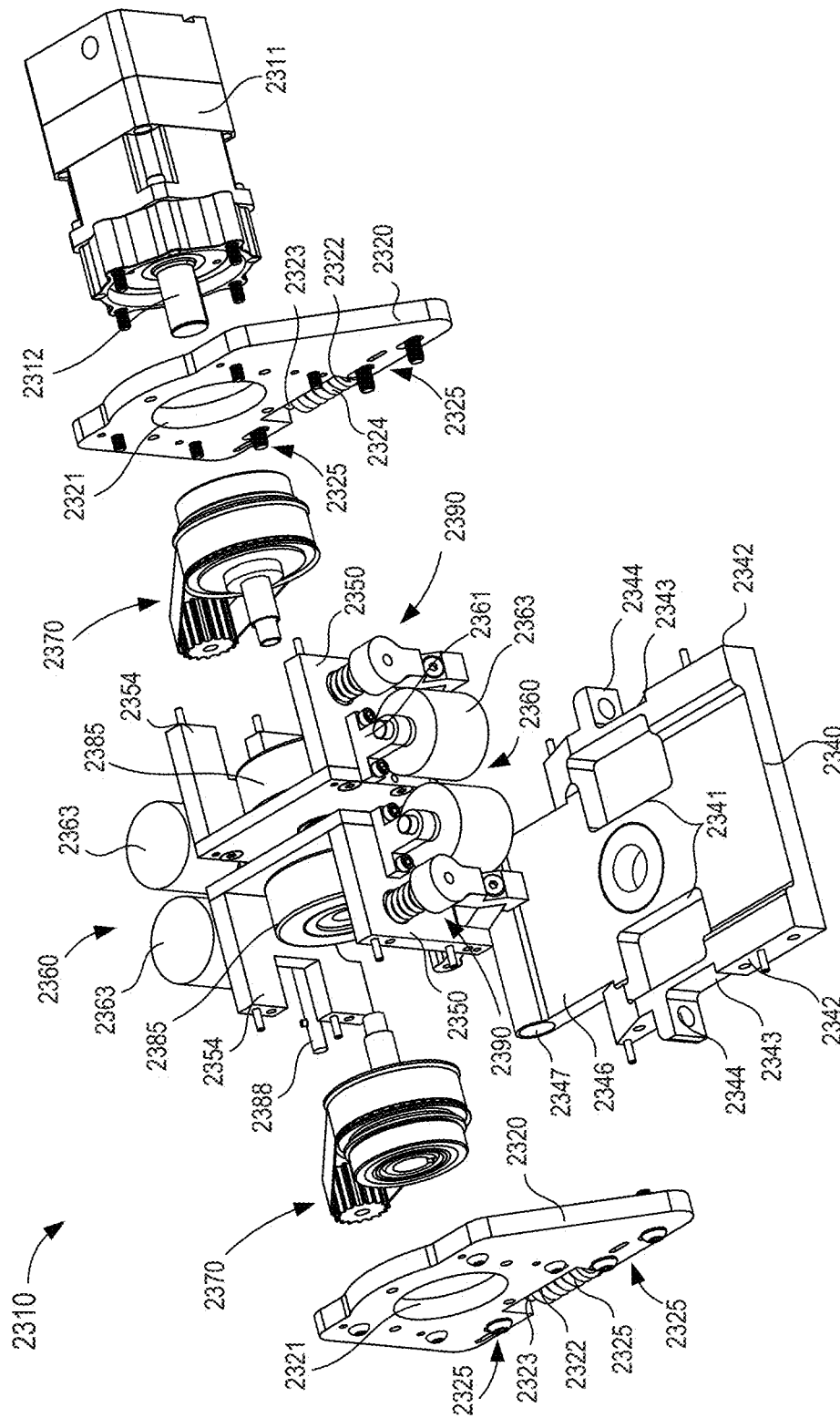
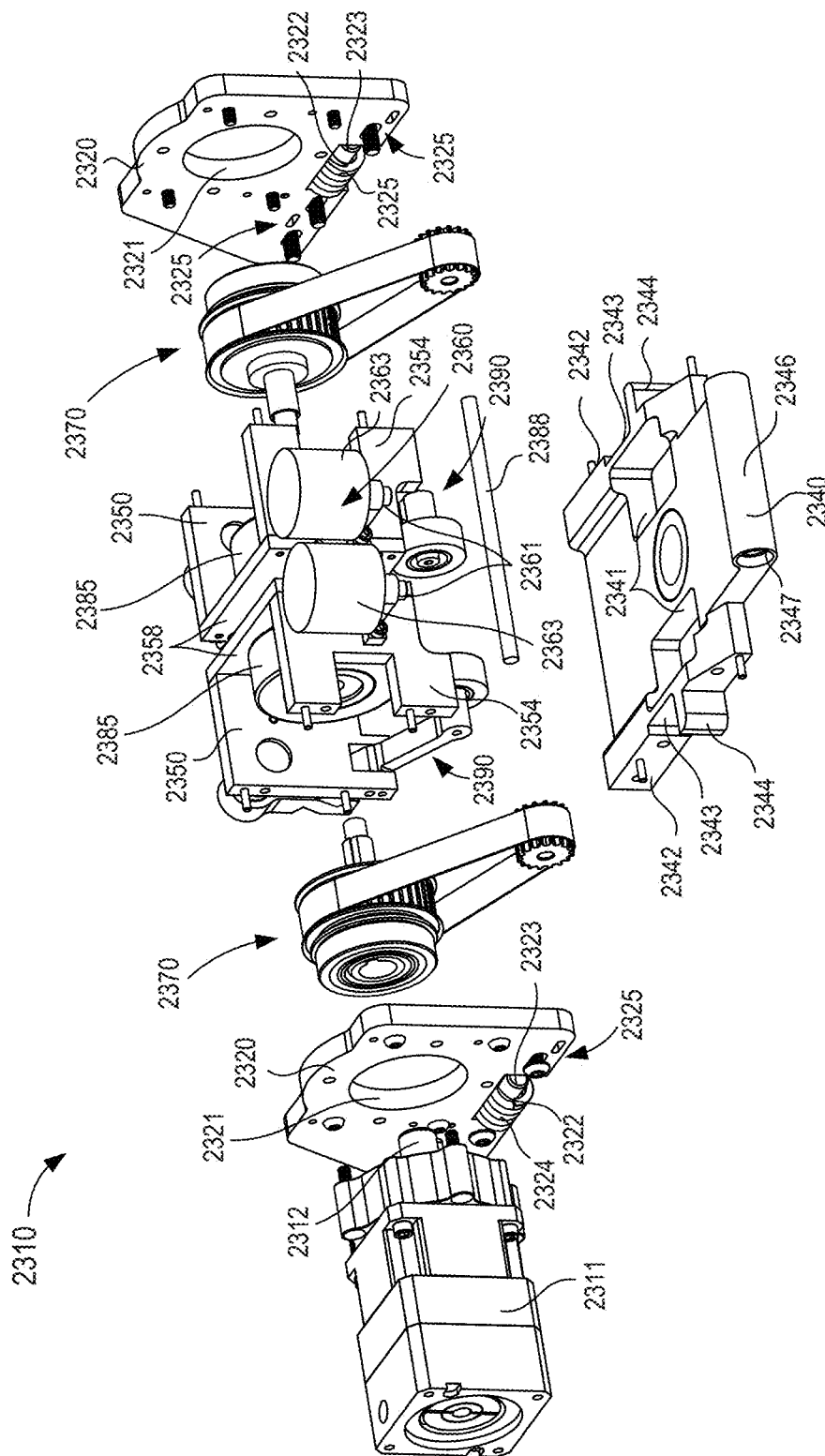


FIG. 14



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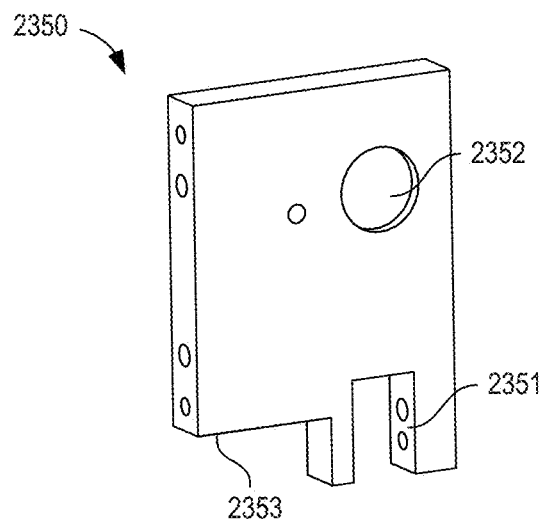


FIG. 17

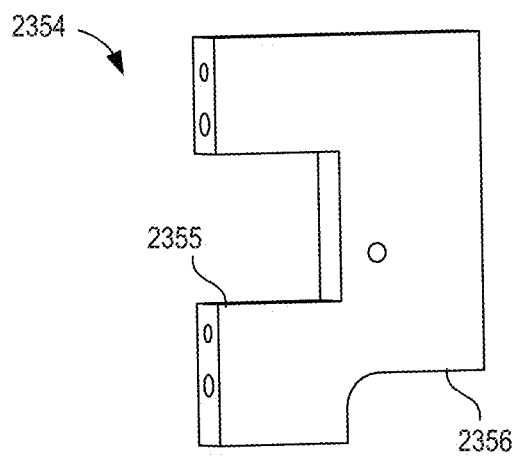


FIG. 18

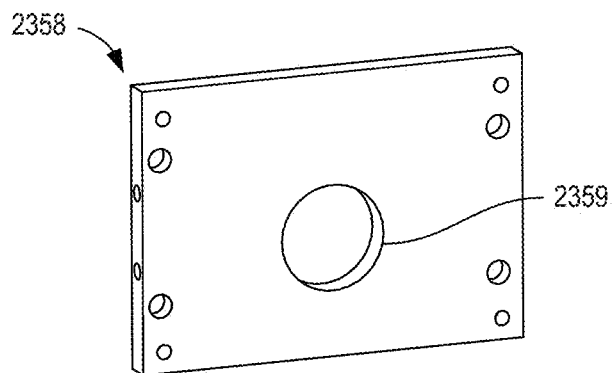


FIG. 19

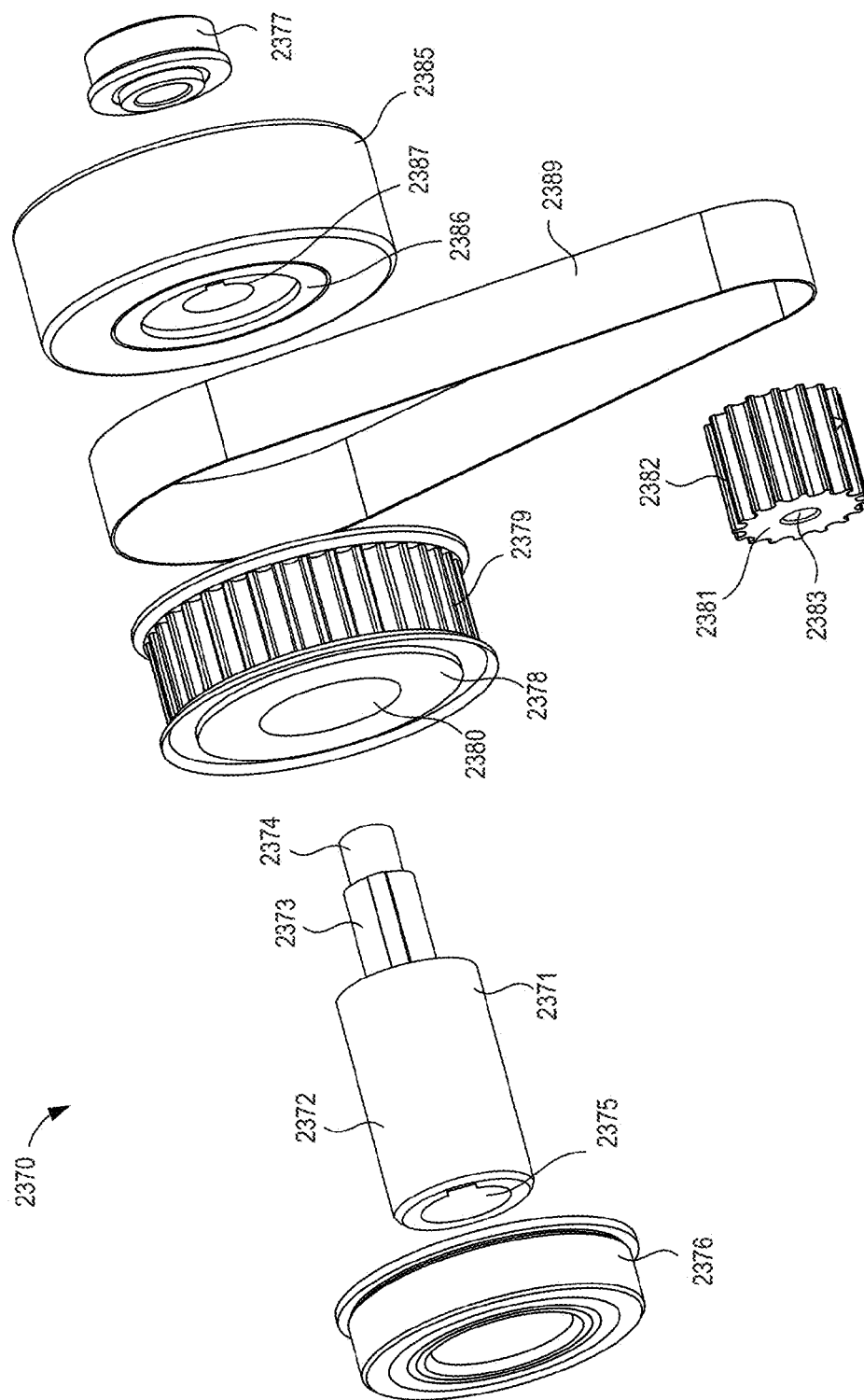


FIG. 20

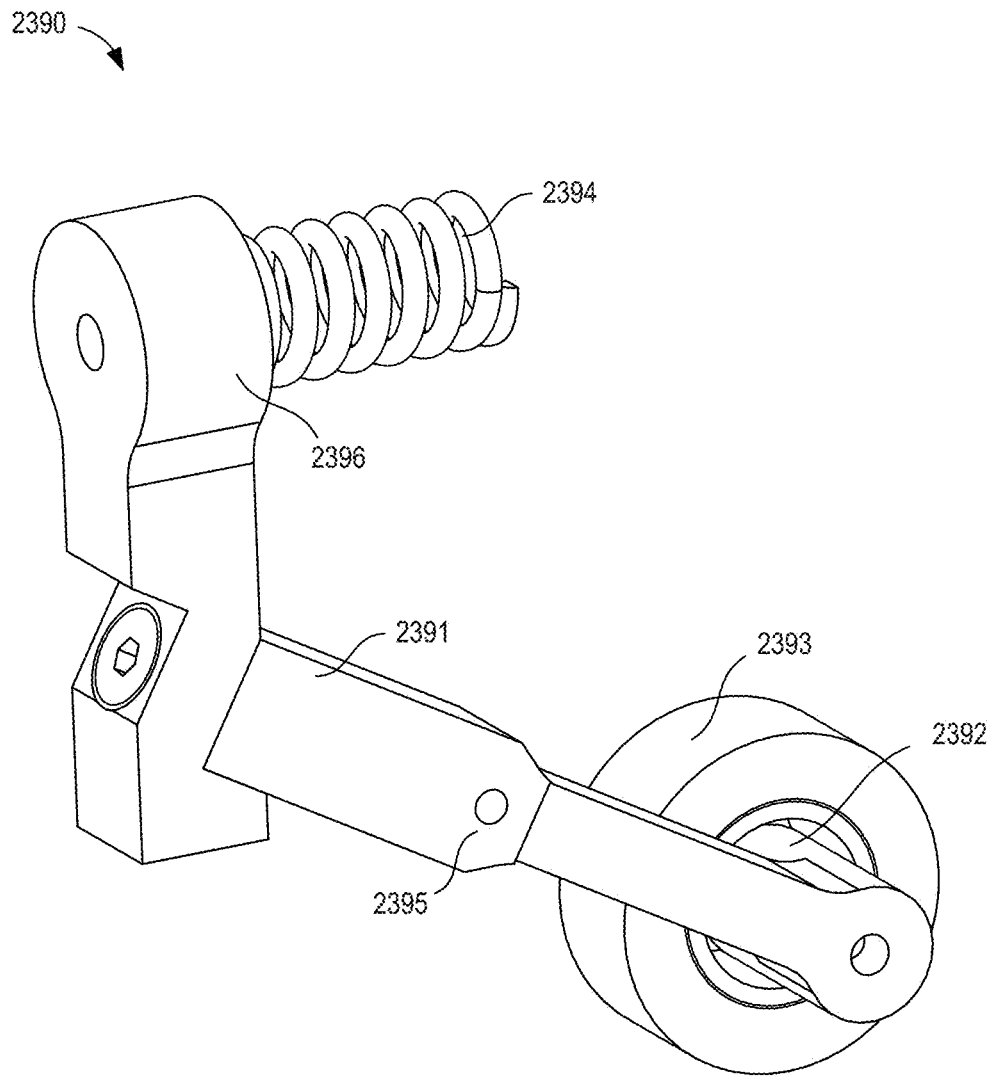


FIG. 21

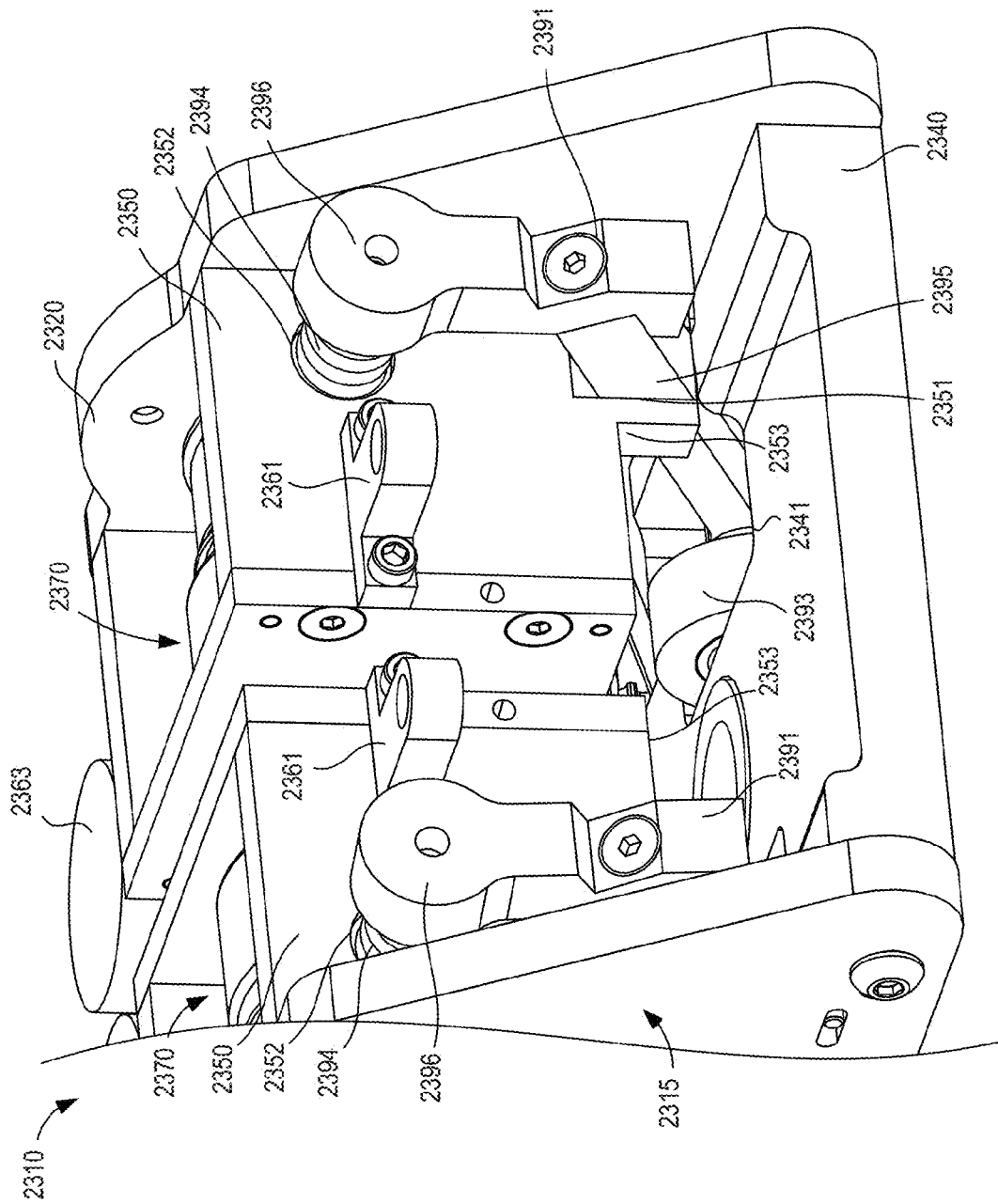


FIG. 22

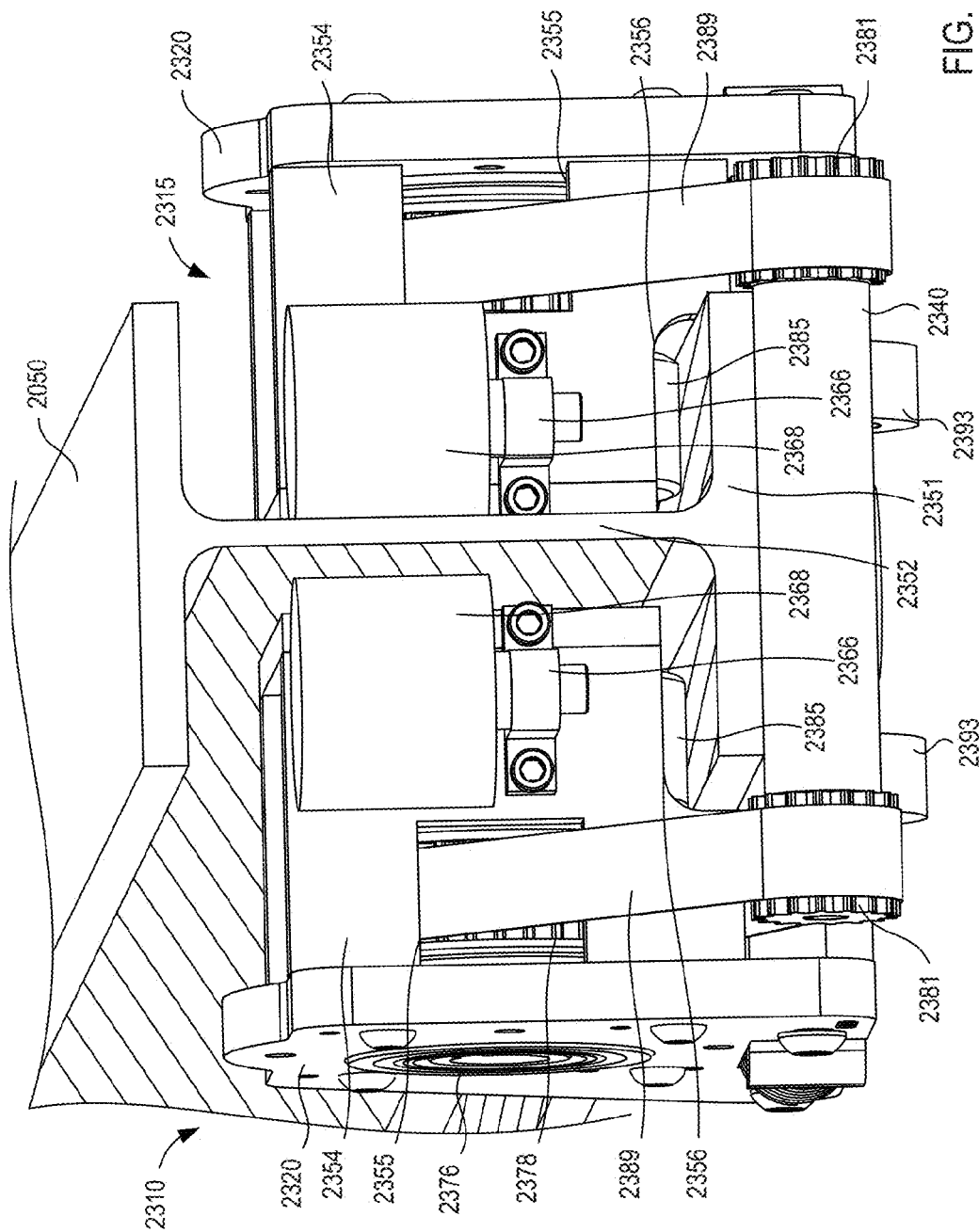


FIG. 23

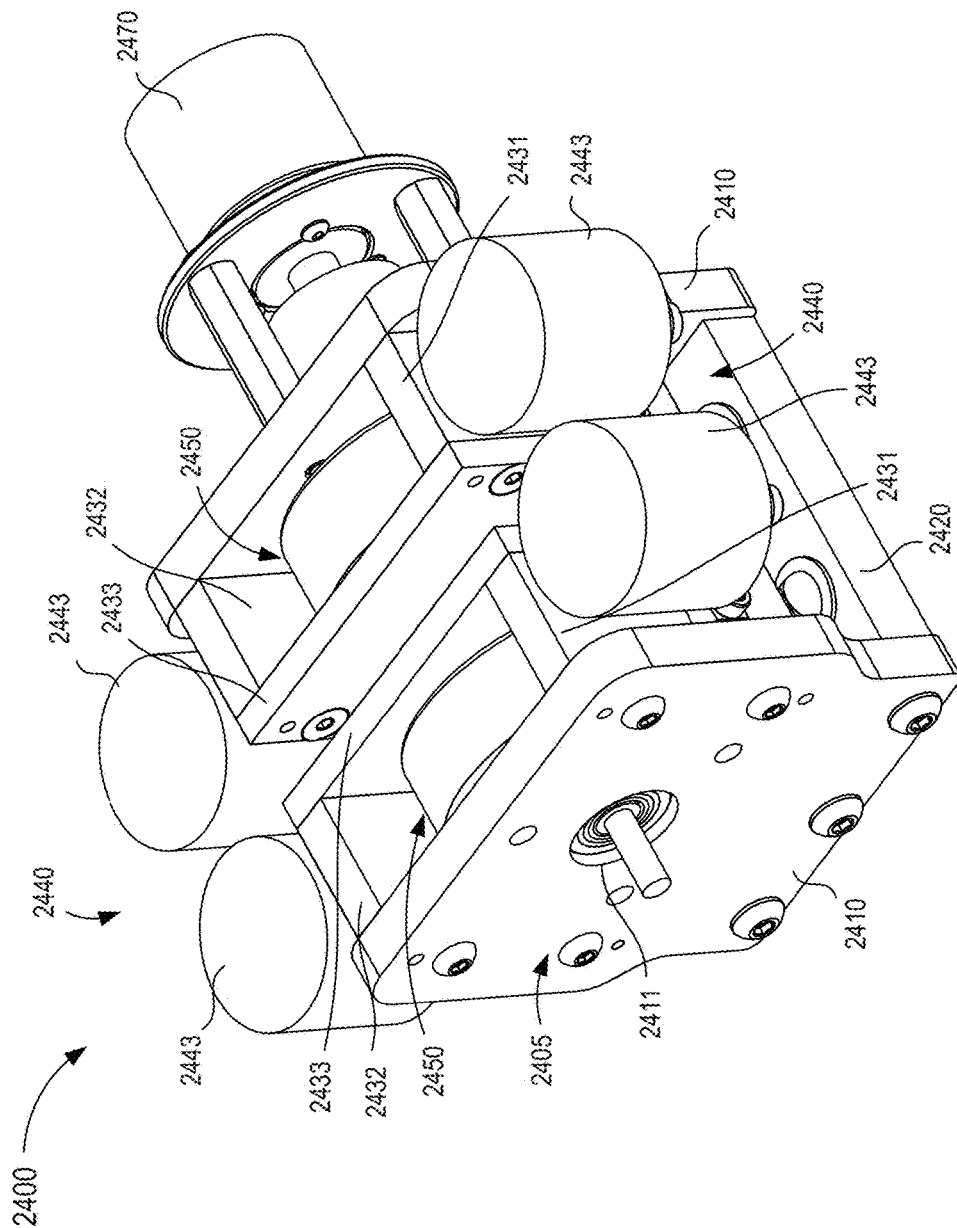


FIG. 24

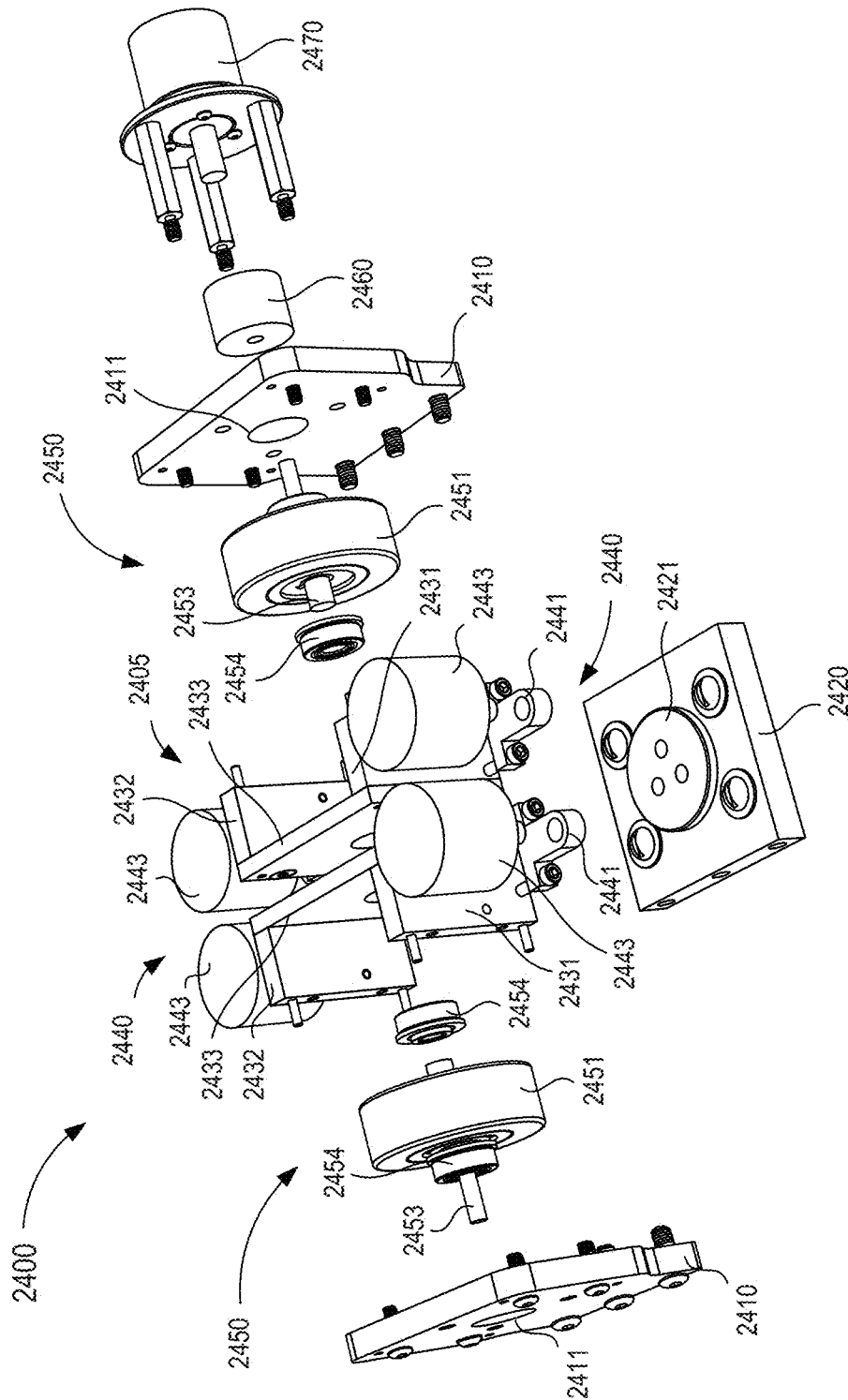


FIG. 25

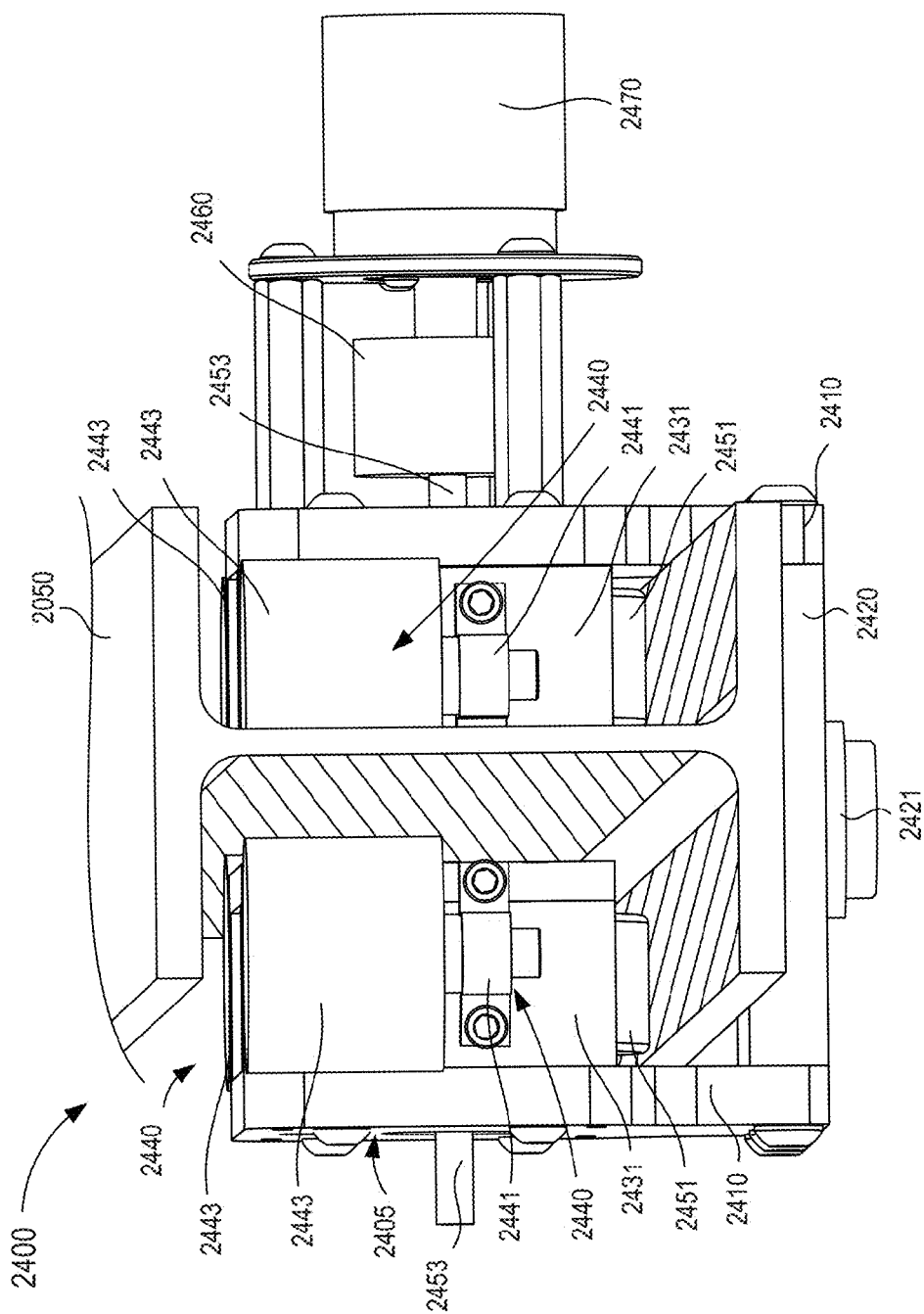
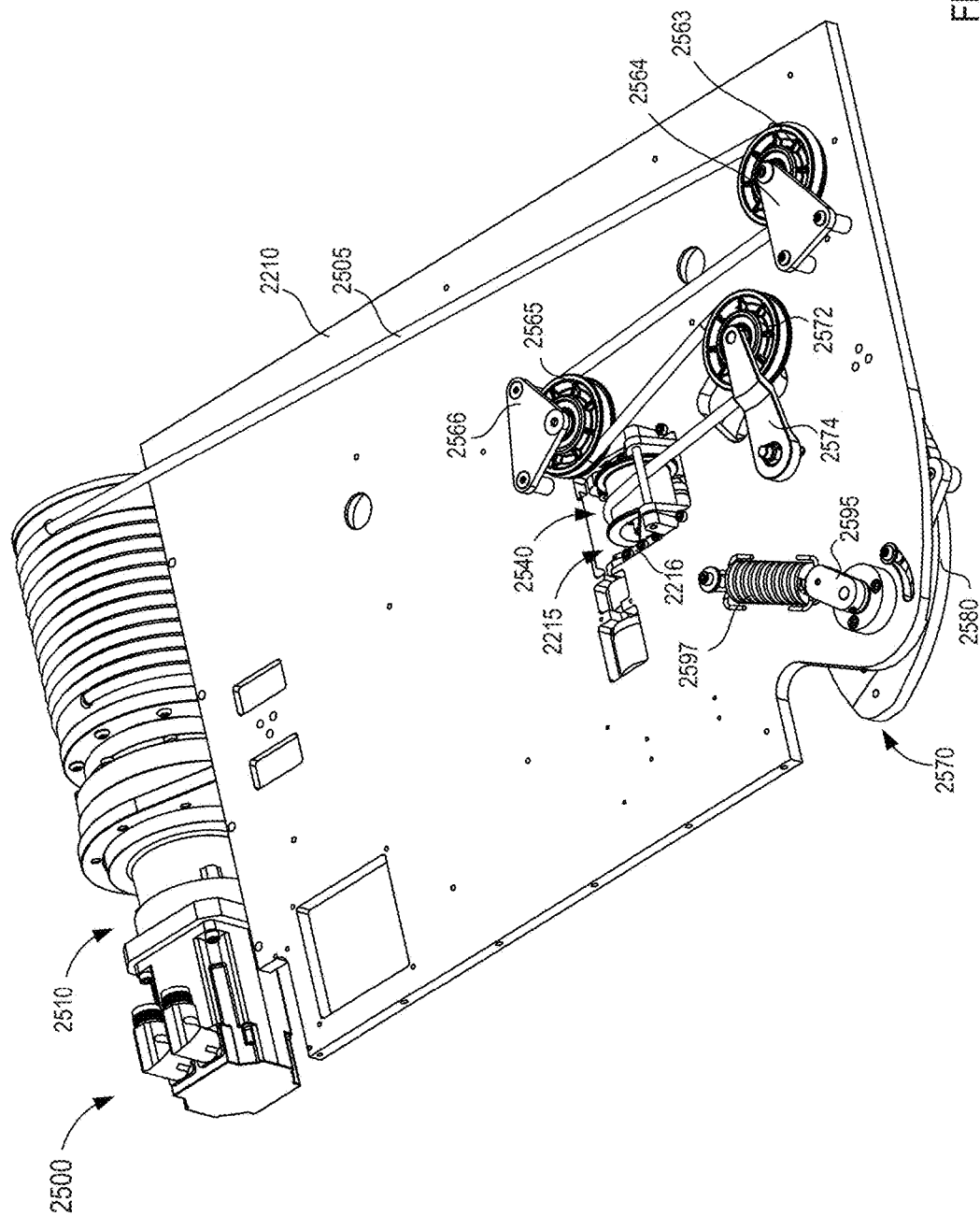
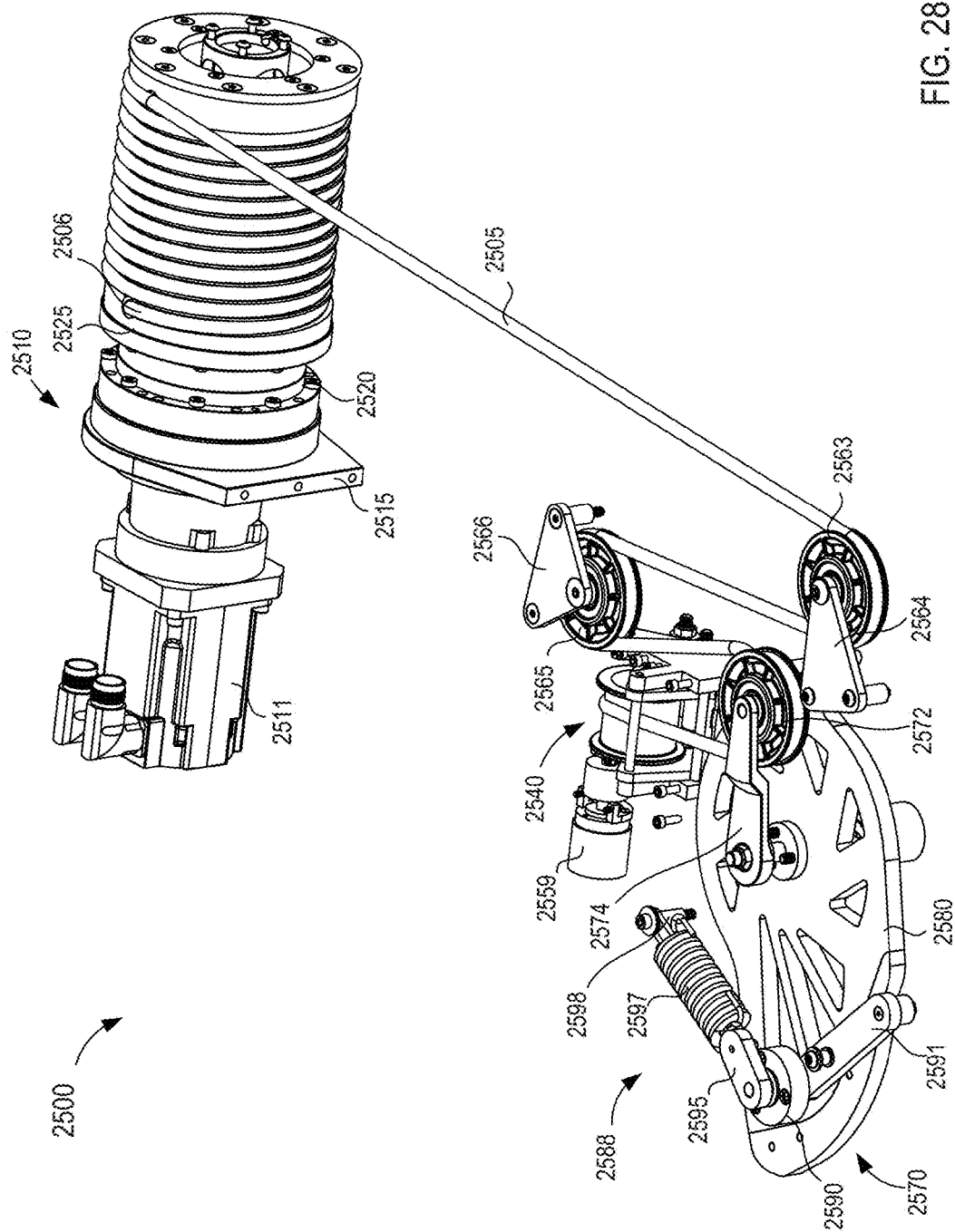


FIG. 26





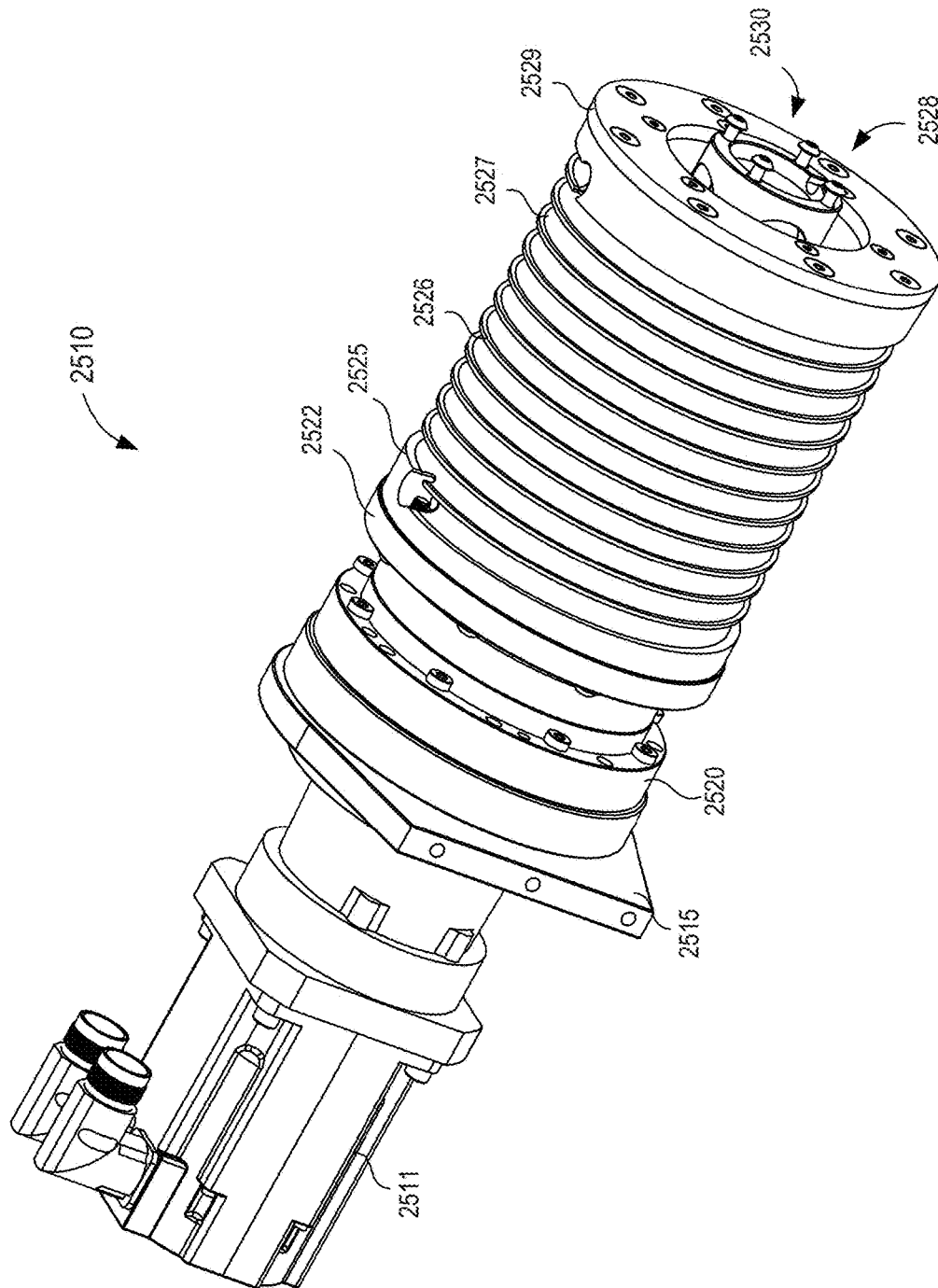


FIG. 29

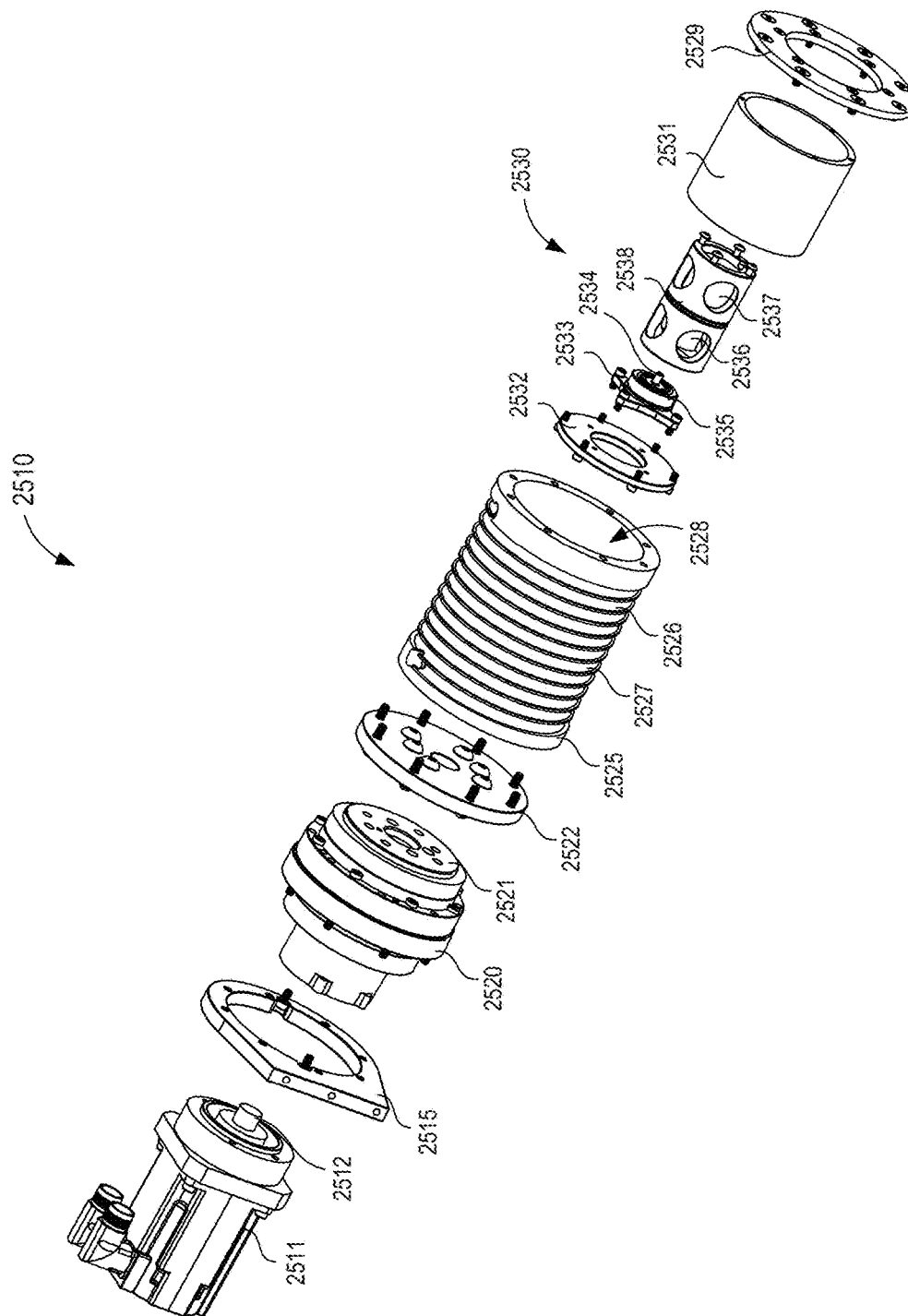
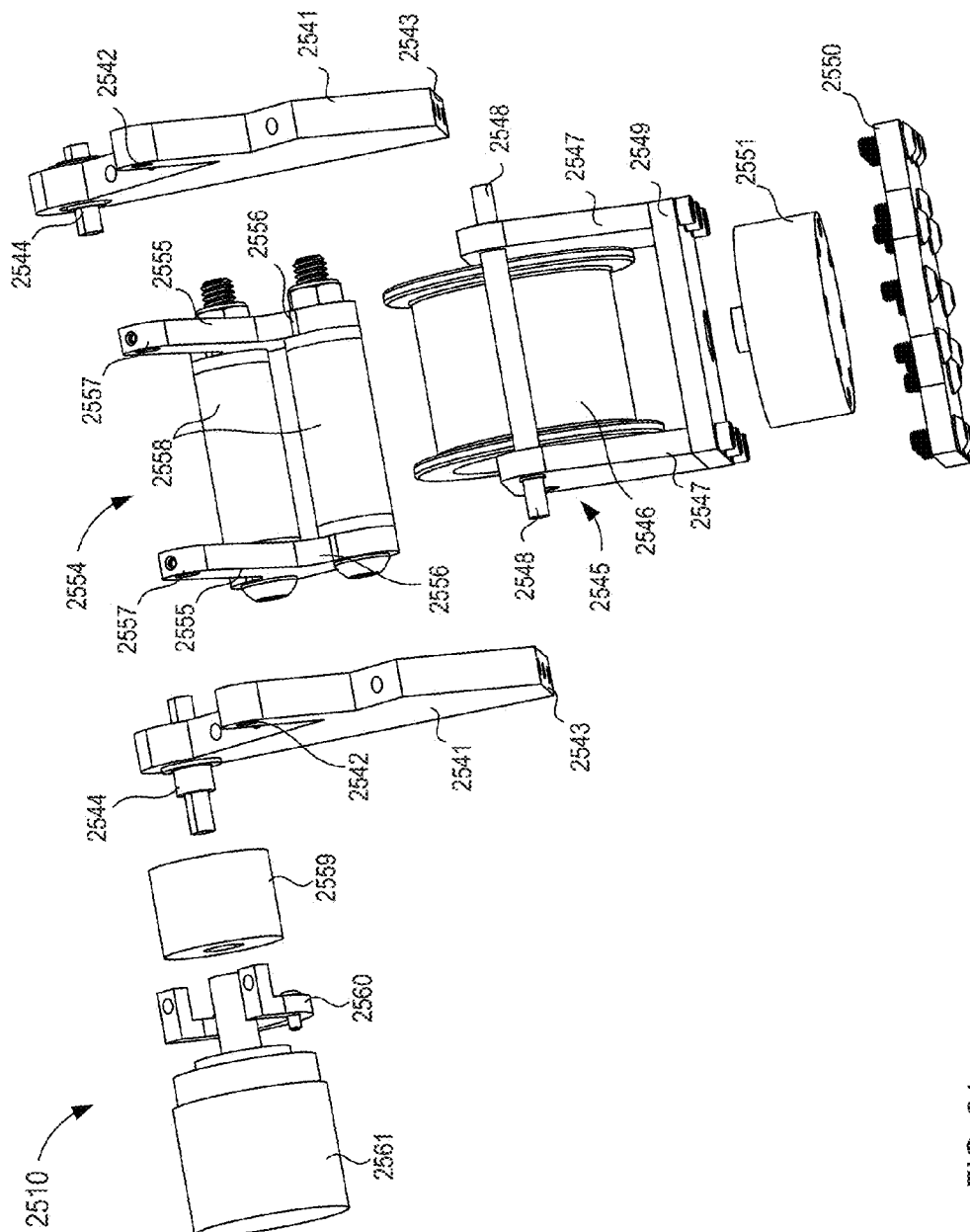


FIG. 30



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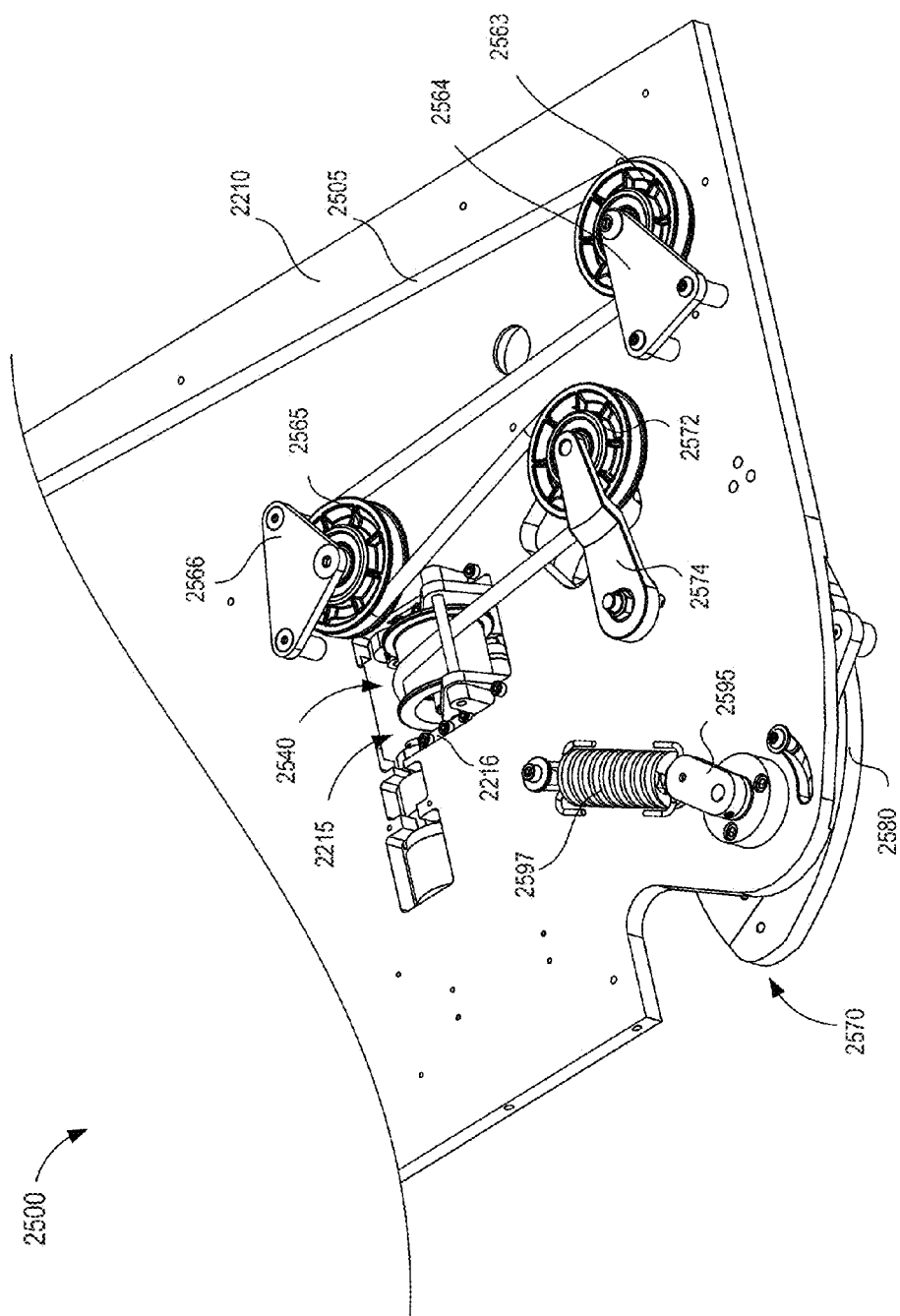


FIG. 32

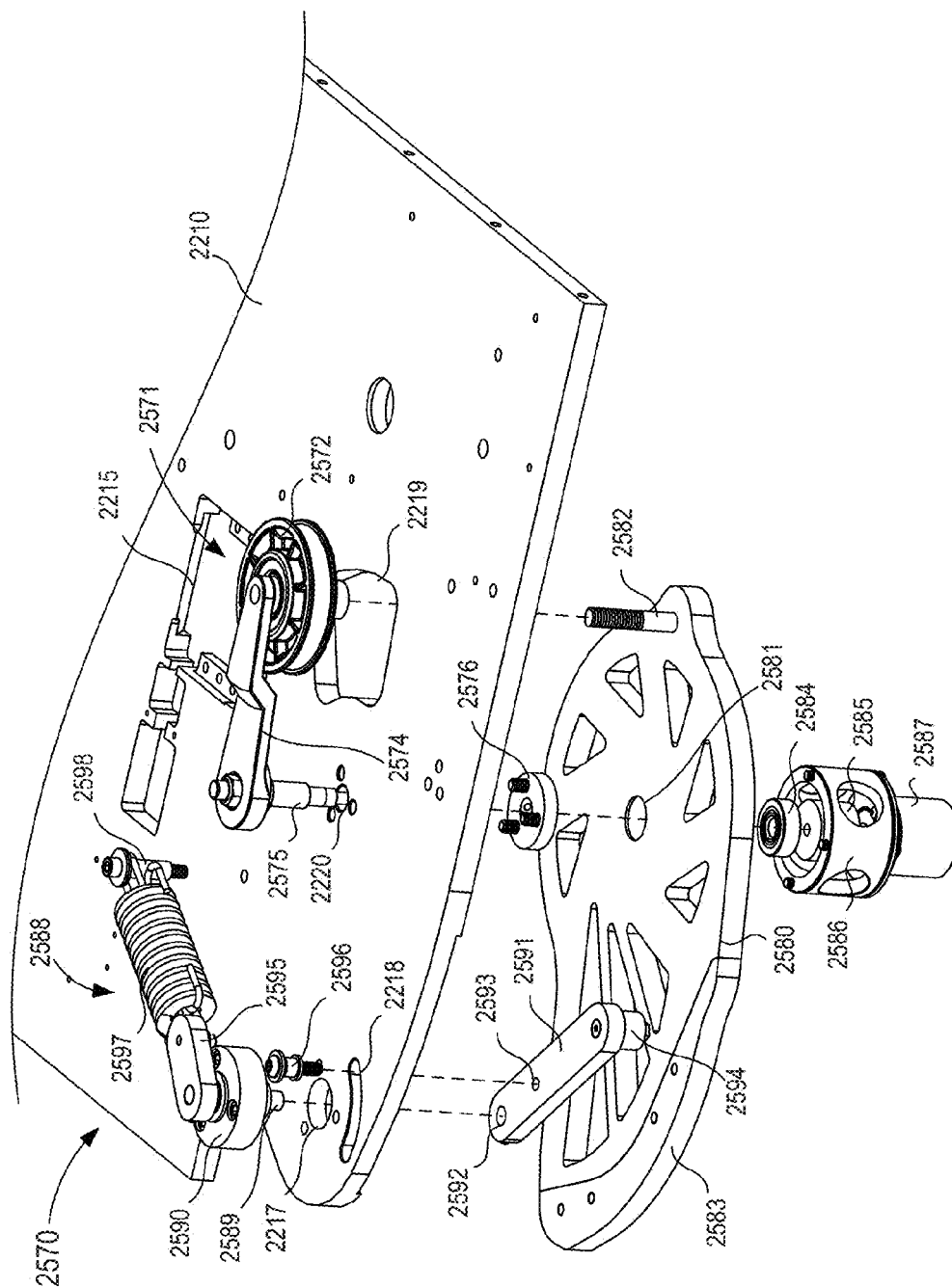


FIG. 33

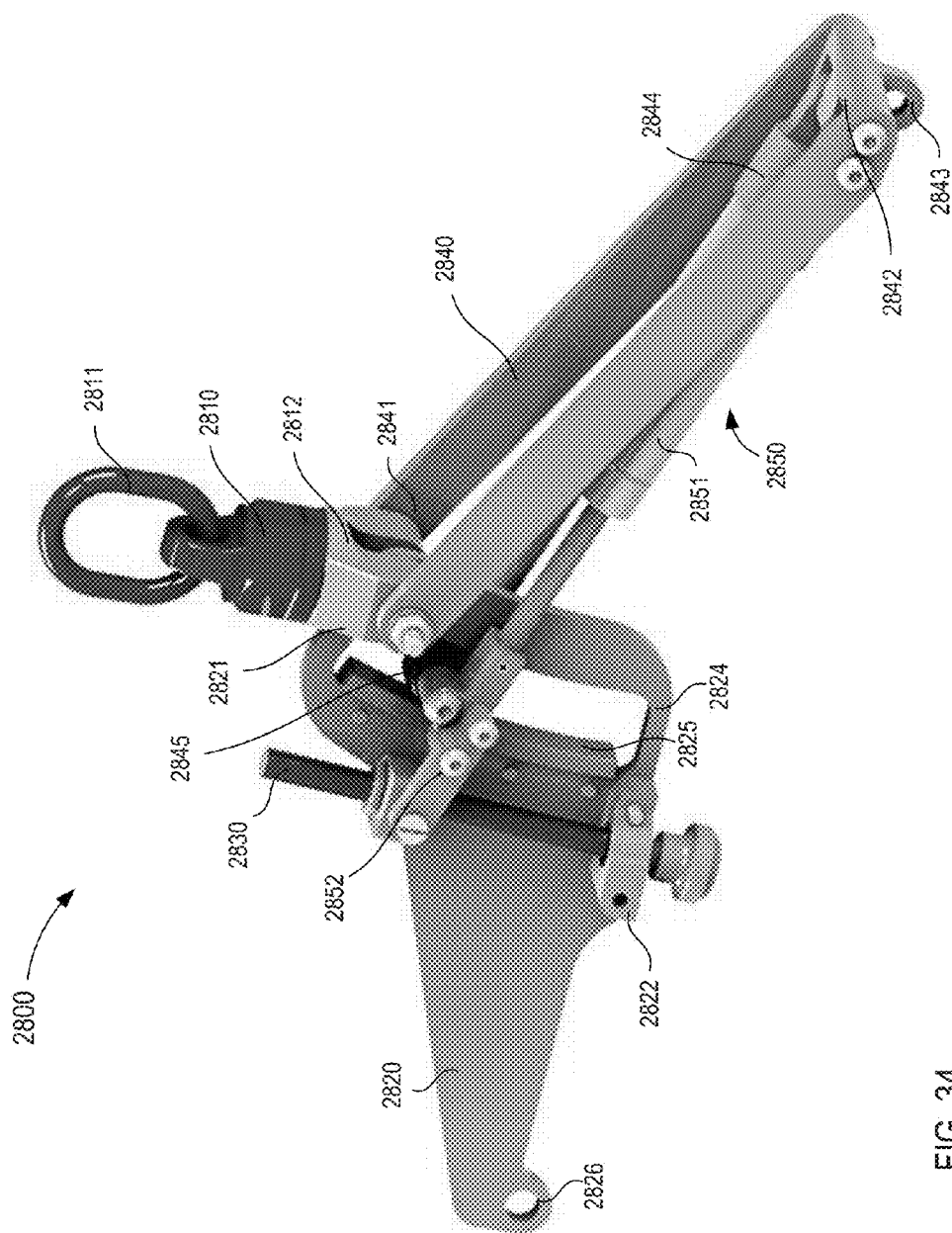


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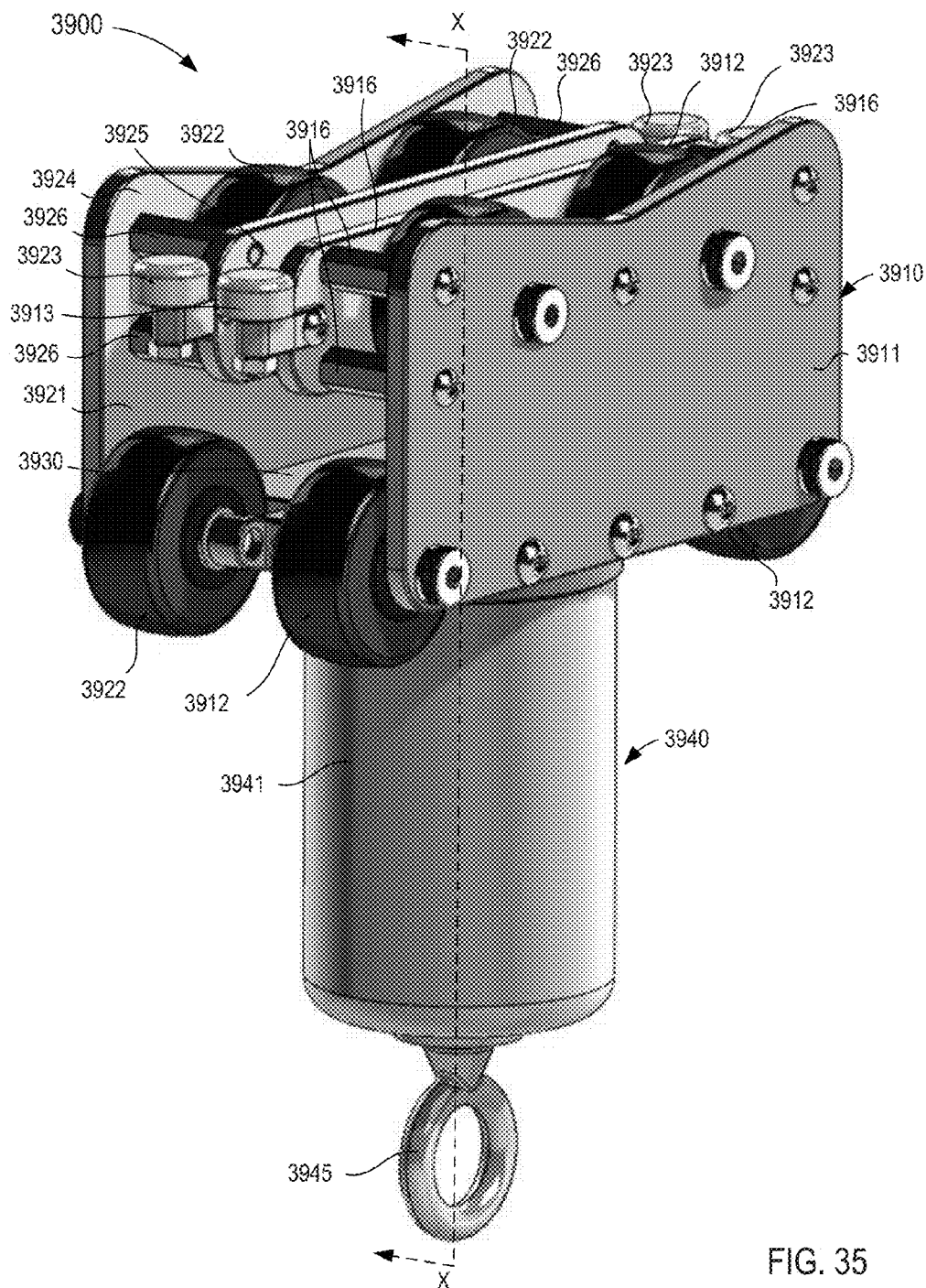


FIG. 35

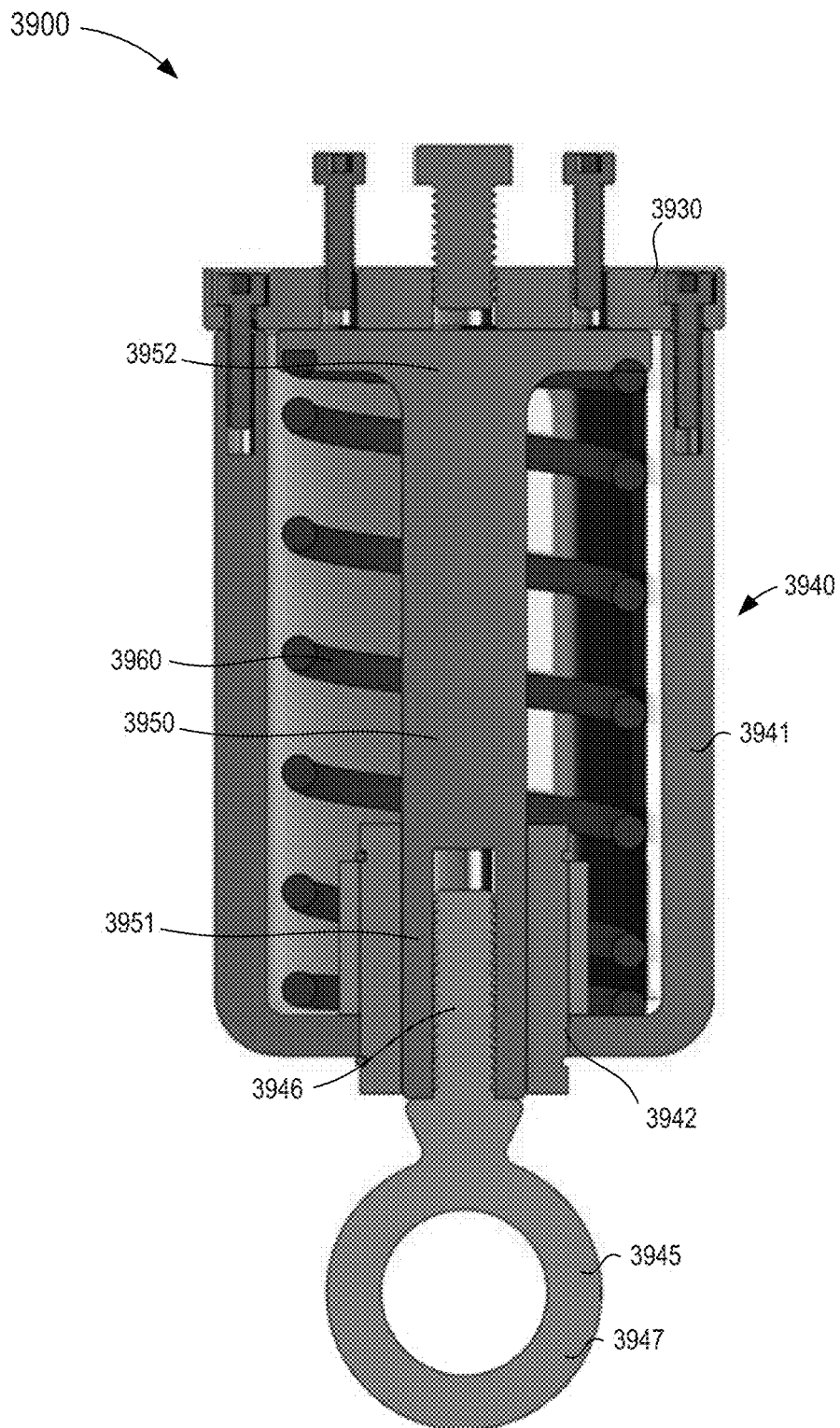


FIG. 36

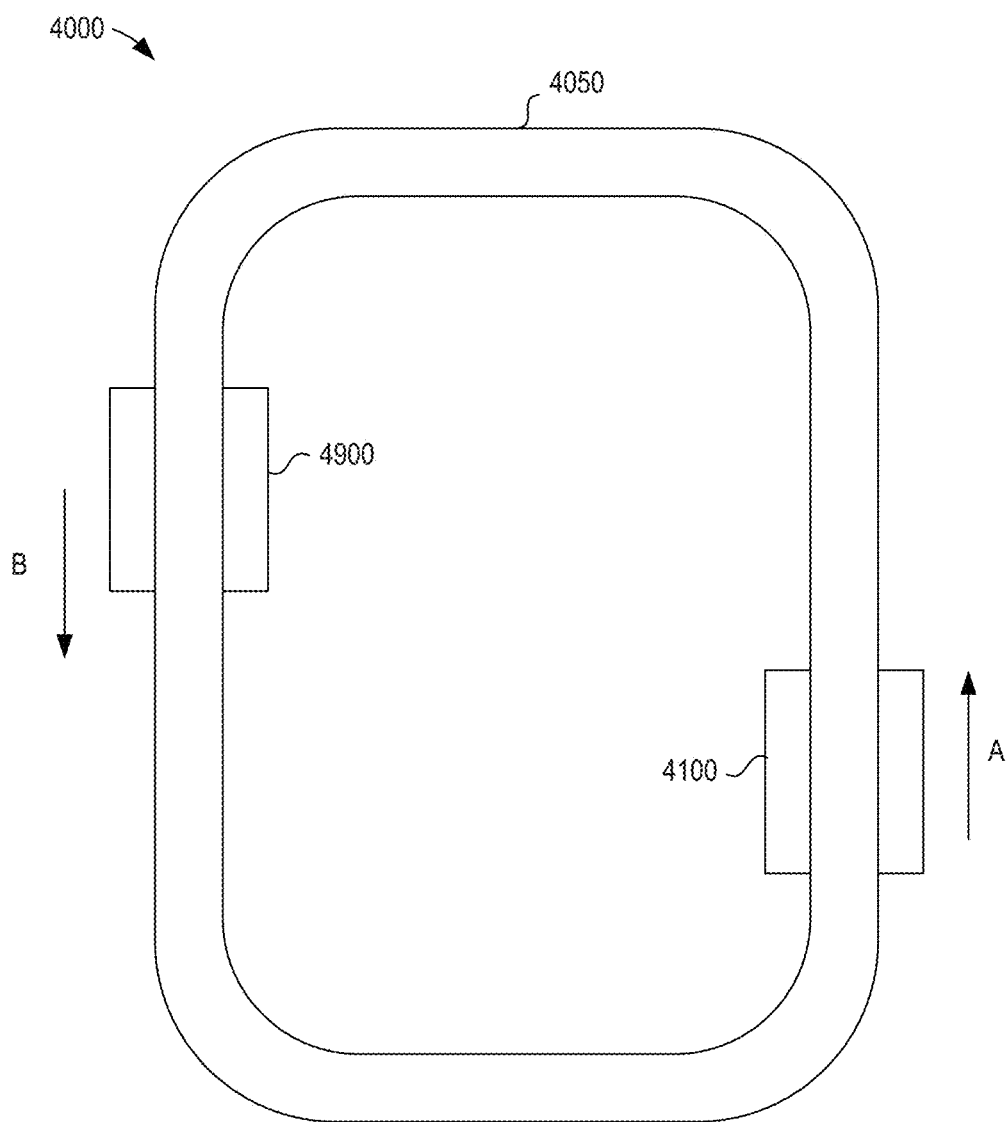
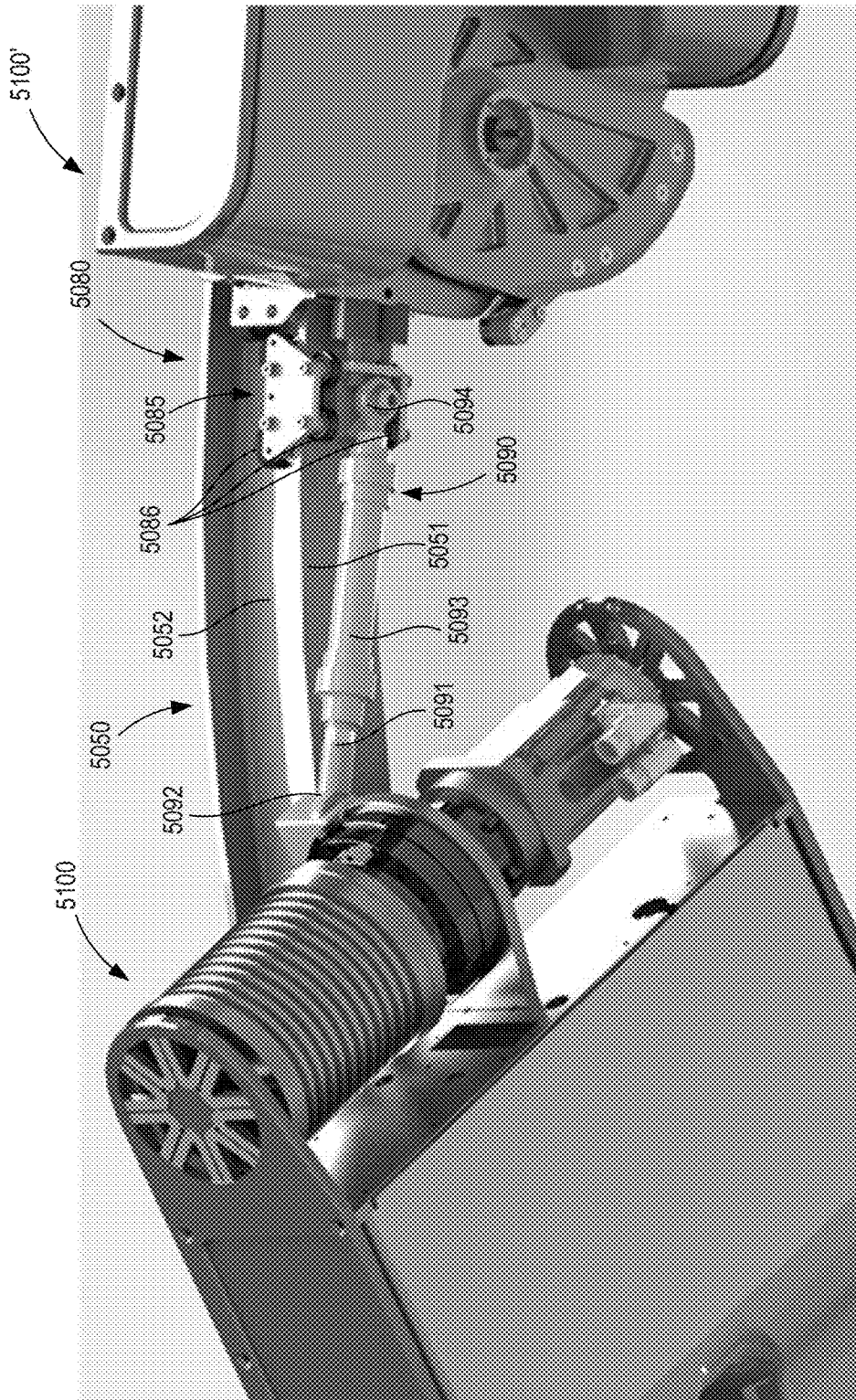


FIG. 37



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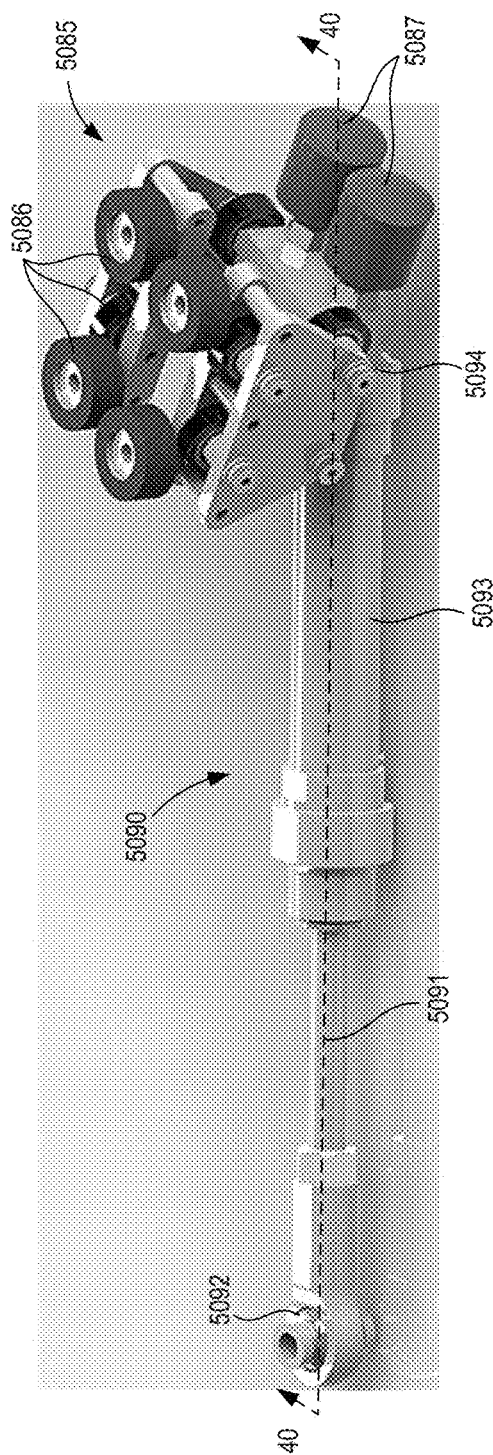


FIG. 39

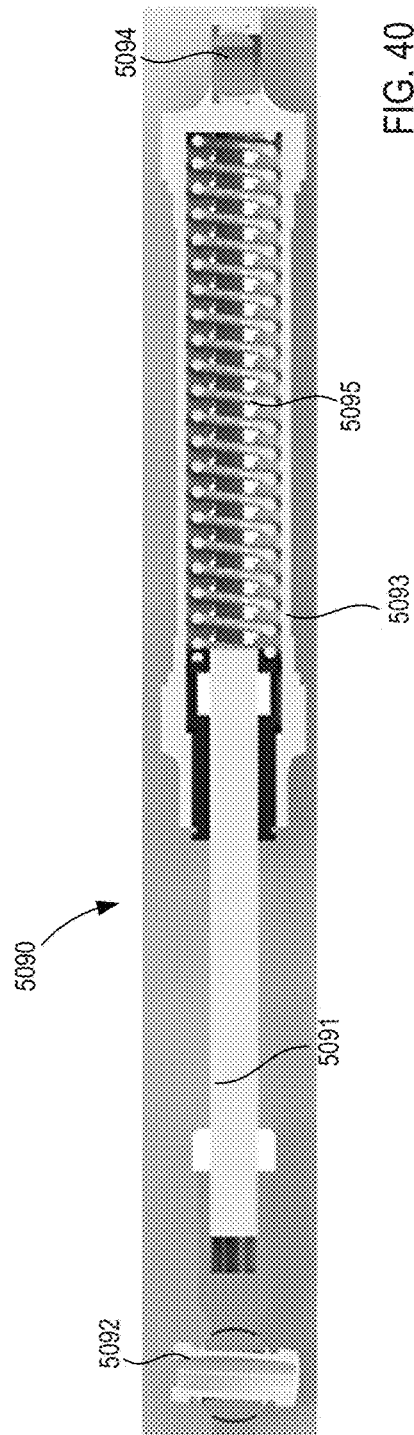


FIG. 40

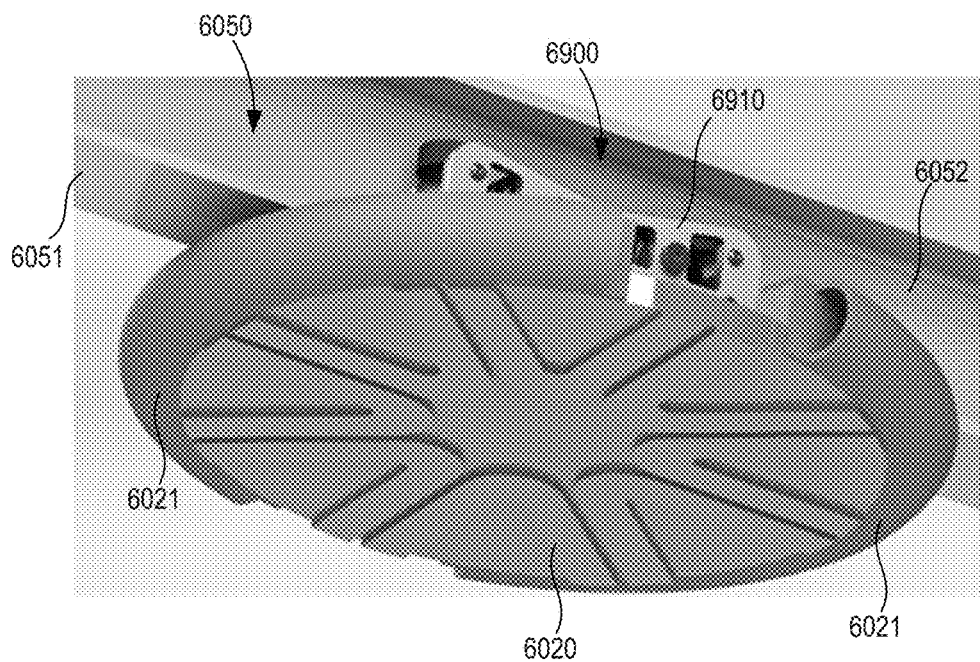


FIG. 41

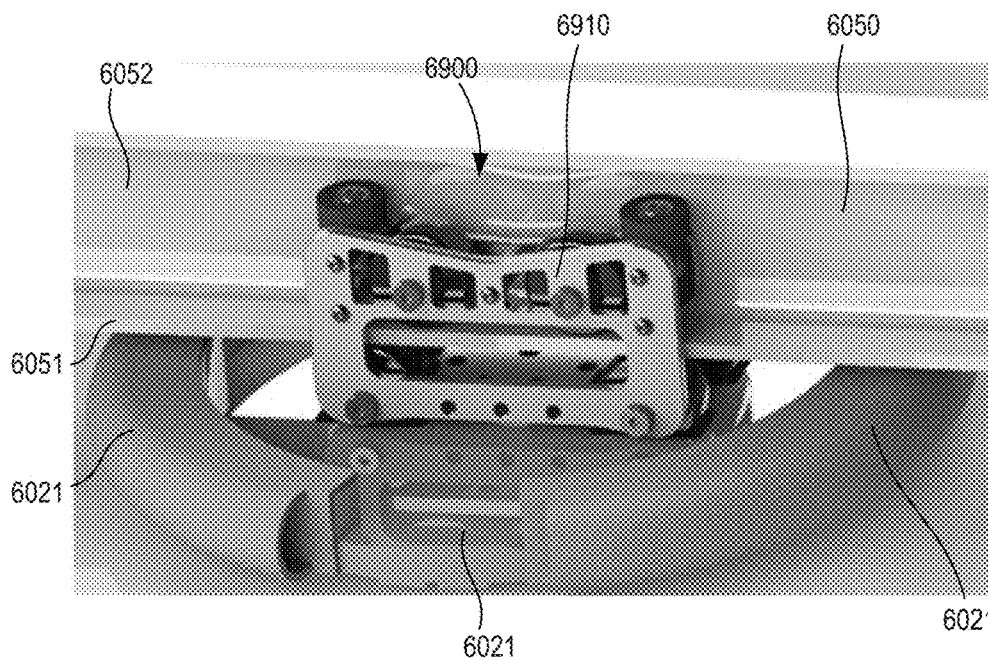


FIG. 42

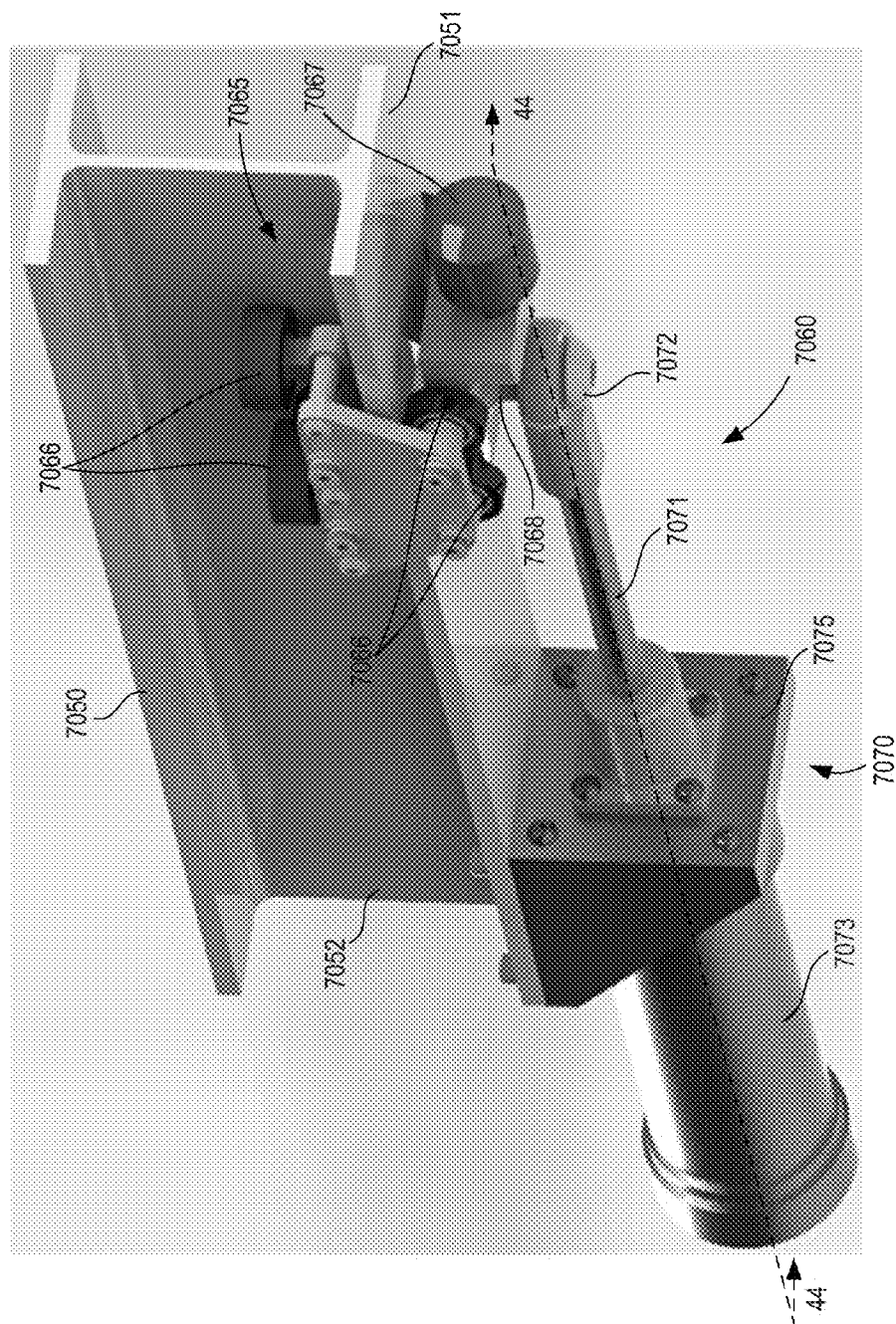


FIG. 43

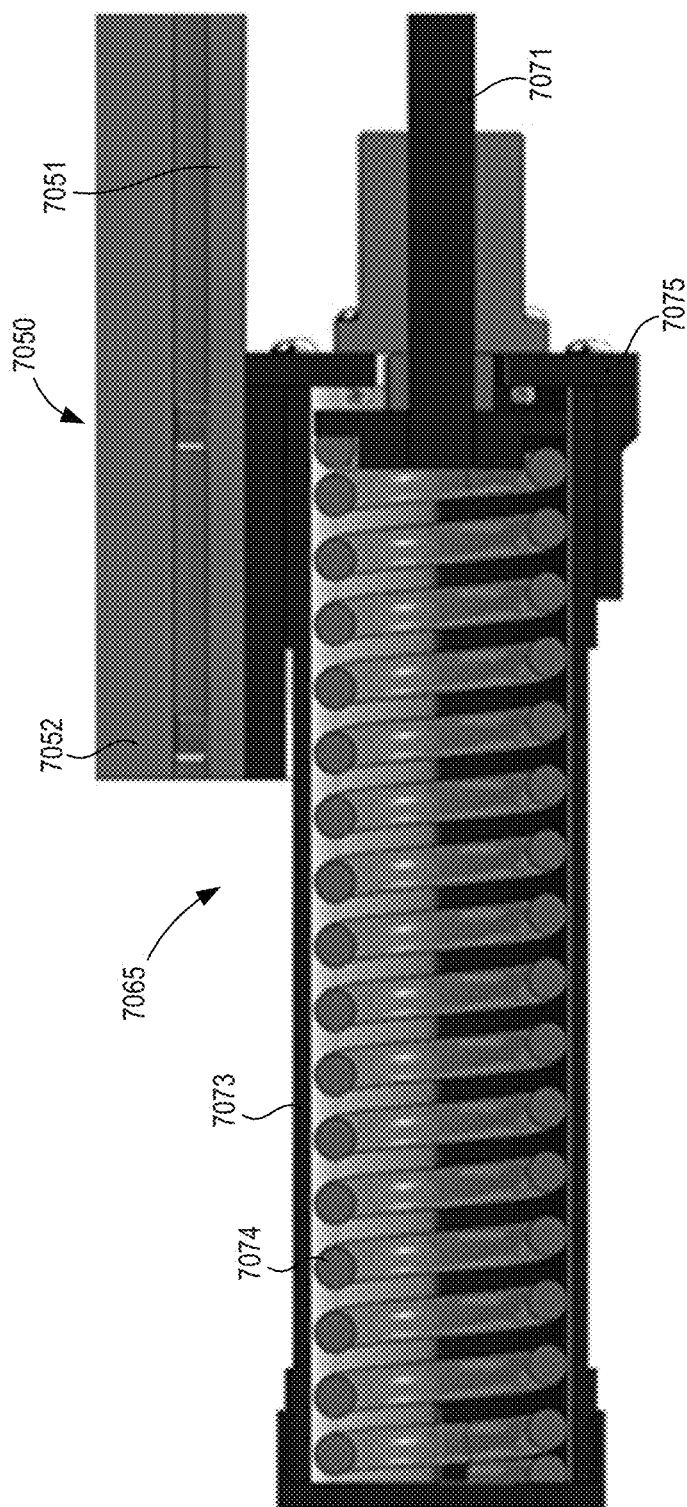


FIG. 44

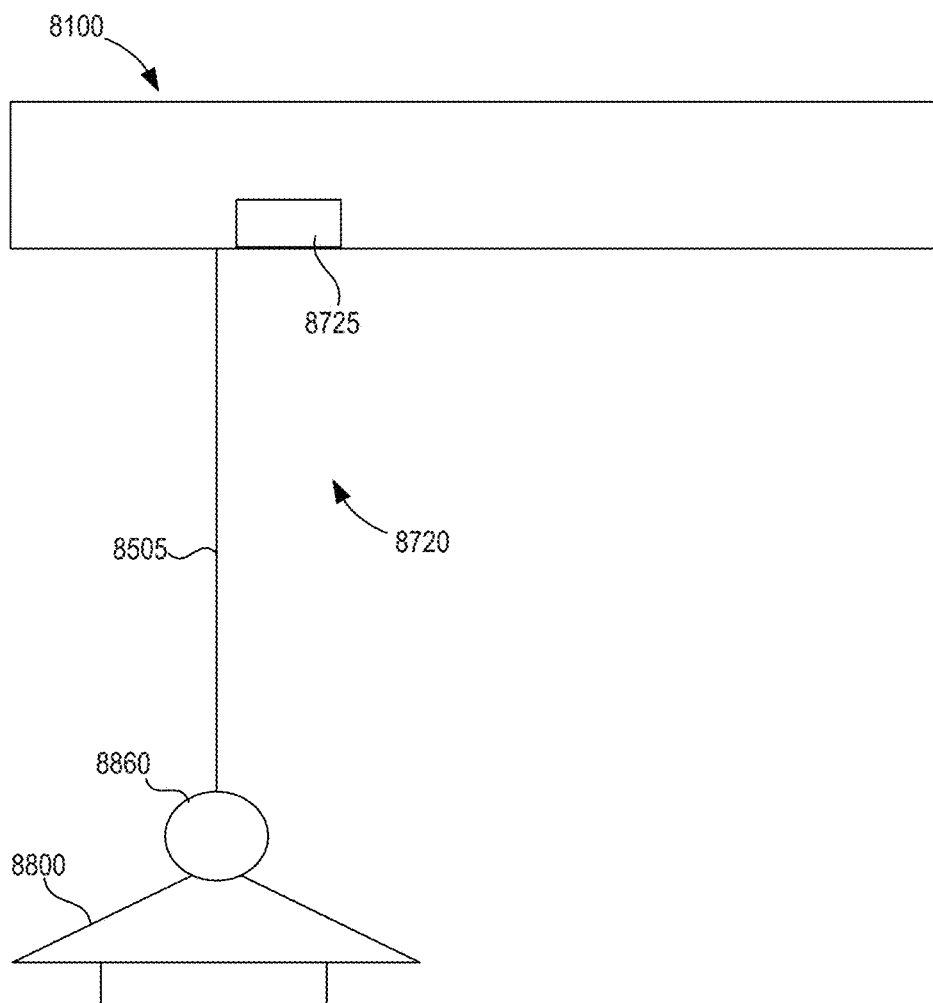


FIG. 45

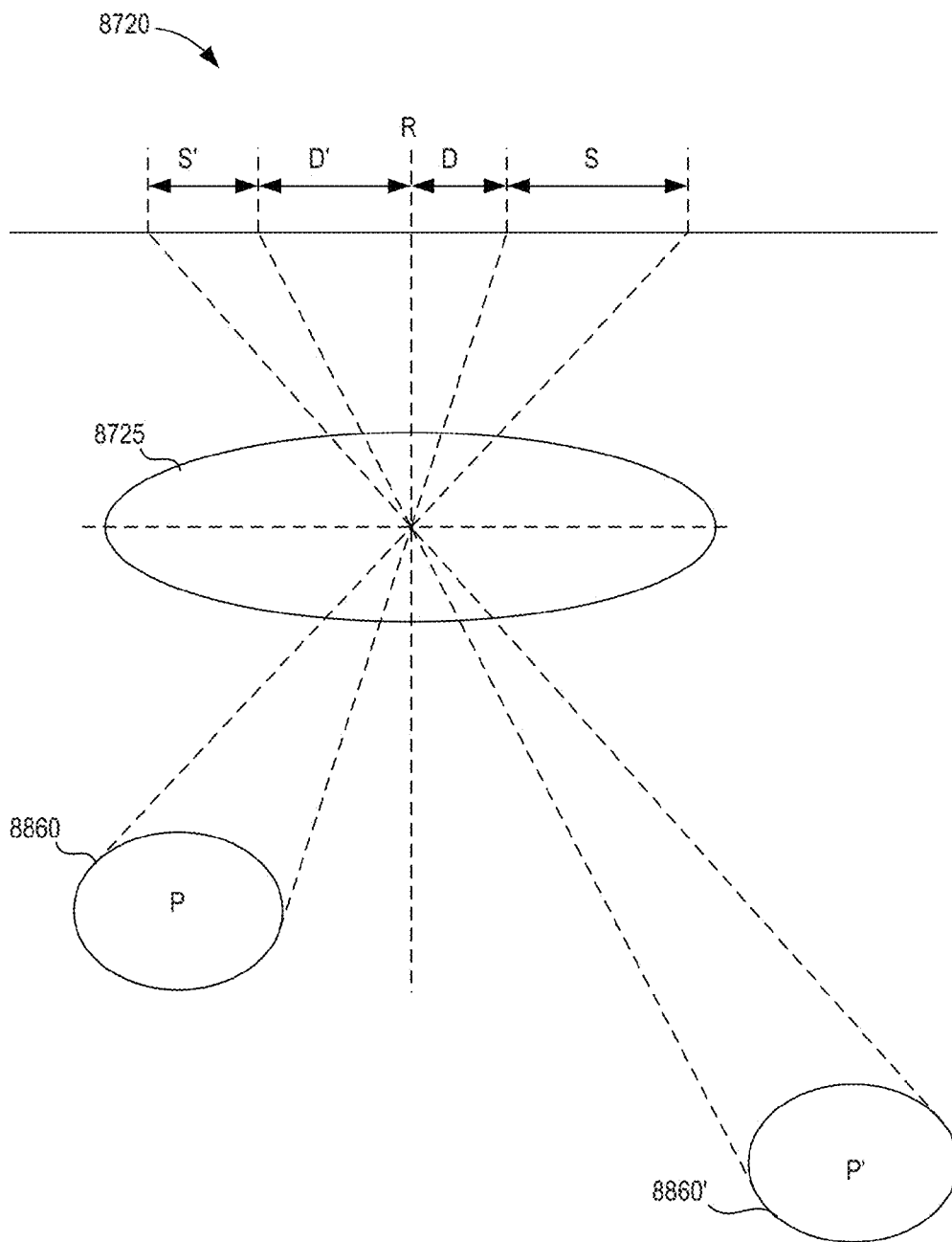


FIG. 46

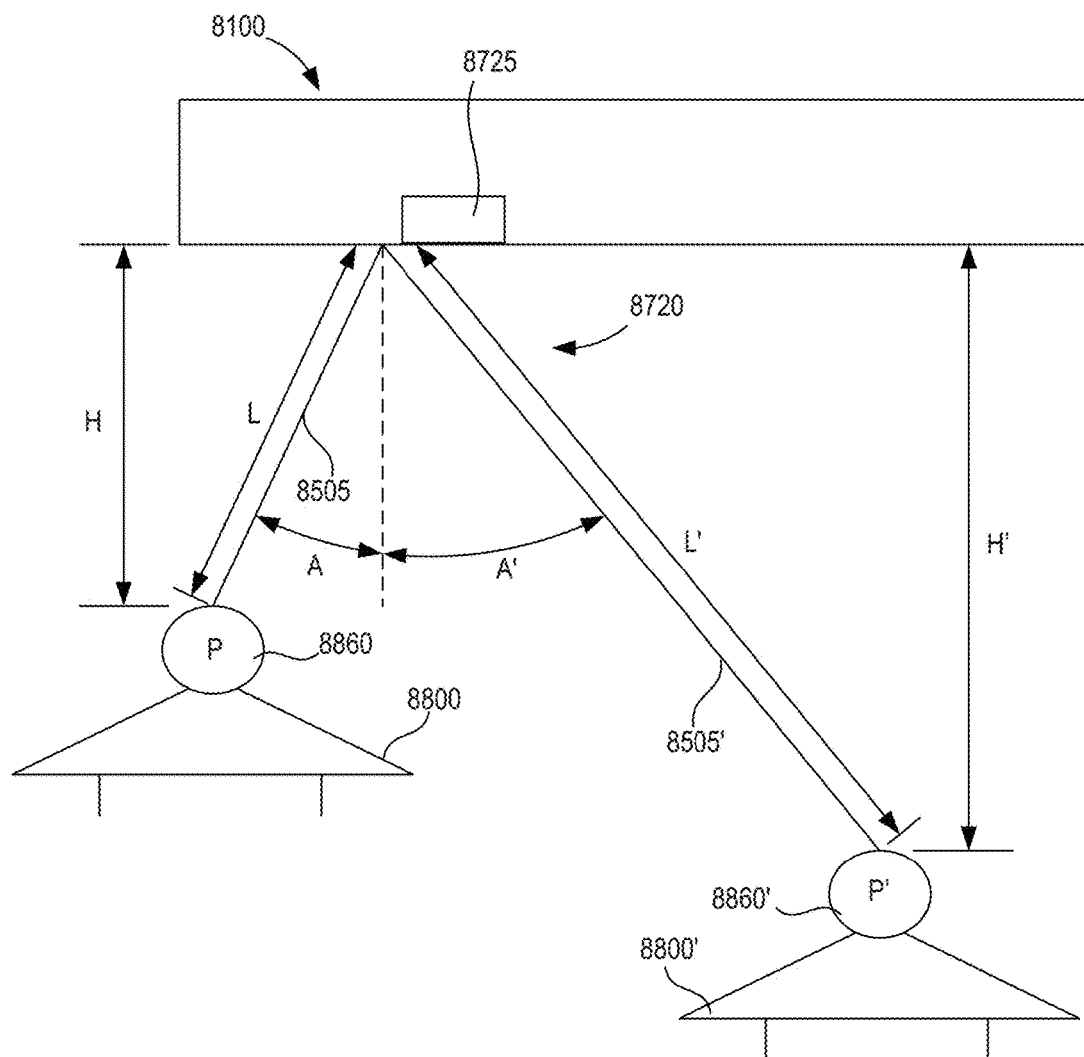


FIG. 47

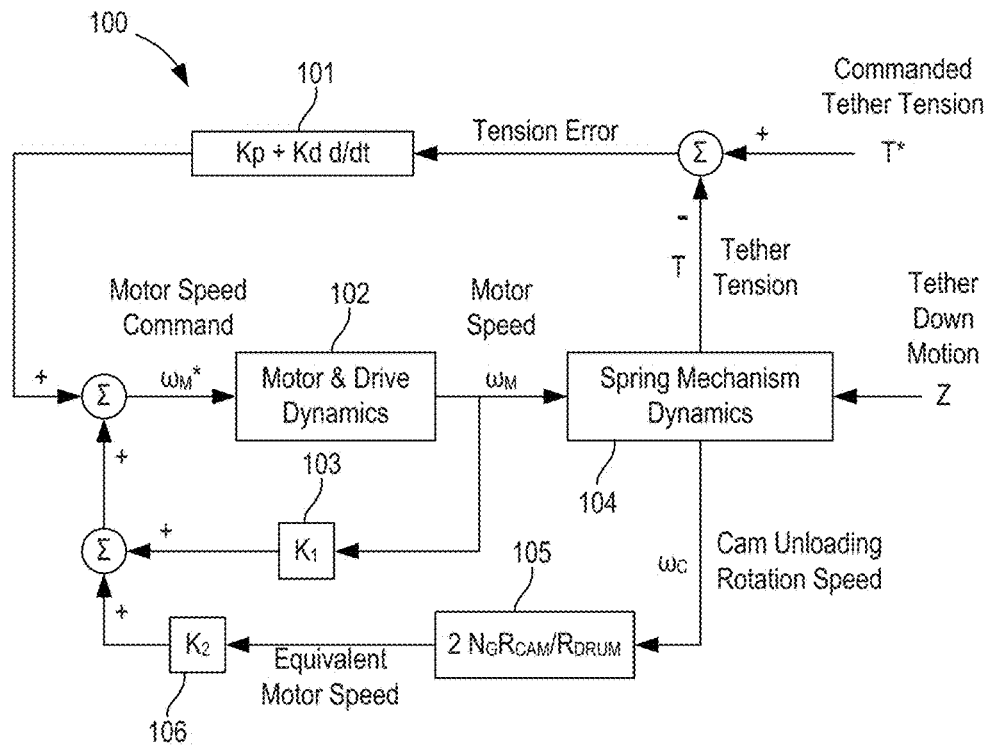


FIG. 48

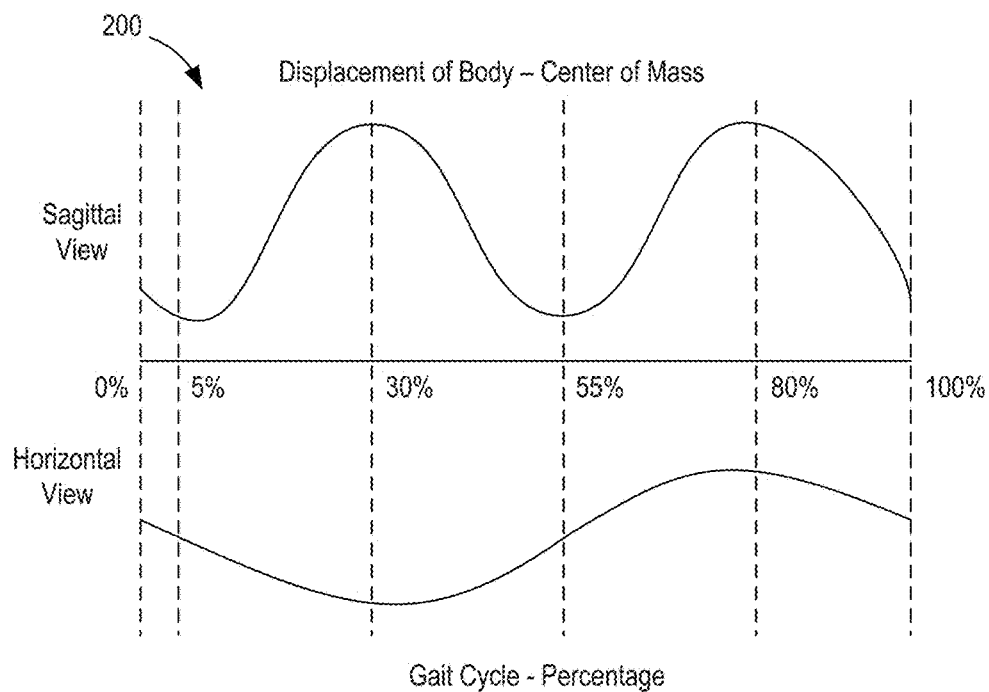


FIG. 49

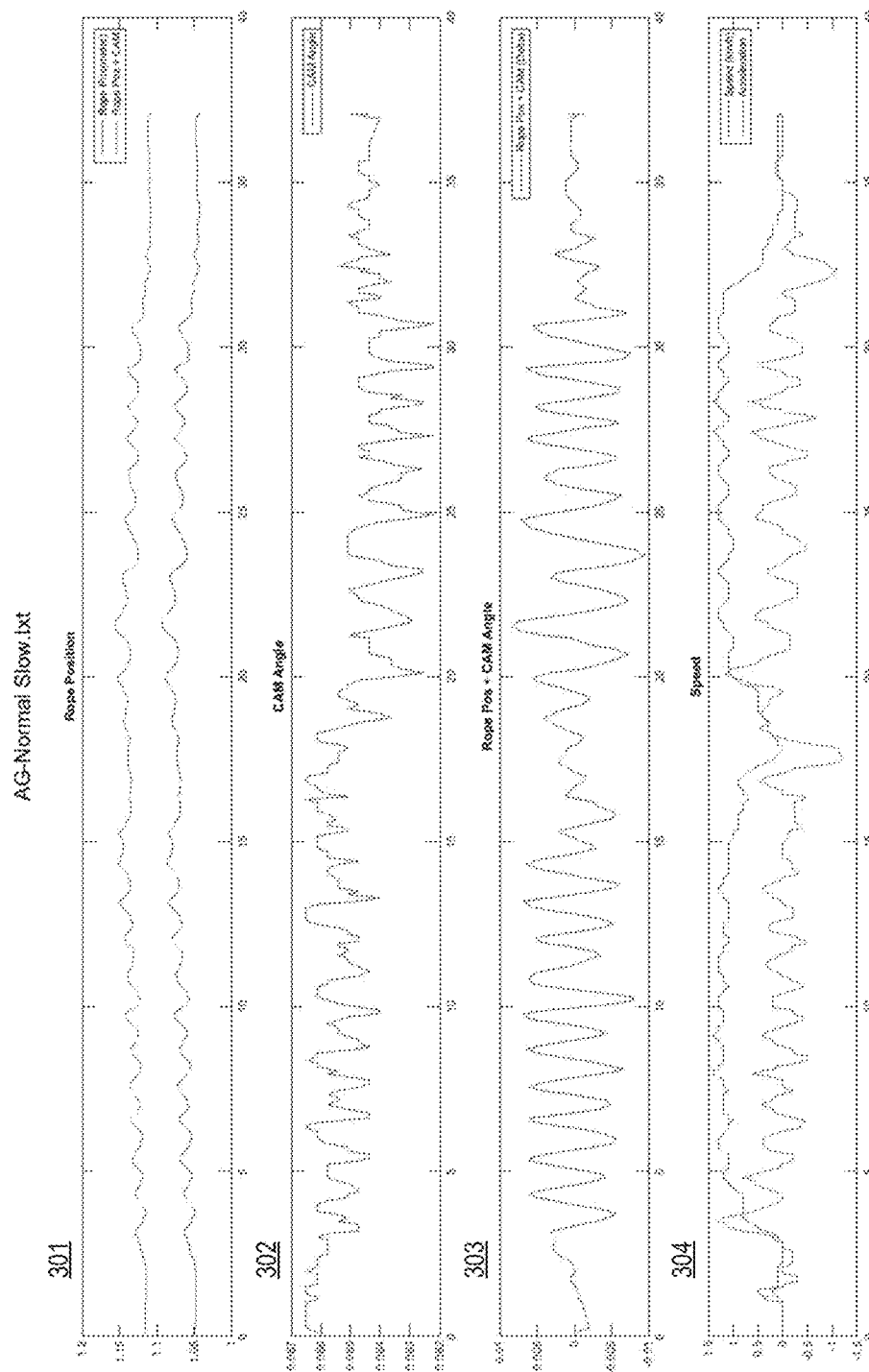


FIG. 50

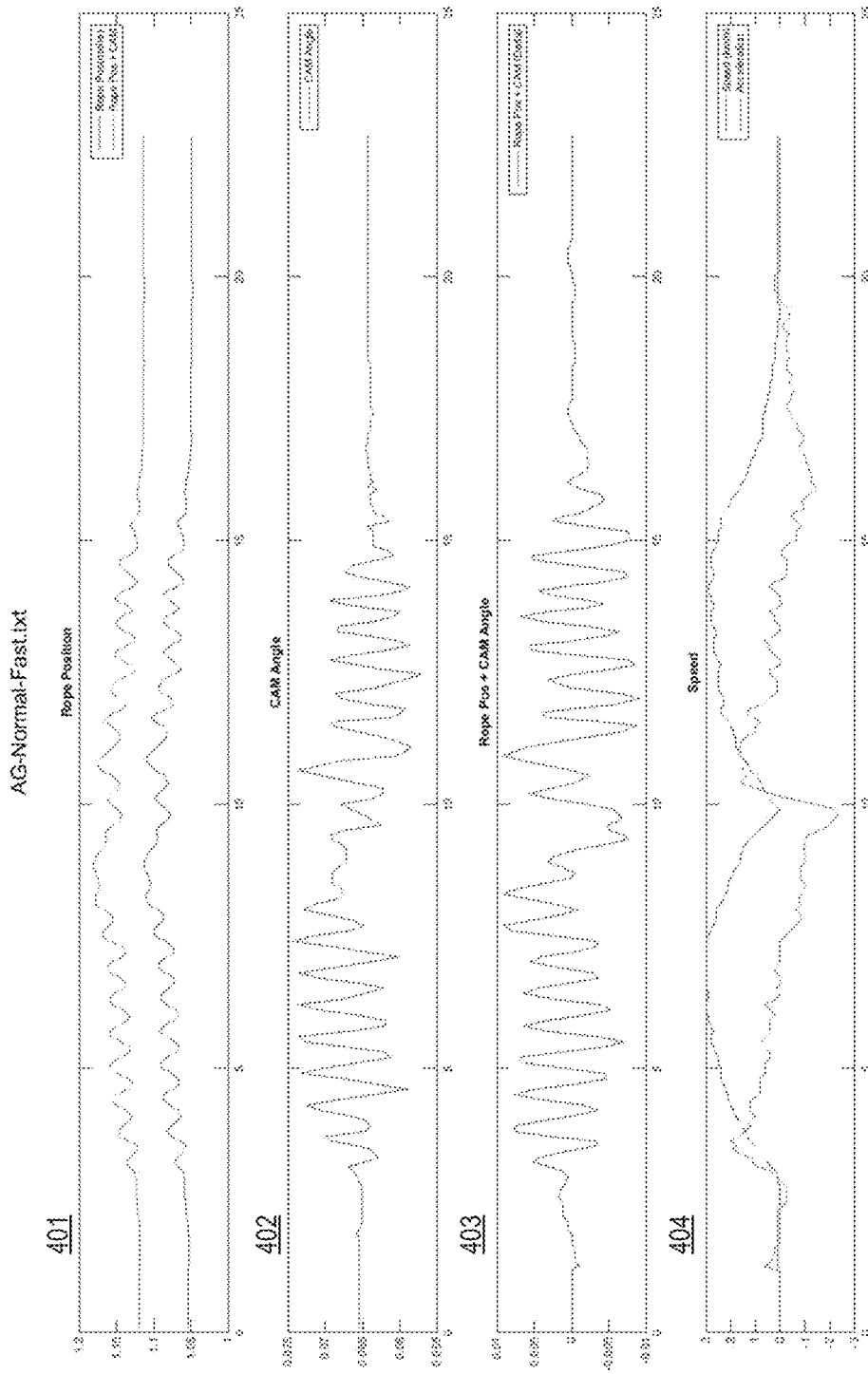


FIG. 51

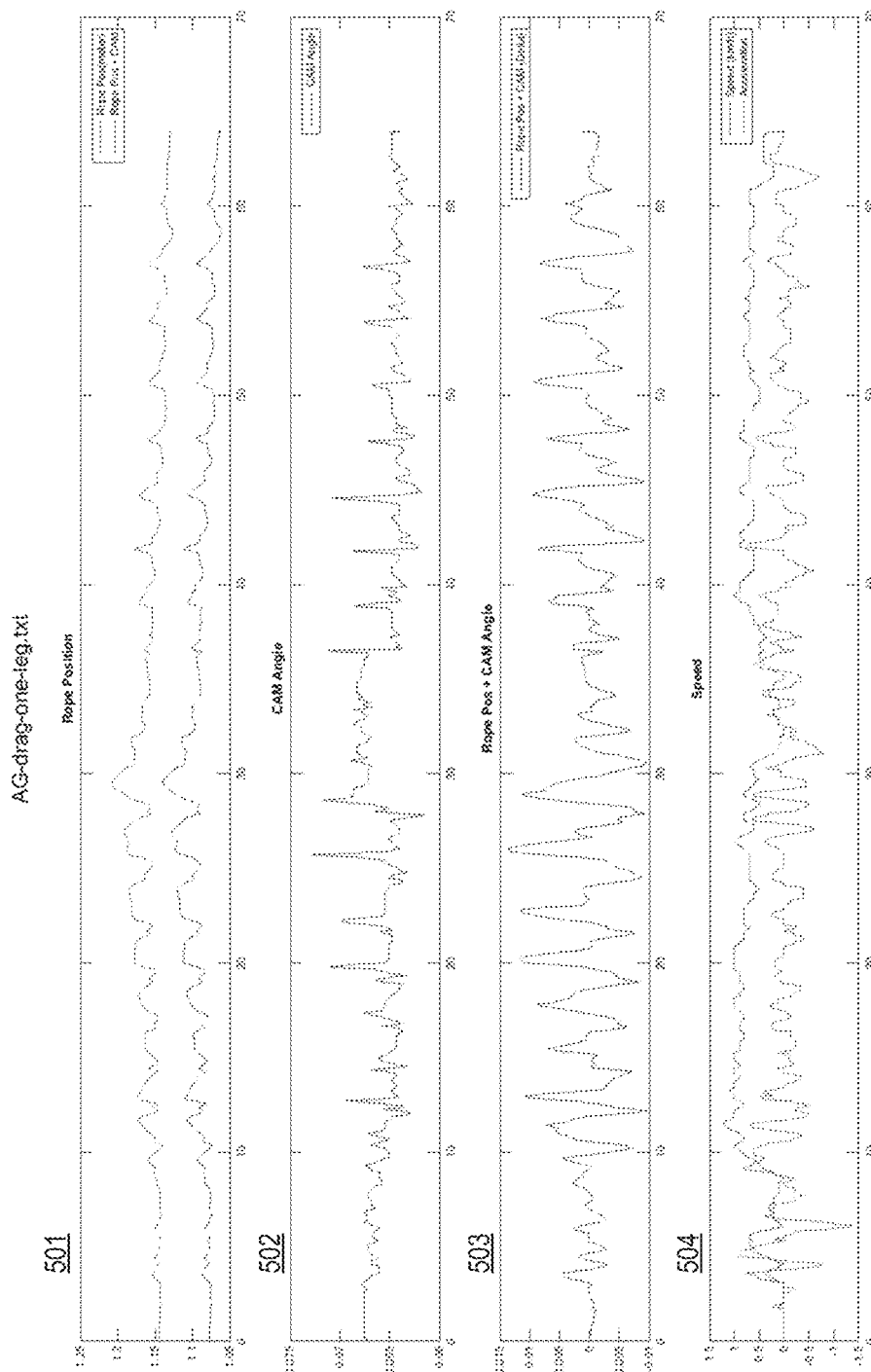


FIG. 52

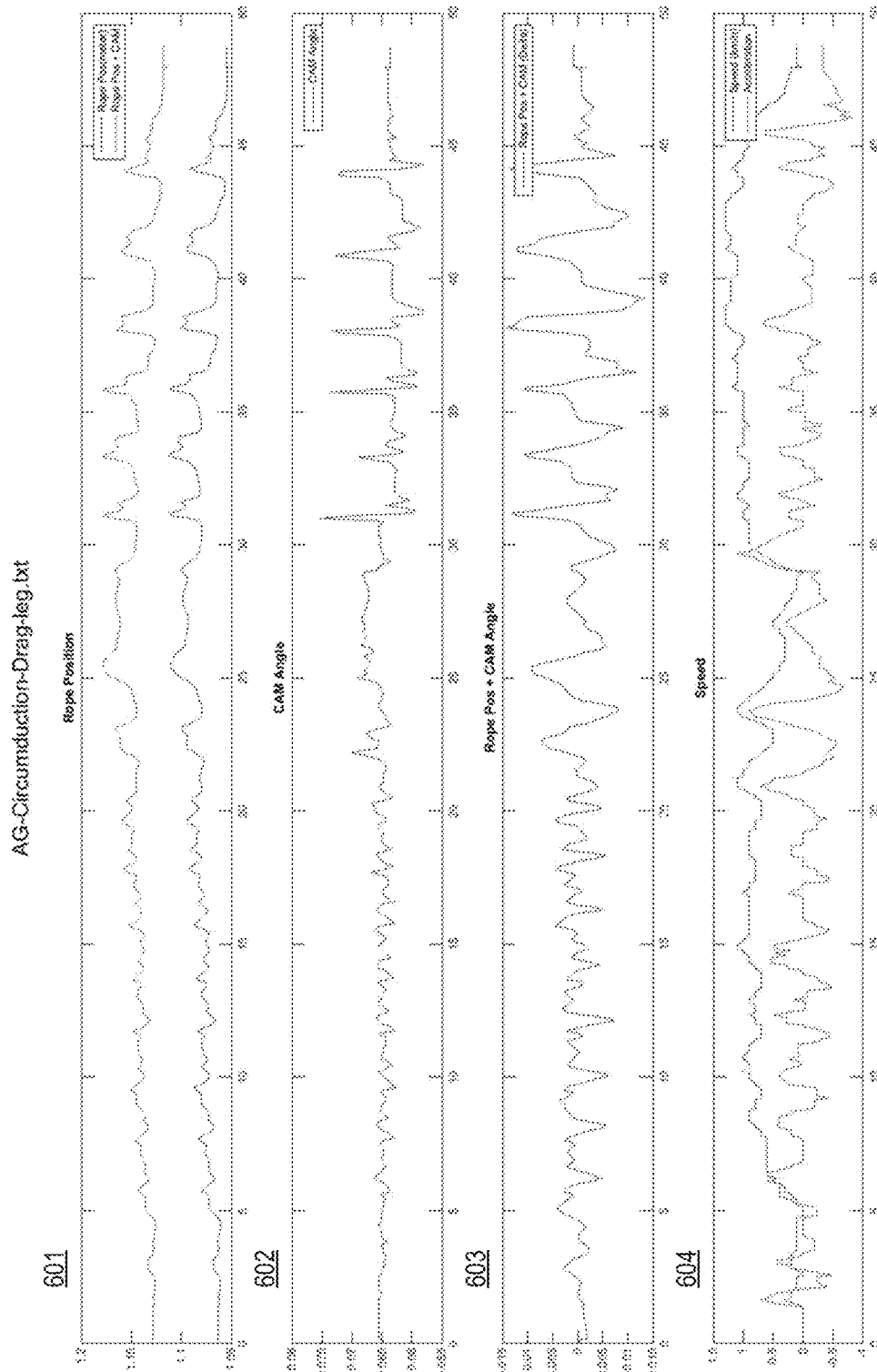


FIG. 53

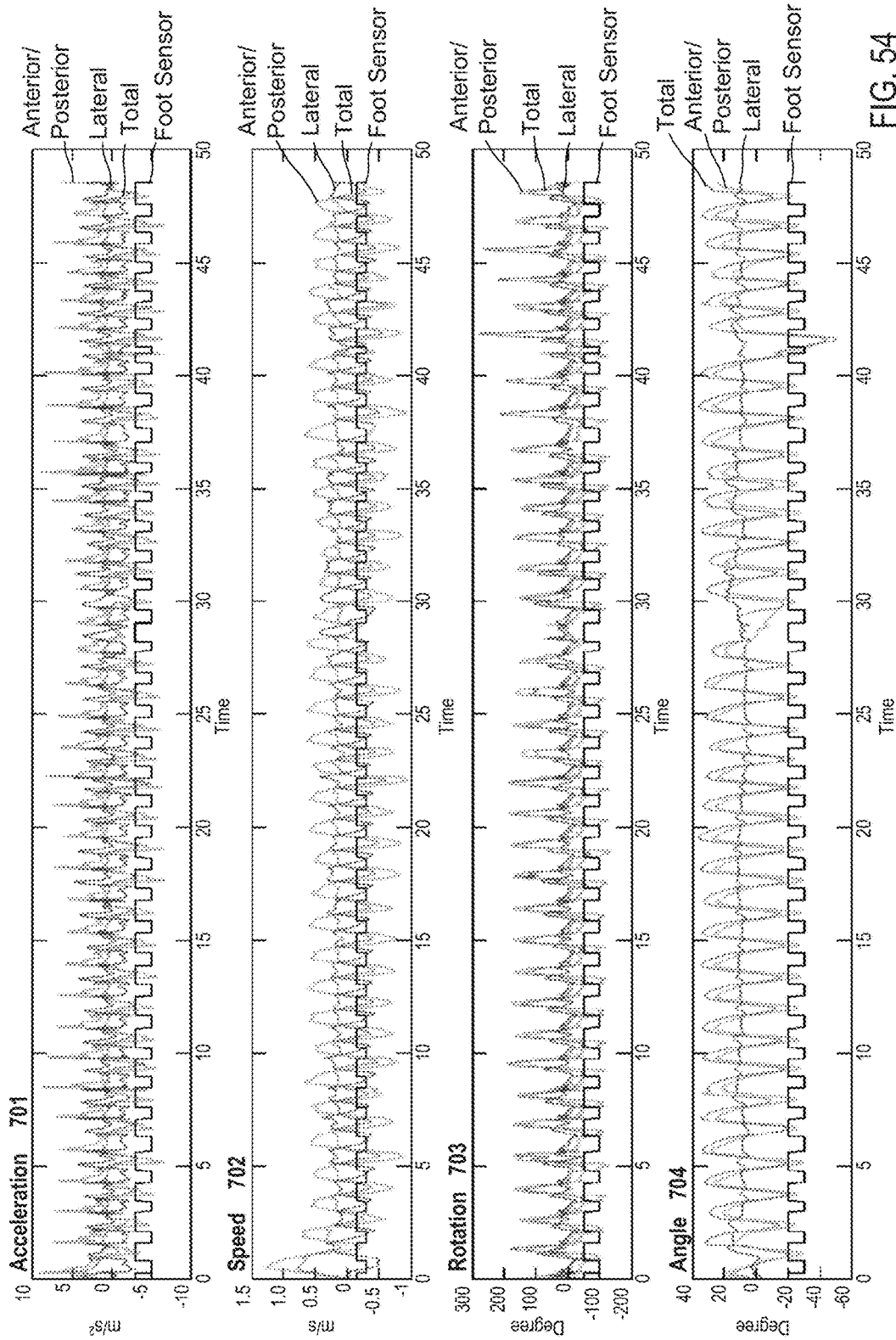


FIG. 54

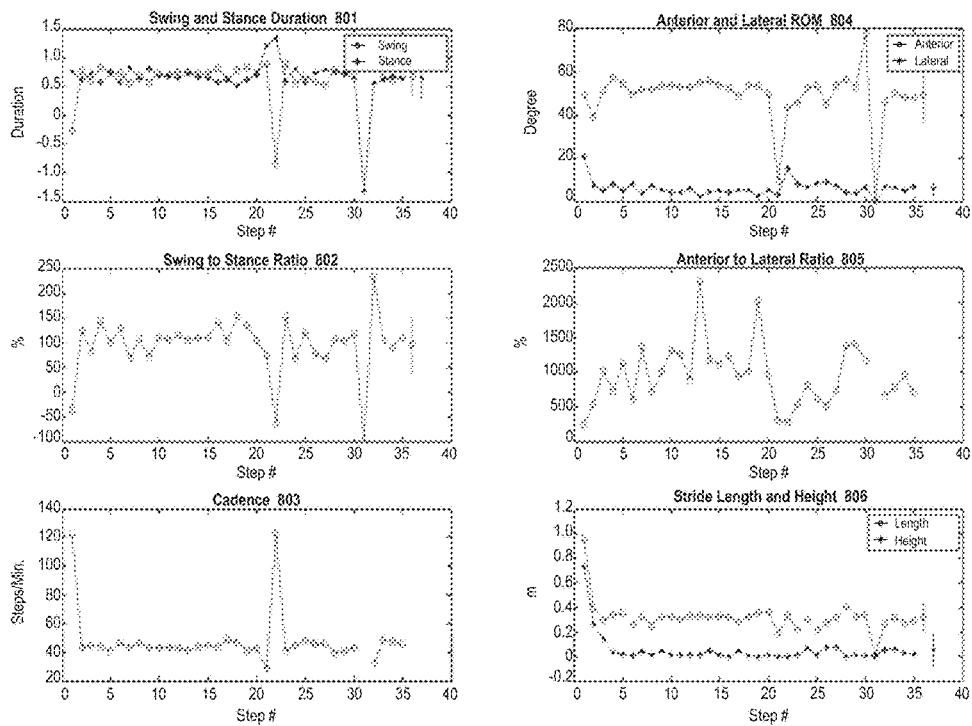


FIG. 55

901

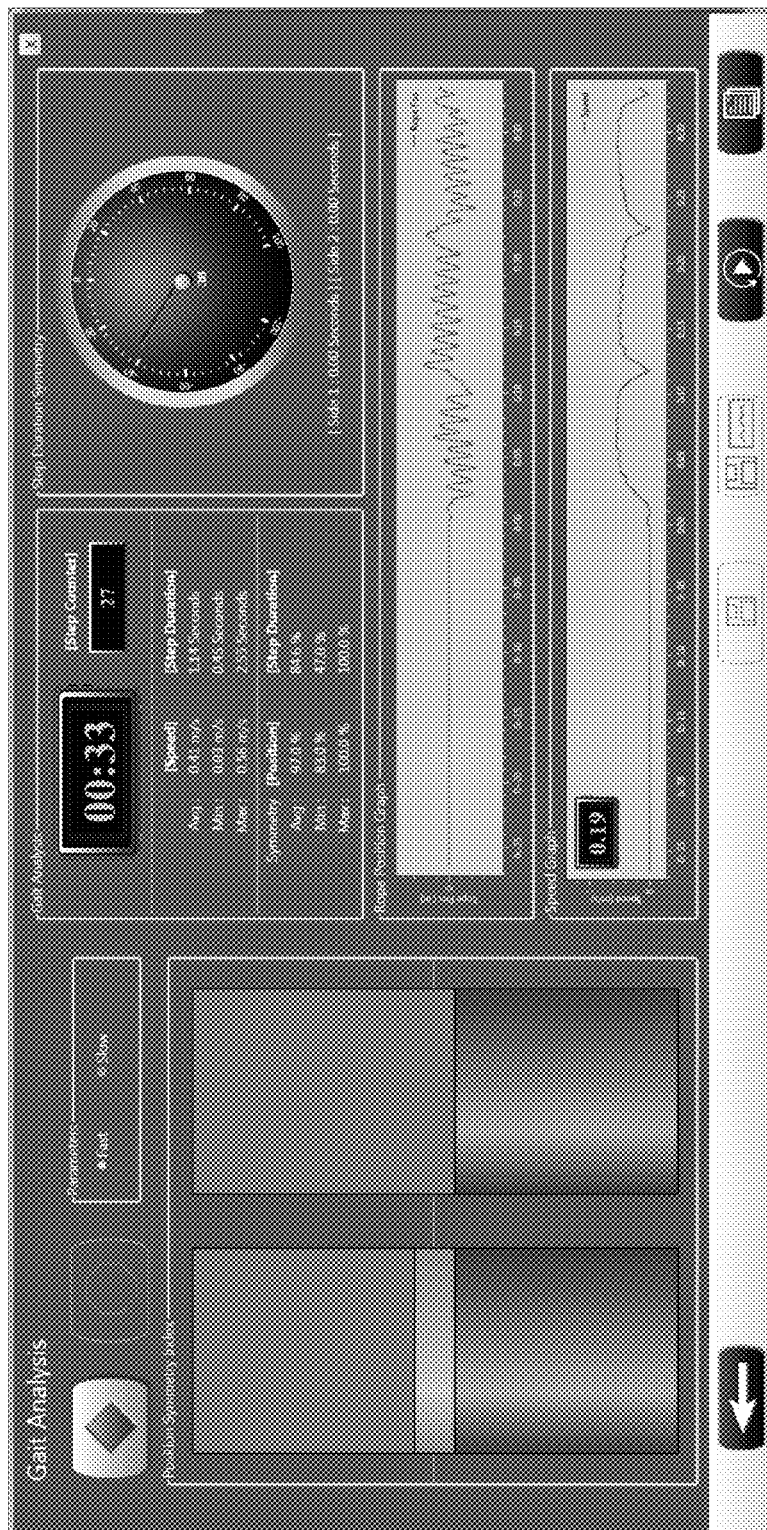


FIG. 56

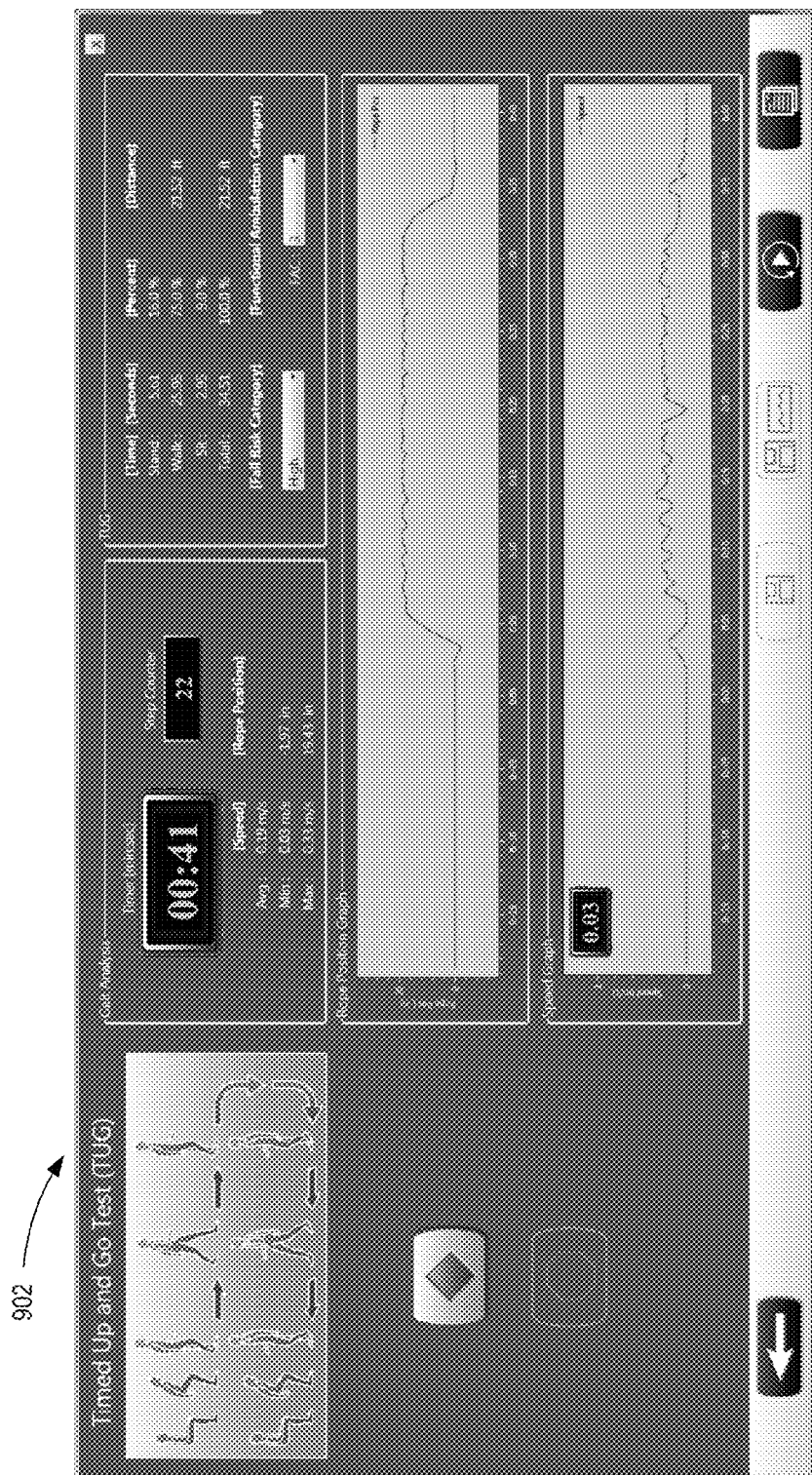


FIG. 57

903

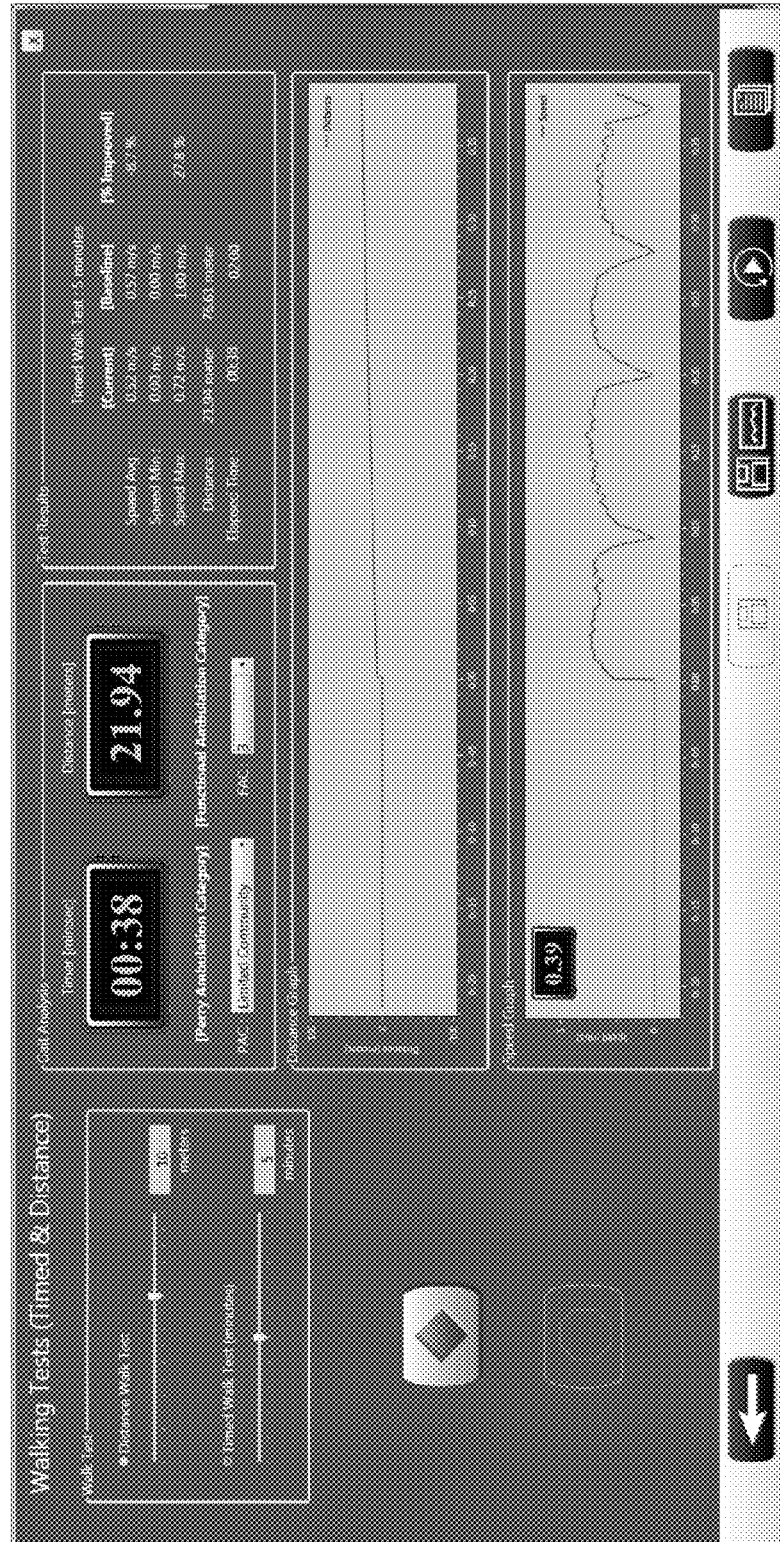


FIG. 58

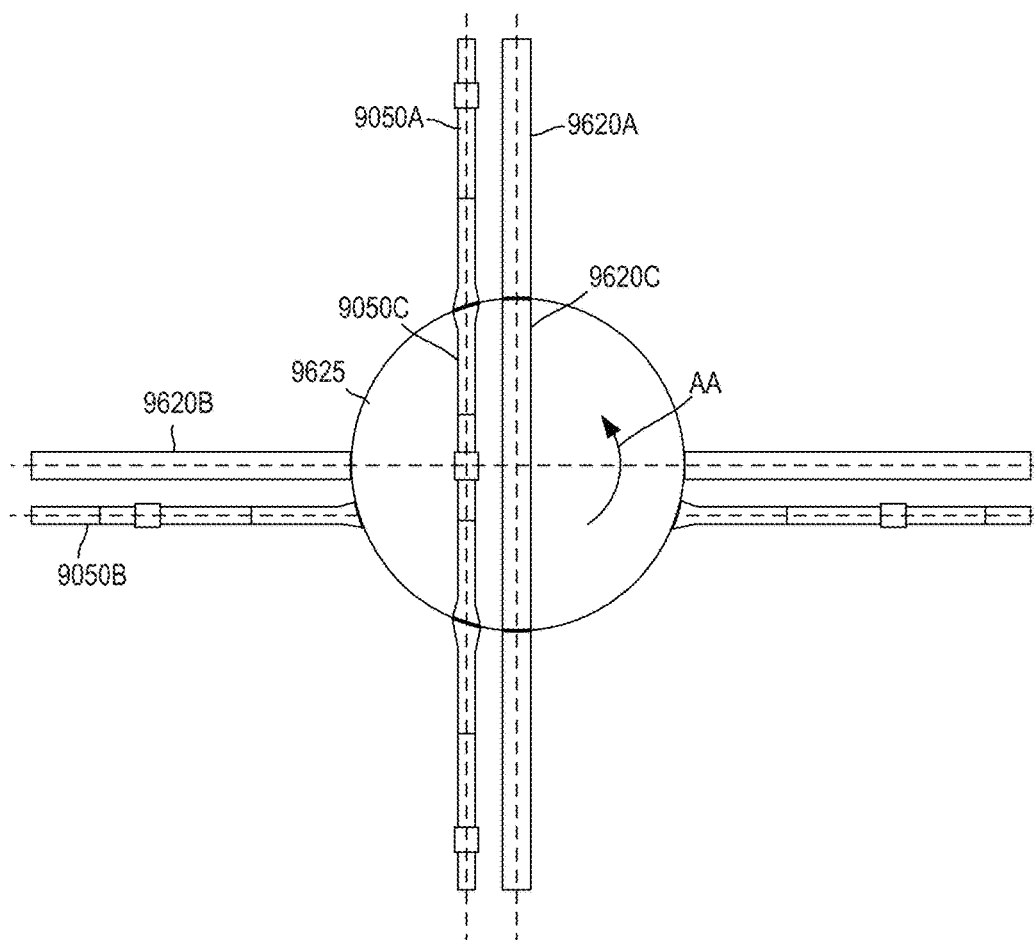


FIG. 59

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METHODS AND APPARATUS FOR BODY WEIGHT SUPPORT SYSTEM

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation-in-part of U.S. Patent Publication No. U.S. 2014/0201906 entitled "Methods and Apparatus for Body Weight Support System," filed Mar. 26, 2014, which is a continuation-in-part of U.S. Patent Publication No. U.S. 2014/0201905 entitled "Methods and Apparatus for Body Weight Support System," filed Jan. 20, 2013, the disclosures of which are incorporated herein by reference in their entireties.

BACKGROUND

The embodiments described herein relate to apparatus and methods for supporting the body weight of a patient. More particularly, the embodiments described herein relate to apparatus and methods for supporting the body weight of a patient during gait therapy.

Successfully delivering intensive yet safe gait therapy to individuals with significant walking deficits can present challenges to skilled therapists. In the acute stages of many neurological injuries such as stroke, spinal cord injury, traumatic brain injury, or the like individuals often exhibit highly unstable walking patterns and poor endurance, making it difficult to safely practice gait for both the patient and therapist. Because of this, rehabilitation centers often move over-ground gait training to a treadmill where body-weight support systems can help minimize falls while raising the intensity of the training.

In some instances, body-weight supported treadmill training can promote gains in walking ability similar to or greater than conventional gait training. Unfortunately, there are few systems for transitioning patients from training on a treadmill to safe, weight-supported over-ground gait training. Furthermore, since a primary goal of most individuals with walking impairments is to walk in their homes and in their communities rather than on a treadmill, it is often desirable that therapeutic interventions targeting gait involve over-ground gait training (e.g., not on a treadmill).

Some known support systems involve training individuals with gait impairments over smooth, flat surfaces. In some systems, however, therapists may be significantly obstructed from interacting with the patient, particularly the lower legs of the patient. For patients that require partial assistance to stabilize their knees and/or hips or that need help to propel their legs, the systems present significant barriers between the patient and the therapist.

Some known gait support systems are configured to provide static unloading to a patient supported by the system. That is, under static unloading, the length of shoulder straps that support the patient are set to a fixed length such that the patient either bears substantially all of their weight when the straps are slack or substantially no weight when the straps are taught. Static unloading systems have been shown to result in abnormal ground reaction forces and altered muscle activation patterns in the lower extremities. In addition, static unloading systems may limit the vertical excursions of a patient that prevent certain forms of balance and postural therapy where a large range of motion is necessary. As a result, some known systems may not be able to raise a patient from a wheelchair to a standing position, thereby restricting the use of the system to individuals who

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are not relegated to a wheelchair (e.g., those patients with minor to moderate gait impairments).

In some known static support systems, there may be a limitation on the amount of body-weight support. In such a system, the body-weight support cannot be modulated continuously, but rather is adjusted before the training session begins and remains substantially fixed at that level during training. Furthermore, the amount of unloading cannot be adjusted continuously since it requires the operator to manually adjust the system.

In other known systems, a patient may be supported by a passive trolley and rail system configured to support the patient while the patient physically drags the trolley along the overhead rail during gait therapy. While the trolley may have a relatively small mass, the patient may feel the presence of the mass. Accordingly, rather than being able to focus on balance, posture, and walking ability, the patient may have to compensate for the dynamics of the trolley. For example, on a smooth flat surface, if the subject stops abruptly, the trolley may continue to move forward and potentially destabilize the subject, thereby resulting in an abnormal compensatory gait strategy that could persist when the subject is removed from the device.

Some known over-ground gait support systems include a motorized trolley and rail system. In such known systems, the motorized trolley can be relatively bulky, thereby placing height restrictions on system. For example, in some known systems, there may be a maximum suitable height for effective support of a patient. In some known systems, a minimum ceiling height may be needed for the system to provide support for patients of varying height.

While the trolley is motorized and programmed to follow the subject's movement, the mechanics and overall system dynamics can result in significant delays in the response of the system such that the patient has the feeling that they are pulling a heavy, bulky trolley in order to move. Such system behavior may destabilize impaired patients during walking. Moreover, some known motorized systems include a large bundle of power cables and/or control cables to power and control the trolley. Such cable bundles present significant challenges in routing and management as well as reducing the travel of the trolley. For example, in some known systems, the cable bundle is arranged in a bellows configuration such that the cable bundle collapses as the trolley moves towards the power supply and expands as the trolley moves away from the power supply. In this manner, the travel of the trolley is limited by the space occupied by the collapsed cable bundle. In some instances, the bundle of cables can constitute a varying inertia that presents significant challenges in the performance of control systems and thus, reduces the efficacy of the overall motorized support system.

Thus, a need exists for improved apparatus and methods for supporting the body-weight of a patient during gait therapy.

SUMMARY

Apparatus and methods for supporting the body weight of a patient during gait therapy are described herein. In some embodiments, an apparatus includes a drive mechanism, a patient support mechanism, and an electronic system. The drive mechanism is included in a trolley and is configured to suspend the trolley from a support track. The drive mechanism includes a first sensor configured to sense an operating condition of the drive mechanism. The patient support mechanism couples to the trolley and includes a tether and

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a second sensor. The tether is configured to be operatively coupled to a patient such that the patient support mechanism supports at least a portion of a weight of the patient. The second sensor is configured to sense an operating condition of the patient support mechanism. The electronic system is included in the trolley and has at least a processor and a memory. The processor is configured to define a gait characteristic of the patient based at least in part on a signal received from the first sensor and a signal received from the second sensor.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a schematic illustration of a body weight support system according to an embodiment.

FIGS. 2 and 3 are perspective views of a body weight support system according to an embodiment.

FIGS. 4-7 are various perspective views of a trolley included in the body weight support system of FIG. 2.

FIG. 8 is a top perspective view of a housing included in the trolley of FIG. 4.

FIG. 9 is an exploded view of the housing of FIG. 8.

FIG. 10 is an enlarged view of a portion of the trolley of FIG. 4 identified as region Z.

FIG. 11 is a bottom perspective view of an electronic system included in the trolley of FIG. 4.

FIG. 12 is a perspective view of a drive mechanism included in the trolley of FIG. 4.

FIGS. 13 and 14 are perspective views of a first drive assembly included in the drive mechanism of FIG. 12.

FIGS. 15 and 16 are exploded views of the first drive assembly of FIG. 13.

FIGS. 17-19 are perspective views of a first support member, a second support member, and a third support member, respectively, included in the first drive assembly of FIG. 13.

FIG. 20 is an exploded view of a drive wheel subassembly included in the first drive assembly of FIG. 13.

FIG. 21 is a perspective view of a secondary wheel subassembly included in the first drive assembly of FIG. 13.

FIG. 22 is a perspective view of a portion of the first drive assembly of FIG. 13, illustrating the secondary wheel subassembly of FIG. 21 coupled to the second support member of FIG. 18.

FIG. 23 is a perspective view of the first drive assembly of FIG. 13 in contact with a support track.

FIG. 24 is a perspective view of a second drive assembly included in the drive mechanism of FIG. 12.

FIG. 25 is an exploded view of the second drive assembly of FIG. 24.

FIG. 26 is a perspective view of the second drive assembly of FIG. 24 in contact with the support track of FIG. 20.

FIG. 27 is a perspective view of a support mechanism and a base included in the housing of FIG. 8 both of which are included in the trolley of FIG. 4.

FIG. 28 is a perspective view of the support mechanism of FIG. 27.

FIG. 29 is a perspective view of a winch assembly included in the support mechanism of FIG. 27.

FIG. 30 is an exploded view of the winch assembly of FIG. 29.

FIG. 31 is an exploded view of a guide assembly included in the support mechanism of FIG. 27.

FIG. 32 is a perspective view the support mechanism of FIG. 27 shown without the winch assembly of FIG. 28.

FIG. 33 is an exploded view of a cam assembly included in the support mechanism of FIG. 27.

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FIG. 34 is a perspective view of a patient attachment mechanism according to an embodiment.

FIG. 35 is a perspective view of a body weight support system according to an embodiment.

FIG. 36 is a cross sectional view of the body weight support system of FIG. 35 taken along the line X-X.

FIG. 37 is a schematic illustration of a support system according to an embodiment.

FIG. 38 is a perspective view of a portion of a support system according to an embodiment.

FIG. 39 is a perspective view of a push cart included in the support system of FIG. 38.

FIG. 40 is a cross-sectional view of a connection member included in the push cart of FIG. 39, taken along the line 40-40.

FIGS. 41 and 42 are a top perspective view and a bottom perspective view of a portion of a support system according to an embodiment.

FIG. 43 is a perspective view of a portion of a support system according to an embodiment.

FIG. 44 is a cross-sectional view of a stopping mechanism included in the support system of FIG. 43, taken along the line 44-44.

FIGS. 45-47 are schematic illustrations of an optical tracking system included in a support system according to an embodiment.

FIG. 48 is a schematic illustration of a control diagram according to an embodiment.

FIG. 49 is a graph illustrating a displacement of a center of mass of a patient according to an embodiment.

FIGS. 50-53 are graphs illustrating operating conditions associated with a patient support mechanism in response to a patient's movement, according to an embodiment.

FIG. 54 illustrates graphical representations of one or more operating conditions associated with an electric stimulator and/or an impaired patient's gait while using a body weight support system, according to an embodiment.

FIG. 55 illustrates graphical representations of a set of gait characteristics of a patient, which were determined based at least in part on data associated with a body weight support system and, for example, an electric stimulator, according to an embodiment.

FIG. 56 is a screen shot of a display showing a graphical representation of data associated with a symmetry analysis of a patient's gait determined, at least in part by a body weight support system, according to an embodiment.

FIG. 57 is a screen shot of a display showing a graphical representation of data associated with a timed-up-and-go test of a patient determined, at least in part by a body weight support system, according to an embodiment.

FIG. 58 is a screen shot of a display showing a graphical representation of data associated with a timed-distance test of a patient determined, at least in part by a body weight support system, according to an embodiment.

FIG. 59 is a schematic illustration of a portion of a support track, a portion of a power rail, and a turntable according to an embodiment.

DETAILED DESCRIPTION

In some embodiments, an apparatus includes a drive mechanism, a patient support mechanism, and an electronic system. The drive mechanism is included in a trolley and is configured to suspend the trolley from a support track. The drive mechanism includes a first sensor configured to sense an operating condition of the drive mechanism. The patient support mechanism couples to the trolley and includes a

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tether and a second sensor. The tether is configured to be operatively coupled to a patient such that the patient support mechanism supports at least a portion of a weight of the patient. The second sensor is configured to sense an operating condition of the patient support mechanism. The electronic system is included in the trolley and has at least a processor and a memory. The processor is configured to define a gait characteristic of the patient based at least in part on a signal received from the first sensor and a signal received from the second sensor.

In some embodiments, a method includes receiving a signal associated with a first operating condition of at least one of a drive mechanism or a patient support mechanism. The patient support mechanism is coupled to an active trolley and configured to support a patient. The drive mechanism is coupled to the active trolley and configured to move the trolley along a support track in response to a movement of the patient. A signal associated with a second operating condition of the at least one of the drive mechanism or the patient support mechanism is received. A difference between the first operating condition and the second operating condition is determined. Based at least in part on the determining, a gait characteristic of the patient supported by the patient support mechanism is defined.

In some embodiments, a method includes receiving a first signal from a first sensor. The first signal is associated with an operating condition of a patient support mechanism included in a patient support system. The patient support mechanism includes a tether configured to tether a patient to the patient support mechanism so that the patient support system supports at least a portion of a weight of the patient. A second signal is received from a second sensor. The second signal is associated with an operating condition of a drive mechanism included in the patient support system. The drive mechanism is configured to (1) suspend the patient support system from a support track and (2) move along the support track in response to a movement of the patient. At least one gait characteristic associated with the movement of the patient is determined based at least in part on the operating condition of the patient support mechanism and the operating condition of the drive mechanism. A third signal is sent to an output device. The third signal is indicative of an instruction to output data associated with the at least one gait characteristic via the output device.

In some embodiments, a system includes a first trolley and a second trolley movably suspended from a support track. The first trolley includes a patient attachment mechanism configured to support a first patient. The first trolley is configured to move relative to the support track. The second trolley includes a patient attachment mechanism configured to support a second patient. The second trolley is configured to move relative to the support track such that the movement of the second trolley is independent of the movement of the first trolley. A collision management assembly is configured to be coupled to one of the first trolley and the second trolley. The collision management assembly includes a bumper that is configured to prevent the first trolley from directly contacting the second trolley.

In some embodiments, an apparatus includes a coupling portion and a trolley portion. The coupling portion is coupled to an end portion of a support track. The coupling portion includes a first member and a second member. The second member is maintained in a fixed position relative to the support track, while the first member is configured to move relative to the support track to transition the coupling portion between a first configuration and a second configuration. The trolley portion is movably suspended from the

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support track and is coupled to an end portion of the first member. The trolley portion includes a bumper that is configured to be placed in contact with a portion of a patient support system such that when the bumper is in contact with the portion of the patient support system and the patient support system moves along the support track towards the end portion, the trolley portion is moved from a first position to a second position relative to the support track. The first member of the coupling portion is moved relative to the second member of the coupling portion as the trolley portion is moved from the first position to the second position, thereby placing the coupling portion in the second configuration. The trolley portion and the coupling portion collectively limit movement of the patient support system towards the end portion of the support track when the coupling portion is in the second configuration.

In some embodiments, an apparatus includes a trolley, a patient attachment mechanism, and a tracking member. The trolley is movably suspended from a support track. The trolley includes an electronic system having an imaging device. The electronic system is configured to control a movement of the trolley along a length of the support track. The patient attachment mechanism is coupled to the trolley and is configured to support a patient as the patient moves from a first position to a second position. The tracking member is coupled to the patient attachment mechanism and is configured to be moved relative to the trolley from a first position, associated with the first position of the patient, to a second position, associated with the second position of the patient. The imaging device of the trolley is configured to capture an image of the tracking member in its first position and an image of the tracking member in its second position. The electronic system is configured to control the movement of the trolley along the length of the support track based at least in part on the image of the tracking member in its first position and the image of the tracking member in its second position.

In some embodiments, a body weight support system includes a trolley, a power rail operative coupled to a power supply, and a patient attachment mechanism. The trolley can include a drive system, a control system, and a patient support system. The drive system is movably coupled to a support rail. At least a portion of the control system is physically and electrically coupled to the power rail. The patient support mechanism is at least temporarily coupled to the patient attachment mechanism. The control system can control at least a portion of the patient support mechanism based at least in part on a force applied to the patient attachment mechanism.

In some embodiments, a body weight support system includes a closed loop track, a powered conductor coupled to the closed loop track, an actively controlled trolley, and a patient support assembly. The actively controlled trolley is movably suspended from the closed loop track and is electrically coupled to the powered conductor. The patient support assembly is coupled to the trolley and is configured to dynamically support a body weight of a patient.

In some embodiments, a body weight support device includes a housing, a drive element, a wheel assembly, and a patient support assembly. At least a portion of the drive element and at least portion of the wheel assembly is disposed within the housing. The patient support assembly is coupled to the drive element and is configured to dynamically support a body weight of a patient.

As used in this specification, the singular forms “a,” “an” and “the” include plural referents unless the context clearly dictates otherwise. Thus, for example, the term “a member”

is intended to mean a single member or a combination of members, “a material” is intended to mean one or more materials, or a combination thereof.

As used herein, the terms “about” and “approximately” generally mean plus or minus 10% of the value stated. For example, about 0.5 would include 0.45 and 0.55, about 10 would include 9 to 11, about 1000 would include 900 to 1100.

As used herein, the term “set” can refer to multiple features or a singular feature with multiple parts. For example, when referring to set of walls, the set of walls can be considered as one wall with multiple portions, or the set of walls can be considered as multiple, distinct walls. Thus, a monolithically constructed item can include a set of walls. Such a set of walls may include multiple portions that are either continuous or discontinuous from each other. For example, a monolithically constructed wall can include a set of detents can be said to form a set of walls. A set of walls can also be fabricated from multiple items that are produced separately and are later joined together (e.g., via a weld, an adhesive, or any suitable method).

As used herein, the term “parallel” generally describes a relationship between two geometric constructions (e.g., two lines, two planes, a line and a plane or the like) in which the two geometric constructions are substantially non-intersecting as they extend substantially to infinity. For example, as used herein, a line is said to be parallel to another line when the lines do not intersect as they extend to infinity. Similarly, when a planar surface (i.e., a two-dimensional surface) is said to be parallel to a line, every point along the line is spaced apart from the nearest portion of the surface by a substantially equal distance. Two geometric constructions are described herein as being “parallel” or “substantially parallel” to each other when they are nominally parallel to each other, such as for example, when they are parallel to each other within a tolerance. Such tolerances can include, for example, manufacturing tolerances, measurement tolerances or the like.

As used herein, the term “tension” is related to the internal forces (i.e., stress) within an object in response to an external force pulling the object in an axial direction. For example, an object with a mass being hung from a rope at one end and fixedly attached to a support at the other end exerts a force to place the rope in tension. The stress within an object in tension can be characterized in terms of the cross-sectional area of the object. For example, less stress is applied to an object having a cross-sectional area greater than another object having a smaller cross-sectional area. The maximum stress exerted on an object in tension prior to plastic deformation (e.g., permanent deformation such as, for example, necking and/or the like) is characterized by the object’s tensile strength. The tensile strength is an intensive property of (i.e., is intrinsic to) the constituent material. Thus, the maximum amount of stress of an object in tension can be increased or decreased by forming the object from a material with a greater tensile strength or lesser tensile strength, respectively.

As used herein, the term “kinematics” describes the motion of a point, object, or system of objects without considering a cause of the motion. For example, the kinematics of an object can describe a translational motion, a rotational motion, or a combination of both translational motion and rotational motion. When considering the kinematics of a system of objects, known mathematical equations can be used to describe to the motion of an object

relative to a plane or set of planes, an axis or set of axes, and/or relative to one or more other objects included in the system of objects.

As used herein, the terms “feedback”, “feedback system”, and/or “feedback loop” relate to a system wherein past or present characteristics influence current or future actions. For example, a thermostat is said to be a feedback system wherein the state of the thermostat (e.g., in an “on” configuration or an “off” configuration) is dependent on a temperature being fed back to the thermostat. Feedback systems can include a control scheme such as, for example, a proportional-integral-derivative (PID) controller. Expanding further, an output of some feedback systems can be described mathematically by the sum of a proportional term, an integral term, and a derivative term. PID controllers are often implemented in one or more electronic devices. In such controllers, the proportional term, the integral term, and/or the derivative term can be actively “tuned” to alter characteristics of the feedback system.

Electronic devices often implement feedback systems to actively control the kinematics of mechanical systems in order to achieve and/or maintain a desired system state. For example, a feedback system can be implemented to control a force within a system (e.g., a mass-spring system and/or the like) by changing the kinematics and/or the position of one or more components relative to any other components included in the system. Expanding further, the feedback system can determine current and/or past states (e.g., position, velocity, acceleration, force, torque, tension, electrical power, etc.) of one or more components included in the mechanical system and return the past and/or current state values to, for example, a PID control scheme. In some instances, an electronic device can implement any suitable numerical method or any combination thereof (e.g., Newton’s method, Gaussian elimination, Euler’s method, LU decomposition, etc.). Thus, based on the past and/or current state of the one or more components, the mechanical system can be actively changed to achieve a desired system state.

FIG. 1 is a schematic illustration of a body weight support system **1000** according to an embodiment. The body weight support system **1000** (also referred to herein as “support system”) includes at least a trolley **1100**, a patient attachment mechanism **1800** (also referred to herein as “attachment mechanism”), a power supply **1610**, a powered conductor or rail **1620**, and a control **1900**. The support system **1000** can be used, for example, in intensive gait therapy to support patients with walking deficiencies brought on by neurological injuries such as stroke, spinal cord injury, traumatic brain injury, or the like. In such instances, the support system **1000** can be used to support at least a portion of the patient’s body weight to facilitate the gait therapy. In other instances, the support system **1000** can be used to simulate, for example, low gravity scenarios for the training of astronauts or the like. In some embodiments, the support system **1000** can be used to support a patient over a treadmill or stairs instead of or in addition to supporting a patient over and across level ground.

The trolley **1100** included in the support system **1000** can be any suitable shape, size, or configuration and can include one or more systems, mechanisms, assemblies, or sub-assemblies (not shown in FIG. 1) that can perform any suitable function associated with, for example, supporting at least a portion of the body weight of a patient. The trolley **1100** can include at least a drive system **1300**, a patient support mechanism **1500**, and an electronic system **1700**. In some embodiments, the drive system **1300** can be movably coupled to a support track (not shown in FIG. 1) and

configured to move (e.g., slide, roll, or otherwise advance) along a length of the support track. The support track can be any suitable shape, size, or configuration. For example, in some embodiments, the support track can be substantially linear or curvilinear. In other embodiments, the support track can be a closed loop such as, for example, circular, oval, oblong, rectangular (e.g., with or without rounded corners), or any other suitable shape. In some embodiments, the support track can be a beam (e.g., an I-beam or the like) included in a roof or ceiling structure from which at least a portion of the trolley **1100** can “hang” (e.g., at least a portion of the trolley **1100** can extend away from the beam). In other embodiments, at least one end portion of the support track can be coupled to a vertical wall or the like. In still other embodiments, the support track can be included in a free-standing structure such as, for example, a gantry or an A-frame.

The drive system **1300** of the trolley **1100** can include one or more wheels configured to roll along a surface of the support track such that the weight of the trolley **1100** and a portion of the weight of a patient utilizing the support system **1000** (e.g., the patient is temporarily coupled to the trolley **1100** via the patient attachment mechanism **1800**, as described in further detail herein) are supported by the support track. Similarly stated, one or more wheels of the drive system **1300** can be disposed adjacent to and on top of a horizontal surface of the support track; thus, the trolley **1100** can be “hung” from or suspended from the support track. In other embodiments, the surface from which the trolley **1100** is hung need not be horizontal. For example, at least a portion of the support track can define a decline (and/or an incline) wherein a first end portion of the support track is disposed at a first height and a second end portion of the support track is disposed at a second height, different from the first height. In such embodiments, the trolley **1100** can be hung from a surface of the support track that is parallel to a longitudinal centerline (not shown) of the trolley **1100**. In such embodiments, the trolley can be used to support a patient moving across an inclined/declined surface, up or down stairs, etc.

In some embodiments, the trolley **1100** can have or define a relatively small profile (e.g., height) such that the space between a surface of the trolley **1100** and a portion of the patient can be sufficiently large to allow the patient to move between a seated position to a standing position such as, for example, when a patient rises out of a wheelchair. Furthermore, with the trolley **1100** being hung from the support track, the weight of the trolley **1100** and the weight of the patient utilizing the support system can increase the friction (e.g., traction) between the one or more wheels of the drive system and the surface of the support track from which the trolley **1100** is hung. Thus, the one or more wheels of the drive system **1300** can roll along the surface of the support track without substantially slipping.

In some embodiments, the trolley **1100** can be motorized. For example, in some embodiments, the trolley **1100** can include one or more motors configured to power (e.g., drive, rotate, spin, engage, activate, etc.) the drive system **1300**. In some embodiments, the motor(s) can be configured to rotate the wheels of the drive system **1300** at any suitable rate and/or any suitable direction (e.g., forward or reverse) such that the trolley **1100** can pace a patient utilizing the support system **1000**, as described in further detail herein. In some embodiments, the electronic system **1700** and/or the control **1900** can be operatively coupled (e.g., electrically connected) to the one or more motors such that the electronic system **1700** and/or the control **1900** can send an electronic

signal associated with operating the motor(s). In some embodiments, the motor(s) can include a clutch, a brake, or the like configured to substantially lock the motor(s) in response to a power failure or the like. Similarly stated, the motor(s) can be placed in a locked configuration to limit movement of the trolley **1100** (e.g., limit movement of the drive system **1300** and/or the patient support mechanism **1500**) in response to a power failure (e.g., a partial power failure and/or a total power failure).

The patient support mechanism **1500** (also referred to herein as “support mechanism”) can be any suitable configuration and can be at least temporarily coupled to the attachment mechanism **1800**. For example, in some embodiments, the support mechanism **1500** can include a tether that can be temporarily coupled to a coupling portion of the attachment mechanism **1800**. Moreover, the attachment mechanism **1800** can further include a patient coupling portion (not shown in FIG. 1) configured to receive a portion of a harness or the like worn by or coupled to the patient. Thus, the attachment mechanism **1800** and the support mechanism **1500** can support a portion of the body weight of a patient and temporarily couple the patient to the trolley **1100**.

In some embodiments, an end portion of the tether can be coupled to, for example, a winch. In such embodiments, the winch can include a motor that can rotate a drum to coil or uncoil the tether. Similarly stated, the tether can be wrapped around the drum and the motor can rotate the drum in a first direction to wrap more of the tether around the drum and can rotate the drum in a second direction, opposite the first direction, to unwrap more of the tether from around the drum. In some embodiments, the support mechanism **1500** can include one or more pulleys that can engage the tether such that the support mechanism **1500** gains a mechanical advantage. Similarly stated, the pulleys can be arranged such that the force exerted by the winch to coil or uncoil the tether around the drum while a patient is coupled to the attachment mechanism **1800** is reduced.

The horizontal drive system/motor that is configured to allow for movement of the trolley along the track, and the vertical drive system configured to move to control the tether can be simultaneously controlled and operated or not. For example, when a patient is walking over a treadmill, there is little or no horizontal movement, but the vertical (weight bearing) drive system is operational to compensate for the changes during the gait, falls, etc.

In some embodiments, the pulley system can include at least one pulley that is configured to move (e.g., pivot, translate, swing, or the like). For example, the pulley can be included in or coupled to a cam mechanism (not shown) that is configured to define a range of motion of the pulley. In such embodiments, the movement of the at least one pulley can coincide and/or be caused by a force exerted on the attachment mechanism **1800**. For example, in some instances, the patient can move relative to the trolley **1100** such that the force exerted on the tether by the weight of the patient is changed (e.g., increased or decreased). In such instances, the pulley can be moved according to the change in the force such that the tension within the tether is substantially unchanged. Moreover, with the pulley included in or coupled to the cam mechanism, the movement of the pulley can move the cam through a predetermined range of motion. In some embodiments, the electronic system **1700** can include a sensor or encoder operatively coupled to the pulley and/or the cam that is configured to determine the amount of movement of the pulley and/or the cam. In this manner, the electronic system **1700** can send a signal to the

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motor included in the winch associated with coiling or uncoiling the tether around the drum in accordance with the movement of the pulley. For example, the pulley can be moved in a first direction in response to an increase in force exerted on the tether and the electronic system **1700** can send a signal to the motor of the winch associated with rotating the drum to uncoil a portion of the tether from the drum. Conversely, the pulley can be moved in a second direction, opposite the first direction, in response to a decrease in force exerted on the tether and the electronic system **1700** can send a signal to the motor of the winch associated with rotating the drum to coil a portion of the tether about the drum. Thus, the support mechanism **1500** can be configured to exert a reaction force in response to the force exerted by the patient such that the portion of the body weight supported by the support system **1000** remains substantially unchanged. Moreover, by actively supporting the portion of the body weight of the patient, the support system **1000** can limit the likelihood and/or the magnitude of a fall of the patient supported by the support system **1000**. Similarly stated, the support mechanism **1500** and the electronic system **1700** can respond to a change in force exerted on the tether in a relatively short amount of time (e.g., much less than a second) to actively limit the magnitude of the fall of the patient.

As described above, the electronic system **1700** included in the trolley **1100** can control at least a portion of the trolley **1100**. The electronic system **1700** includes at least a processor and a memory. The memory can be, for example, a random access memory (RAM), a memory buffer, a hard drive, a read-only memory (ROM), an erasable programmable read-only memory (EPROM), and/or the like. In some embodiments, the memory stores instructions to cause the processor to execute modules, processes, and/or functions associated with controlling one or more mechanical and/or electrical systems included in the patient support system **1000**, as described above. In some embodiments, control signals are delivered through the powered rail using, for example, a broadband over power-line (BOP) configuration.

The processor of the electronic device can be any suitable processing device configured to run or execute a set of instructions or code. For example, the processor can be a general-purpose processor (GPU), a central processing unit (CPU), an accelerated processing unit (APU), and/or the like. The processor can be configured to run or execute a set of instructions or code stored in the memory associated with controlling one or more mechanical and/or electrical systems included in a patient support system **1000**. For example, the processor can run or execute a set of instructions or code associated with controlling one or more motors, sensors, communication devices, encoders, or the like, as described above. More specifically, the processor can execute a set of instructions in response to receiving a signal from one or more sensors and/or encoders associated with a portion of the drive system **1300** and/or the support mechanism **1500**. Similarly stated, the processor can be configured to execute a set of instructions associated with a feedback loop (e.g., based on a proportional-integral-derivative (PID) control method) wherein the electronic system **1700** can control the subsequent action of the drive system **1300** and/or the support system **1500** based at least in part on current and/or previous data (e.g., position, velocity, force, acceleration, angle of the tether, or the like) received from the drive system **1300** and/or the support system **1500**, as described in further detail herein.

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In some embodiments, the electronic system **1700** can include a communication device (not shown in FIG. **1**) that can be in communication with the control **1900**. For example, in some embodiments, the communication device can include one or more network interface devices (e.g., a network interface card). The communication device can be configured to transmit data over a wired and/or wireless network (not shown in FIG. **1**) associated with sending data to and/or receiving data from the control **1900**. The control **1900** can be any suitable device or module (e.g., hardware module or software module stored in the memory and executed in the process). For example, in some embodiments, the control **1900** can be an electronic device that includes at least a processor and a memory (not shown in FIG. **1**) and is configured to run, for example, a personal computer application, a mobile application, a web page, and/or the like. In this manner, a user can engage the control **1900** to establish a set of system parameters associated with the support system **1000**, as described in further detail herein. In some embodiments, the control **1900** can be implemented as a handheld controller.

In some embodiments, control of the trolley **1100** can be accomplished using one or more controllers. In embodiments in which multiple controllers are utilized (e.g., a personal computer control and a handheld control), only one controller can be used at a time. In other embodiments, one of the controllers (e.g., the handheld controller) can override the personal computer controller. In other embodiments, a user can designate which controller is utilized by actuating the relevant controller. In other words, the user either can take control using a controller or can pass control to the other controller by actuating the controller.

In some embodiments, the patient support system **1000** is configured to improve gait and stability rehabilitation training by adding visual and audio feedback to a gait and stability assistance device. The trolley **1100** coordinates the feedback with heuristic patient data from past training sessions, and stores the data for each therapy/training.

As shown in FIG. **1**, the trolley **1100** is operatively coupled to the power rail **1620**. The power rail **1620** is further coupled to the power source **1610** that is configured to provide a flow of electrical current (e.g., electrical power) to the power rail **1620**. More specifically, the power rail **1620** can include any suitable transformer, converter, conditioner, capacitor, resistor, insulator, and/or the like (not shown in FIG. **1**) such that the power rail **1620** can receive the flow of electrical current from the power source **1610** and transfer at least a portion of the flow of electrical current to the trolley **1100**. The power rail **1620** can include one or more electrical conductors to deliver, for example, single or multiphase electrical power to one or more trolleys **1100**. For example, in some embodiments, the power rail **1620** is a substantially tubular rail configured to receive a conductive portion of the electronic system **1700** of the trolley **1100**. More specifically, the power rail **1620** can include one or more conductive surfaces disposed within an inner portion of the tubular rail along which a conductive member of the electronic system **1700** can move (e.g., slide, roll, or otherwise advance). In this manner, the power rail **1620** can transmit a flow of electrical current from the power source **1610** to the electronic system **1700** of the trolley **1100**, as described in further detail herein. The power rail **1620** can be any suitable shape, size, or configuration. For example, the power rail **1620** can extend in a similar shape as the support track (not shown in FIG. **1**) and can be arranged such that the power rail **1620** is substantially parallel to the support track. In this manner, the trolley **1100** can advance

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along a length of the support track while remaining in electrical contact with the power rail **1620**. Furthermore, the arrangement of the power rail **1620** and the trolley **1100** is such that movement of the trolley **1100** along the length of the support track is not hindered or limited by a bundle of cables, as described above with reference to known support systems.

Moreover, the control **1900** can also be operatively coupled to the power supply **1610** and can be configured to control the amount of power delivered to the power rail **1620**. For example, the control **1900** can be configured to begin a flow of electrical current from the power supply **1610** to the power rail **1620** to turn on or power up the support system **1000**. Conversely, the control **1900** can be configured to stop a flow of electrical current from the power supply **1610** to the power rail **1620** to turn off or power down the support system **1000**.

While the control **1900** is shown in FIG. **1** as being independent from and operatively coupled to the trolley **1100**, in some embodiments, the control **1900** can be included in the electronic system **1700** of the trolley **1100**. For example, in some embodiments, the control **1900** can be a hardware module and/or a software module that can be executed by the processor of the electronic system **1700**. In such embodiments, the electronic system **1700** can include a user interface (e.g., a touch screen and/or one or more dials, buttons, switches, toggles, or the like). Thus, a user (e.g., a physical therapist, a doctor, a nurse, a technician, etc.) can engage the user interface associated with the control **1900** to establish a set of system parameters for the support system **1000**.

Although not shown in FIG. **1**, in some embodiments, more than one trolley **1100** can be coupled to the same support track. In such embodiments, the trolleys **1100** hung from the support track can include, for example, sensors (e.g., ultrasonic proximity sensors and/or the like) that can send a signal to the electronic system **1700** associated with the proximity of one or more trolleys **1100** relative to a specific trolley **1100**. In this manner, the electronic system **1700** of the trolleys **1100** can control, for example, a motor included in the drive system **1300** to prevent collision of the trolleys **1100**. Thus, the support system **1000** can be used to support more than one patient (e.g., a number of patients corresponding to a number of trolleys **1100** disposed about the support track) while keeping the patients at a desired distance from one another.

In some embodiments, the support system is configured to provide feedback to a patient during use. In some embodiments, a laser or culminated light source is coupled to the trolley **1100** to create a light path for a patient to follow during a session. The light path allows the patient to look ahead or look at their feet while attempting to train their brain to properly control the leg/foot/hip motion. In some embodiments, a second light source is configured to illuminate a "target" location at which the patient can aim to plant their foot in a proper location. In some embodiments, the size of the target can be varied depending upon the dexterity of the user. In other words, for a user with greater muscle control, the target can be smaller. The light path and target location can be modified using a user interface as described in greater detail herein.

In some embodiments, audible feedback is provided to the patient when the patient's gait is incorrect. In some embodiments, audible feedback can be provided when the patient begins to fall. Different audible tones can be provided for different issues/purposes.

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In some embodiments, a CCD camera interface is configured for video monitoring for future analysis and can be correlated to sensed rope position, speed, tension, etc. In some embodiments, monitors can be coupled to a patient's body to monitor muscle usage (e.g., leg muscles, torso muscles, etc.). Such information can be wirelessly transmitted to the electronic system **1700** and coordinated in the feedback provided to the patient during and after a therapy/rehabilitation session. Said another way, all of the data collected by the various sensors, cameras, etc. can be coordinated to provided dynamic, real-time feedback and/or post-session feedback.

Although described above as being coupled to a power rail **1620**, in some embodiments, a trolley can be battery powered. In such embodiments, the trolley can include a battery system that is suitable for providing the trolley with a flow of electrical current. The battery system included in such embodiments can be rechargeable. For example, in some embodiments, the trolley and more specifically the battery system can be temporarily coupled the power source **1610** to charge the battery system. In other embodiments, the battery system can be at least temporarily coupled to the power rail **1620** to recharge the battery system. In some embodiments, the charging station(s) can be located in certain location(s) on the track. The trolley(s) can automatically dock to the charging stations according to a certain algorithm. For example, the trolley may travel to and dock to the charging station when the battery level is below certain level or during the break periods (for example when the system is not in use for certain time, at night, or at pre-determined times).

FIGS. **2-33** illustrate a body weight support system **2000** according to an embodiment. The body weight support system **2000** (also referred to herein as "support system") can be used to support a portion of a patient's body weight, for example, during gait therapy or the like. FIGS. **2** and **3** are perspective views of the support system **2000**. The support system **2000** includes a trolley **2100**, a power system **2600**, and a patient attachment mechanism **2800** (see e.g., FIG. **34**). As shown in FIGS. **2** and **3**, the trolley **2100** is movably coupled to a support track **2050** that is configured to support the weight of the trolley **2100** and the weight of the patient utilizing the support system **2000**. Although the support track **2050** is shown as having an I-shape, the support track **2050** can be any suitable shape. Furthermore, while the support track **2050** is shown as being substantially linear, the support track **2050** can extend in a curvilinear direction. In other embodiments, the support track **2050** can be arranged in a closed loop such as, for example, circular, oval, oblong, square, or the like. As described in further detail herein, the power system **2600** can include a power rail **2620** that extends substantially parallel to the support track **2050** and is at least electrically coupled to the trolley **2100** to transfer a flow of electrical current from a power source (not shown in FIGS. **2-32**) to the trolley **2100**.

FIGS. **4-7** are perspective views of the trolley **2100**. The trolley **2100** can be any suitable shape, size, or configuration. For example, the trolley **2100** can be suspended from the support track **2050** (as described in further detail herein) and can have or define a relatively small profile (e.g., height) such that the space between the trolley **2100** and a patient can be maximized. In this manner, the support system **2000** can be used to support patients of varying heights as well as supporting a patient rising from a sitting position to a standing position as is common in assisting patient at least partially relegated to a wheelchair. The trolley **2100** includes a housing **2200** (see e.g., FIGS. **8** and **9**), an electronic

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system **2700** (see e.g., FIGS. **10** and **11**), a drive system **2300** (see e.g., FIGS. **12-26**), and a patient support mechanism **2500** (see e.g., FIGS. **27-33**).

As shown in FIGS. **8** and **9** the housing **2200** includes a base **2210**, a first side member **2230**, a second side member **2240**, a third side member **2250**, and a cover **2260**. The housing **2200** is configured to enclose and/or cover at least a portion of the electronic system **2700**, as described in further detail herein. As shown in FIG. **9**, the base **2210** has a first side **2211** and a second side **2212**. The base **2210** defines a set of drive mechanism openings **2213**, a fan opening **2214**, a guide mechanism opening **2215**, a bias mechanism opening **2217**, a guide member opening **2218**, and a cam pulley opening **2219**, a cam pivot opening **2220**. As described in further detail herein, the drive mechanism openings **2213** receive at least a portion of a first drive assembly **2310** included in the drive mechanism **2300** such that a set of wheels included therein can rotate without contacting the base **2210**. The fan opening **2214** receives a portion of a fan **2740** included in the electronic system **2700**. More specifically, a portion of the fan **2740** can extend through the opening such that the fan can remove heat from within the housing **2200** produced by the electronic system **2700**. The guide mechanism opening **2215** receives a portion of a guide mechanism **2540** included in the patient support mechanism **2500** (also referred to herein as “support mechanism”). More specifically, the base **2210** includes a set of mounting tabs **2216** configured to extend from a surface of the base **2210** that defines the guide mechanism opening **2215**. In this manner, the guide mechanism **2540** can be coupled to the mounting tabs **2216**. The bias mechanism opening **2217**, the guide member opening **2218**, the cam pulley opening **2219**, and the cam pivot opening **2220** can each movably receive a portion of a cam mechanism **2570** included in the support mechanism **2500**, as described in further detail herein.

The first side member **2230** has a first side **2231** and a second side **2232**. The second side **2232** defines a slot **2233** that receives a portion of the base **2210** to couple the base **2210** thereto. The first side member **2230** also includes a mounting portion **2235** that is coupled to a portion of a collector **2770** included in the electronic system **2700**, as described in further detail herein. The second side member **2240** has a first side **2241** and a second side **2242**. The second side **2242** defines a slot **2243** that receives a portion of the base **2210** to couple the base **2210** thereto. The second side **2242** also includes a recessed portion **2244** that is coupled to a portion of a winch assembly **2510** included in the support mechanism **2500**. The third side member **2250** is coupled to the first side member **2230**, the second side member **2240**, and the base **2210** and defines a light opening **2251** that receives an indicator light and a power outlet opening that receives a power outlet module.

The cover **2260** is disposed adjacent to the second side **2212** of the base **2210**. More specifically, the cover **2260** can be removably coupled to the second side **2212** of the base **2210** such that the portion of the electronic system **2700** enclosed therein can be accessed. The cover **2260** has a first end portion **2261** and a second end portion **2262**. The first end portion **2261** is open-ended and defines a notch **2265** configured to receive a portion of the collector **2770**, as described in further detail herein. The second end portion **2262** of the cover **2260** is substantially enclosed and is configured to include a recessed region **2264**. In this manner, a portion of the support mechanism **2500** can extend into and/or through the recessed region **2264** to couple to the patient attachment mechanism **2800**, as described in further

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detail herein. The cover **2260** also defines a set of vents **2263** that can be arranged to provide a flow of air into the area enclosed by the cover **2260** such that at least a portion of the electronic system **2700** disposed therein can be cooled.

FIGS. **10** and **11** illustrate the electronic system **2700** of the trolley **2100**. The electronic system **2700** includes a set of electronic devices that are collectively operated to control at least a portion of the trolley **2100**. As described above, the electronic system **2700** includes the collector **2770** that is coupled to a portion of the housing **2200** and that is placed in physical and/or electrical contact with the power rail **2620**. The collector **2770** can be any suitable shape, size, or configuration and can be formed from any suitable conductive material, such as, for example, iron, steel, or the like. In this manner, the collector **2770** can receive a flow of electrical current from the power rail **2620**. For example, as shown in FIG. **10**, the power rail **2620** is a substantially hollow tube that houses or substantially encloses one or more conductive portions **2621** (e.g., individual conductors or surfaces) that are electrically coupled to a power source (not shown). In this manner, the collector **2770** can be disposed within the hollow tube of the power rail **2620** such that a conductive portion **2771** (e.g., individual conductors, a conductive surface, or the like) of the collector **2770** is placed in electrical communication with the one or more conductive portions **2621** of the power rail **2620**. Thus, the collector **2770** receives a flow of current from the power source and transferred by the power rail **2620**. Moreover, the collector **2770** can be disposed within the power rail **2620** such that a coupling portion **2772** of the collector **2770** extends through a slot **2622** defined by the power rail **2620** to be coupled to the mounting portion **2235** of the housing **2200**. The coupling portion **2772** can further be coupled to a power module (not shown) of the trolley **2100**. Thus, the trolley **2100** receives power from the power source via the power rail **2620**.

While not shown in FIGS. **10** and **11**, the electronic system **2700** includes at least a processor, a memory, and a communication device. The memory can be, for example, a random access memory (RAM), a memory buffer, a hard drive, a read-only memory (ROM), an erasable programmable read-only memory (EPROM), and/or the like. In some embodiments, the memory stores instructions to cause the processor to execute modules, processes, and/or functions associated with controlling one or more mechanical and/or electrical systems included in the patient support system **2000**. For example, the memory can store instructions, information, and/or data associated with a proportion-integral-derivative (PID) control system. In some embodiments, the PID control system can be included in, for example, a software package. In some embodiments, the PID control can be a set of user controlled instructions executed by the processor that allow the user to “tune” the PID control, as described in further detail herein.

The processor of the electronic device can be any suitable processing device configured to run or execute a set of instructions or code. For example, the processor can be a general-purpose processor (GPU), a central processing unit (CPU), an accelerated processing unit (APU), and/or the like. The processor can be configured to run or execute a set of instructions or code stored in the memory associated with controlling one or more mechanical and/or electrical systems included in a patient support system. For example, the processor can run or execute a set of instructions or code associated with the PID control stored in the memory and further associated with controlling with a portion of the drive system **2300** and/or the patient support mechanism

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2500. More specifically, the processor can execute a set of instructions in response to receiving a signal from one or more sensors and/or encoders (shown and described below) that can control one or more subsequent actions of the drive system 2300 and/or the support mechanism 2500. Similarly stated, the processor can execute a set of instructions associated with a feedback loop that includes one or more sensors or encoders that send a signal that is at least partially associated with current and/or previous data (e.g., position, velocity, force, acceleration, or the like) received from the drive system 2300 and/or the support mechanism 2500, as described in further detail herein.

The communication device can be, for example, one or more network interface devices (e.g., network cards) configured to communicate with an electronic device over a wired or wireless network. For example, in some embodiments, a user can manipulate a remote control device that sends one or more signals to and/or receives one or more signals from the electronic system 2700 associated with the operation of the trolley 2100. The remote control can be any suitable device or module (e.g., hardware module or software module stored in the memory and executed in the process). For example, in some embodiments, the remote control can be an electronic device that includes at least a processor and a memory and that runs, for example, a personal computer application, a mobile application, a web page, and/or the like. In this manner, a user can engage the remote control to establish a set of system parameters associated with the support system 2000 such as, for example, the desired amount of body weight supported by the support system 2000.

As shown in FIG. 12, the drive system 2300 includes a first drive assembly 2310 and a second drive assembly 2400. The drive system 2300 is coupled to the first side 2211 of the base 2210 (see e.g., FIGS. 2 and 3) and arranged such that the first drive assembly 2310 and the second drive assembly 2400 are aligned (e.g., coaxial). In this manner, the first drive assembly 2310 and the second drive assembly 2400 can receive a portion of the support track 2050, as described in further detail herein.

FIGS. 13-23 illustrate the first drive assembly 2310. The first drive assembly 2310 includes a motor 2311, a support structure 2315, a set of guide wheel assemblies 2360, a set of drive wheel assemblies 2370, and a set of secondary wheel assemblies 2390. The motor 2311 is coupled to a side member 2320 of the support structure 2315 and is in electrical communication with a portion of the electronic system 2700. The motor 2311 includes an output shaft 2312 (see e.g., FIGS. 15 and 16) that engages a portion of one of the drive wheel assemblies 2370 to rotate a drive wheel 2385 included therein. More specifically, the motor 2311 receives an activation signal (e.g., a flow of electrical current) from the electronic system 2700 to cause the motor 2311 to rotate the output shaft 2312, which, in turn, rotates the drive wheel 2385. As shown in FIGS. 13 and 14, at least a portion of the first drive assembly 2310 is substantially symmetrical about a longitudinal plane (not shown) defined by the first drive assembly 2310. In this manner, each side of the first drive assembly 2310 includes similar components, thereby increasing versatility and decreasing manufacturing costs. For example, while the first drive assembly 2310 is shown including two side members 2320 with the motor 2311 being coupled to a particular side member 2320, in other embodiments, the motor 2311 can be coupled to the other side member 2320.

The support structure 2315 includes two side members 2320, a base 2340, two leading support members 2350, two

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trailing support members 2354, and two transverse support members 2358. As shown in FIGS. 13-16, the side members 2320 are the same (e.g., due to the symmetry of the first drive assembly 2310). The side members 2320 each define a bearing opening 2321, a notch 2322, and a set of slots 2325. The bearing opening 2321 of each side member 2320 receives a drive bearing 2376 (FIG. 20) included in the drive wheel assembly 2370. More specifically, the drive bearing 2376 can be disposed within the bearing opening 2321 such that an outer surface of the drive bearing 2376 forms a friction fit with a surface of the side member 2320 that defines the bearing opening 2321. Similarly stated, the drive bearing 2376 and the surface of the side 2320 defining the bearing opening 2321 form a press fit to retain the drive bearing 2376 within the bearing opening 2321.

The notch 2322 defined by each of the side members 2320 receives a spring rod 2323 and a spring 2324. The spring 2324 is disposed about the spring rod 2323 such that the spring rod 2323 substantially limits the motion of the spring 2324. More specifically, the spring rod 2323 is configured to allow the spring 2324 to move in an axial direction (e.g., compress and/or expand) while substantially limiting movement of the spring 2324 in a transverse direction. As described in further detail herein, the spring rod 2323 and the spring 2324 extend from a surface of the notch 2322 to engage a spring protrusion 2344 of the base 2340. The set of slots 2325 is configured such that each slot 2325 receives mounting hardware (e.g., a mechanical fastener, a pin, a dowel, etc.) configured to movably couple the side members 2320 to the base 2340, as described in further detail herein.

As described above, the base 2340 is movably coupled to the side members 2320. The base 2340 includes a set of sidewalls 2342, and an axle portion 2346. The axle portion 2346 of the base 2340 defines an opening 2347 that receives a transfer axle 2388 included in the drive wheel assembly 2370. More specifically, the transfer axle 2388 can rotate within the opening 2347 of the axle portion 2346 such that a rotational motion can be transferred from one of the drive assemblies 2370 to the other drive assembly 2370, as described in further detail herein.

The sidewalls 2342 each define a notch 2343 and include the spring protrusion 2344. More specifically, the spring protrusions 2344 each extend in a substantially perpendicular direction from the sidewalls 2342. As shown in FIGS. 13 and 14, when the side members 2320 are coupled to the base 2340, the notches 2322 of the side members 2320 each receive one of the spring protrusions 2344 of the base 2340. Similarly, when the side members 2320 are coupled to the base 2340, the notches 2343 defined by the base 2340 each receive a portion of one of the springs 2324. In this manner, the spring rod 2323 and the spring 2324 of each side member 2320 are aligned with the spring protrusion 2344 extending from the side walls 2342 of the base 2340 such that the spring 2324 is placed in contact with a surface of the corresponding spring protrusion 2344. With the side members 2320 movably coupled to the base 2340 (e.g., by disposing the mounting hardware in the slots 2325), the spring 2324 of each side member 2320 can dampen a movement of the side member 2320 relative to the base 2340. Similarly stated, the spring 2324 of each side member 2320 can engage the surface of the corresponding spring protrusion 2344 to exert a reaction force (e.g., brought on by a compression of the spring) in response to an external force (e.g., operational vibration, torque exerted by the motor, or the like) applied to one or both of the side members 2320.

FIGS. 17-19 illustrate one of each of the leading support members 2350, the trailing support members 2354, and the

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transverse support members **2358**, respectively. As described above, the symmetry of the first drive assembly **2310** is such that the two leading support member **2350** are the same, the two trailing support members **2354** are the same, and the two transverse support members **2358** are the same. The leading support members **2350** are each fixedly coupled to one of the side members **2320**. As shown in FIG. 17, the leading support members **2350** each define a lever arm notch **2355** that receives a lever arm **2391** of the secondary wheel assembly **2390**, a spring recess **2352** that receives a spring **2394** of the secondary wheel assembly **2390**, and a support track notch **2353** that receives, for example, a horizontal portion **2051** of the support track **2050** (see e.g., FIG. 23).

The trailing support members **2354** are each fixedly coupled to one of the side members **2320** and are disposed in a rearward position relative to the leading support members **2354**. Expanding further, the trailing support members **2354** are spaced apart from the leading support members **2354** at a distance sufficiently large to allow a portion of the drive wheel assemblies **2370** to be disposed therebetween. As shown in FIG. 18, the trailing support members **2354** each define a belt notch **2355** configured to receive a drive belt **2389** of the drive wheel assembly **2370** and a support track notch **2353** configured to receive the horizontal portion **2051** of the support track **2050** (e.g., as described with reference to the leading support member **2350**).

The transverse support members **2358** are each fixedly coupled to one of the leading support members **2350** and one of the trailing support members **2354**. Therefore, with the leading support members **2350** and the trailing support members **2354** each coupled to the corresponding side member **2320**, the transverse support member **2358** substantially encloses a space configured to house or receive a portion of the drive wheel assemblies **2370**. Furthermore, the arrangement of the support structure **2315** is such that a space defined between adjacent surfaces of the transverse support member **2358** is sufficiently large to receive, for example, a vertical portion **2052** of the support track **2050**.

As shown in FIG. 19, the transverse support member **2358** defines a bearing opening **2359** that receives a support bearing **2377** of the drive wheel assemblies **2370**. More specifically, the support bearing **2377** is disposed within the bearing opening **2359** such that an outer surface of the support bearing **2377** forms a friction fit with a surface of the transverse support member **2358** that defines the bearing opening **2359**. Similarly stated, the outer surface of the support bearing **2377** and the surface of the transverse support member **2358** form a press fit to retain the support bearing **2377** within the bearing opening **2359**.

Referring back to FIGS. 13-15, the first drive assembly **2310** includes four guide wheel assemblies **2360**. The guide wheel assemblies **2360** each include a mounting bracket **2361** and a guide wheel **2363**. More specifically, each of the guide wheels **2363** are rotatably coupled to one of the mounting brackets **2361** such that the guide wheels **2363** can rotate relative to the mounting brackets **2361**.

The guide wheel assemblies **2360** are each configured to be coupled to a portion of the support structure **2315**. Expanding further, as shown in FIGS. 13-16, the mounting bracket **2361** of each guide wheel assembly **2360** is coupled to one of the leading support members **2350** or one of the trailing support members **2354**. Similarly stated, both of the leading support members **2350** are coupled to the mounting bracket **2361** included in one of the guide wheel assemblies **2360** and both of the trailing support members **2354** are coupled to the mounting bracket **2361** included in one of the

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guide wheel assemblies **2360**. The guide wheel assemblies **2360** are coupled to the support structure **2315** such that a portion of the guide wheel **2363** extends into the space defined between the transverse members **2358**. In this manner, the guide wheels **2363** can roll along a surface of the vertical portion **2052** of the support track **2050** when the first drive assembly **2310** is coupled thereto (see e.g., FIG. 23).

As shown in FIGS. 13-15, the guide wheel assemblies **2360** can be arranged relative to the support structure **2315** such that the guide wheels **2363** included in the guide wheel assemblies **2360** that are coupled to the leading support member **2350** are disposed substantially below the mounting bracket **2361**. Conversely, the guide wheels **2363** included in the guide wheel assemblies **2360** that are coupled to the trailing support member **2350** are disposed substantially above the mounting bracket **2361**. This arrangement can increase the surface area of the vertical portion **2051** of the support track **2050** that is in contact with at least one guide wheel **2360**. In this manner, a rotational motion about a longitudinal centerline (not shown) of the support track **2050** can be minimized or eliminated. While shown in as being in a particular arrangement, in other embodiments, the guide wheels **2363** can be arranged in any suitable manner. For example, in some embodiments, all the guide wheels **2363** can be mounted below the mounting brackets **2361**. In other embodiments, all the guide wheels **2363** can be mounted above the mounting brackets **2361**. In still other embodiments, the guide wheels **2363** can be mounted to the mounting brackets **2361** in any combination of configurations (e.g., mounted above or below the mounting brackets **2361** in any suitable arrangement).

FIG. 20 is an exploded view of the drive wheel assembly **2370**. As described above, the symmetry of the first drive assembly **2310** is such that the drive wheel assemblies are the same. Thus, a discussion of the drive wheel assembly **2370** shown in FIG. 20 applies to both drive wheel assemblies **2370**. The drive wheel assembly **2370** includes a drive shaft **2371**, the drive bearing **2376**, the support bearing **2377**, a drive sprocket **2379**, a transfer sprocket **2381**, a drive wheel **2385**, the transfer axle **2388** (not shown in FIG. 20), and a drive belt **2389**. The drive shaft **2371** has a first portion **2372**, a second portion **2373**, and a third portion **2374** and defines an opening **2375**. The first portion **2372** has a first diameter that is at least partially associated with the drive sprocket **2378**. Expanding further, the drive sprocket **2378** defines an opening **2380** that has a diameter that is associated with the diameter of the first portion **2372** of the drive shaft **2371**. In this manner, the drive sprocket **2378** is disposed about the first portion **2372** of the drive shaft **2371** such that a surface of the drive sprocket **2378** defining the opening **2380** forms a friction fit with an outer surface of the first portion **2372** of the drive shaft **2371**. Similarly, the drive bearing **2376** is disposed about the first portion **2372** such that an inner surface of the bearing forms a friction fit with the outer surface of the second portion **2372** of the drive shaft **2371**. Thus, a rotation of the drive shaft **2371** within the drive bearing **2376** rotates the drive sprocket **2378**. Moreover, with the drive bearing **2376** being retained with the bearing opening **2321** of one of the side member **2370**, the drive shaft **2371** can be rotated relative to the corresponding side member **2370**, as described in further detail herein.

The second portion **2373** of the drive shaft **2371** has a second diameter that is smaller than the diameter of the first portion **2372** and that is at least partially associated with the drive wheel **2385**. Expanding further, the drive wheel **2385** includes a hub **2386** that defines an opening **2387** with a

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diameter that is associated with the diameter of the second portion 2373 of the drive shaft 2371. As shown in FIG. 20, the opening 2387 of the drive wheel 2385 includes a keyway configured to receive a key that extends from an outer surface of the second portion 2373 of the drive shaft 2371. In this manner, the drive wheel 2385 is fixedly disposed about the second portion 2373 of the drive shaft 2373.

The third portion 2374 of the drive shaft 2371 has a third diameter that is smaller than the diameter of the second portion 2372 and that is at least partially associated with the support bearing 2377. Expanding further, the support bearing 2377 is disposed about the third portion 2374 of the drive shaft 2371 such that an outer surface of the third portion 2374 forms a friction fit with an inner surface of the support bearing 2377. Moreover, with the support bearing 2377 being disposed within the bearing opening 2359 of the transverse support member 2358, the third portion 2374 of the drive shaft 2371 can be at least partially supported.

The opening 2375 defined by the drive shaft 2371 receives the output shaft 2312 of the motor 2311. More specifically, the drive shaft 2371 can be fixedly coupled, at least temporarily, to the output shaft 2312 of the motor 2311; thus, when the output shaft 2312 is rotated (e.g., in response to an activation signal from the electronic system 2700), the drive shaft 2371 is concurrently rotated. With the drive bearing 2376 and the support bearing 2377 being disposed within the bearing opening 2321 of the side member 2320 and the bearing opening 2359 of the transverse support member 2358, respectively, the drive shaft 2371 can rotate relative to the support structure 2315. Moreover, the rotation of the drive shaft 2371 rotates both the drive sprocket 2378 and the drive wheel 2385.

The drive sprocket 2378 is configured to engage the belt 2389. More specifically, the drive sprocket 2389 includes a set of teeth 2379 that engage a set of teeth (not shown) that extend from an inner surface of the belt 2389. The belt 2389 is further coupled the transfer sprocket 2381. The transfer sprocket 2381 includes a set of teeth 2382 that engage the teeth of the belt 2389. In this manner, the rotation of the drive sprocket 2378 (described above) rotates the belt 2389, which, in turn, rotates the transfer sprocket 2381. The transfer sprocket 2381 defines an opening 2383 configured to receive the transfer axle 2388 (see e.g., FIG. 16). More specifically, the transfer axle 2388 can be fixedly coupled to the transfer sprockets 2381 of each drive wheel assembly 2370 such that a rotation of the transfer sprocket 2381 of the first drive wheel assembly 2370 (e.g., the drive wheel assembly 2370 coupled to the output shaft 2312 of the motor 2311) rotates the transfer sprocket 2381 of the second drive wheel assembly 2370. Thus, when the motor 2311 is activated to rotate the output shaft 2312, both the drive wheels 2385 of both the drive wheel assemblies 2370 are urged to rotate.

In some embodiments, the side members 2320 and the base 2340 of the support structure 2315 can be arranged such that the spring 2324 of the side members 2320 is in a preloaded configuration (e.g., partially compressed without an additional external force being applied to one or both of the side members 2320). More specifically, each spring 2324 can exert a force (e.g., due to the preload) on the surface of the corresponding spring protrusion 2344 of the base 2340 to place the corresponding side member 2320 in a desired position relative to the base 2340. Moreover, with the drive bearings 2376 fixedly disposed within the bearing opening 2321 of the corresponding side members 2320 and with the transfer axle 2388 being disposed within the opening 2347 defined by the axle portion 2346 of the base 2340, the belt

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2379 disposed about the drive sprocket 2378 and the transfer sprocket 2381 can be placed in tension. Thus, the arrangement of the side members 2320 being movably coupled to the base 2340 can retain the belt 2379 in a suitable amount tension such that the belt 2379 does not substantially slip along the teeth 2379 of the drive sprocket 2378 and/or along the teeth 2382 of the transfer sprocket 2381.

As shown in FIG. 21, the first drive assembly 2310 includes the secondary wheel assembly 2390. The secondary wheel assembly 2390 includes a lever arm 2391, a secondary wheel 2393, and a spring 2394. The lever arm 2391 is a substantially angled member that includes an axle portion 2392, a pivot portion 2395, and an engagement portion 2396. The axle portion 2392 is disposed at a first end of the lever arm 2391 and is movably coupled to the secondary wheel 2393 such that the secondary wheel 2393 rotates about the axle portion 2392. The pivot portion 2395 is movably coupled to a portion of the leading support member 2350 that defines the lever arm notch 2351. For example, in some embodiments, the pivot portion 2395 of the lever arm 2391 can include an opening configured to receive, for example, a pivot pin (not shown) included in the leading support member 2350. In this manner, the pivot pin can define an axis about which the pivot portion 2395 can pivot or rotate.

The engagement portion 2396 is configured to engage a portion of the spring 2394. More specifically, as shown in FIG. 22, a first end portion of the spring 2394 is in contact with the spring recess 2352 defined by the leading support member 2350 and a second end portion of the spring 2394 is in contact with the engagement portion 2396. In this manner, the spring 2394 can exert a force on the engagement portion 2396 to pivot the lever arm 2391 about the pivot portion 2395. Expanding further, as shown in FIG. 22, the force exerted by the spring 2394 can pivot the lever arm 2391 such that the secondary wheel 2393 is pivoted towards the drive wheel 2385. Therefore, when the first drive assembly 2310 is disposed about the support track 2050, the secondary wheel 2393 can be placed in contact with a bottom surface of the horizontal portion 2051 of the support track 2050. Moreover, the force exerted by the spring 2394 can be such that the drive wheel 2385 and the secondary wheel 2393 exert a compressive force on a top surface and the bottom surface, respectively, of the horizontal portion 2051 of the support track 2051. This arrangement can, for example, increase the friction between the drive wheel 2385 and the horizontal portion 2051 of the support track 2050.

FIGS. 24-26 illustrate the second drive assembly 2400. The second drive assembly 2400 can function similarly to the first drive assembly 2310, thus, some portions of the second drive assembly 2400 are not described in further detail herein. The second drive assembly 2400 includes a support structure 2405, a set of guide wheel assemblies 2430, a set of primary wheel assemblies 2440, a coupler 2460, and an encoder 2470. As shown, at least a portion of the second drive assembly 2400 is substantially symmetrical about a longitudinal plane (not shown) defined by the second drive assembly 2400. In this manner, each side of the second drive assembly 2400 includes similar components, thereby increasing versatility and decreasing manufacturing costs. For example, while the second drive assembly 2400 is shown including two side members 2420 with the coupler 2460 and encoder 2470 being coupled to a particular side member 2420, in other embodiments, the coupler 2460 and encoder 2470 can be coupled to the other side member 2420.

The support structure 2405 includes two side members 2410, a base 2420, a set of leading support members 2431,

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a set of trailing support members **2432**, and a set of transverse support members **2433**. As shown in FIGS. **24-26**, the side members **2410** are the same (e.g., due to the symmetry of the first drive assembly **2400**). The side members **2410** each define a bearing opening **2411** that receives a bearing **2454** (FIG. **25**) included in the drive wheel assembly **2470**. More specifically, the bearing **2454** can be disposed within the bearing opening **2411** such that an outer surface of the drive bearing **2454** forms a friction fit with a surface of the side member **2410** that defines the bearing opening **2411**. Similarly stated, the drive bearing **2454** and the surface of the side **2410** defining the bearing opening **2411** form a press fit to retain the drive bearing **2454** within the bearing opening **2411**.

The base **2420** is configured to be fixedly coupled to the side members **2410**. The base **2420** includes a mounting plate **2421** configured to extend from a top surface and from a bottom surface of the base **2420** to couple the second drive assembly **2400** to the base **2210** of the housing **2200** (e.g., via any suitable mounting hardware such as, for example, mechanical fasteners or the like). The arrangement of the mounting plate **2421** can be such that when the second drive assembly **2400** is disposed about the support track **2050**, the mounting plate **2421** can substantially limit a movement of the second drive mechanism **2400** in transverse direction relative to the longitudinal centerline (not shown) of the support track **2050**. In some embodiments, the mounting plate **2421** can include any suitable surface finish that can be sufficiently smooth to slide along a bottom surface of the horizontal portion **2051** of the support track **2050**. In other embodiments, the mounting plate **2421** can be formed from a material such as, for example, nylon or the like that facilitates the sliding of the mounting plate **2421** along the bottom surface of the support track **2050**.

The leading support members **2431**, the trailing support members **2432**, and the transverse support members **2433** can be arranged similar to the leading support members **2350**, the trailing support members **2354**, and the transverse support members **2358** described above with reference to FIGS. **17-19**. In this manner, the side members **2410** and the support members **2431**, **2432**, and **2433** can define a space configured to substantially enclose at least a portion of the primary wheel assemblies **2440**. Moreover, the transverse support members **2433** can define an opening configured to receive a bearing **2454** of the primary wheel assembly **2350** in a similar manner as the transverse member **2333** described above. As shown in FIGS. **24-26**, the leading support members **2431**, the trailing support members **2432**, and the transverse support members **2433** can differ, however, in that the leading support members **2431**, the trailing support members **2432**, and the transverse support members **2433** need not include one or more notches and/or recesses to accommodate any portion of the second drive assembly **2400**.

The second drive assembly **2400** includes four guide wheel assemblies **2440**. The guide wheel assemblies **2440** each include a mounting bracket **2441** and a guide wheel **2443**. More specifically, each of the guide wheels **2443** are rotatably coupled to one of the mounting brackets **2441** such that the guide wheels **2443** can rotate relative to the mounting brackets **2441**. The guide wheel assemblies **2440** are each configured to be coupled to a portion of the support structure **2405**. Expanding further, as shown in FIGS. **24-26**, the mounting bracket **2441** of each guide wheel assembly **2440** is coupled to one of the leading support members **2431** or one of the trailing support members **2432**. Similarly stated, both of the leading support members **2431** are

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coupled to the mounting bracket **2441** included in one of the guide wheel assemblies **2440** and both of the trailing support members **2432** are coupled to the mounting bracket **2441** included in one of the guide wheel assemblies **2440**. The guide wheel assemblies **2440** are coupled to the support structure **2405** such that a portion of the guide wheel **2443** extends into the space defined between the transverse members **2433**. In this manner, the guide wheels **2443** can roll along a surface of the vertical portion **2052** of the support track **2050** when the second drive assembly **2400** is coupled thereto (see e.g., FIG. **26**). As described above with reference to the first drive assembly **2310**, the guide wheel assemblies **2440** can be arranged in any suitable configuration to limit a rotational movement of the second drive assembly **2400** about the longitudinal centerline of the support track **2050**.

The primary wheel assemblies **2450** each include a primary wheel **2451** having a hub **2452** and an axle **2453**, and the bearings **2454**. As described above, the axle **2453** can be disposed within the bearings **2354** while the bearings **2354** are coupled to the side members **2410** and the transverse members **2433**. In this manner, each primary wheel **2451** can rotate about the corresponding axle **2453** relative to the support structure **2405**. As shown in FIG. **26**, the second drive assembly **2400** is disposed about the support track **2050** such that the primary wheels **2451** roll along the top surface of the horizontal portion **2051**. Similarly, the guide wheels **2443** roll along a surface of the vertical portion **2052** of the support track **2050**.

As shown in FIGS. **24** and **26**, the axle **2453** is configured to extend through the bearing **2454** disposed within the opening **2411** of the side members **2410**. In this manner, the coupler **2460** can couple to the axle **2453** to couple the axle **2453** to the encoder **2470**. Thus, the encoder **2470** can receive and/or determine information associated with the rotation of the primary wheel **2451**. For example, the encoder **2470** can determine position, rotational velocity, rotational acceleration, or the like. Furthermore, the encoder **2470** can be in electrical communication (e.g., via a wired communication or a wireless communication) with a portion of the electronic system **2700** and can send information associated with the second drive assembly **2400** to the portion of the electronic system **2700**. Upon receiving the information from the encoder **2470**, a portion of the electronic system **2700** can send a signal to any other suitable system associated with performing an action (e.g., increasing or decreasing the power of one or more motors or the like), as described in further detail herein. In some instances, the electronic system **2700** can determine the position of the trolley **2100** relative to the support track **2050** based at least in part on the information sent from the encoder **2470** associated with the second drive assembly **2400**. In such instances, a user (e.g., doctor, physician, nurse, technician, or the like) can input a set of parameters associated with a portion of the support track **2050** along which the trolley **2100** moves. In this manner, the user can define a desired path along the support track **2050** for a therapy session.

FIGS. **27-33** illustrate the support mechanism **2500** included in the trolley **2100**. As shown in FIG. **27**, the support mechanism **2500** includes a tether **2505**, a winch assembly **2510**, a guide mechanism **2540**, a first pulley **2563**, a second pulley **2565**, and a cam mechanism **2570**. The tether **2505** can be, for example, a rope or other long flexible member that can be formed from any suitable material such as nylon or other suitable polymer. The tether **2505** includes a first end portion **2506** that is coupled to a portion of the winch assembly **2510** and a second end portion **2507** that

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can be coupled to any suitable patient attachment mechanism such as, for example, the patient attachment mechanism **2800** shown in FIG. **34**. The tether **2505** is configured to engage a portion of the winch assembly **2510**, the guide mechanism **2540**, the cam mechanism **2570**, the first pulley **2563**, and the second pulley **2565** such that the support mechanism **2500** actively supports at least a portion of the body weight of a patient, as described in further detail herein.

As shown in FIGS. **29** and **30**, the winch assembly **2510** includes a motor **2511**, a mounting flange **2515**, a coupler **2520**, a drum **2525**, and encoder assembly **2530**. The motor **2511** is coupled to the coupler **2520** and is in electrical communication with a portion of the electronic system **2700**. The motor **2511** includes an output shaft **2512** that engages an input portion (not shown) of the coupler **2520** such that rotation of the output shaft **2512** of the motor **2511** rotates an output member **2521** of the coupler **2520**. More specifically, the motor **2511** receives an activation signal (e.g., a flow of electrical current) from the electronic system **2700** to cause the motor **2511** to rotate the output shaft **2512** in a first rotational direction or in a second rotational direction, opposite the first rotational direction. The output shaft **2512**, in turn, rotates the output member **2521** of the coupler **2520** in the first rotational direction or the second rotational direction, respectively.

The mounting flange **2515** is disposed about a portion of the coupler **2520** and includes a portion that can be coupled to the third side member **2250** of the housing **2200**. In this manner, the motor **2511** is supported by the mounting flange **2515** and the housing **2200**. The output member **2521** of the coupler **2520** is coupled to a mounting plate **2522** of the drum **2525** such that when the output shaft **2512** of the motor **2511** is rotated in the first direction or the second direction, the drum **2525** is rotated in first direction or the second direction, respectively. While not shown, in some embodiments, the coupler **2520** can include one or more gears that can be arranged in any suitable manner to define a desirable gear ratio. In this manner, the rotation of the output shaft **2512** can be in the first direction or the second direction with a first rotational velocity and the rotation of the drum **2525** can be in the first direction or the second direction, respectively, with a second rotational velocity that is different from the first rotational velocity of the output shaft **2512** (e.g., a greater or lesser rotational velocity). In some embodiments, the coupler **2520** can include one or more clutches that can be configured to reduce and/or dampen an impulse (i.e., a force) that can result from the electronic system **2700** sending a signal to the motor **2511** that is associated with changing the rotational direction of the output shaft **2512**.

The drum **2525** is disposed between the mounting plate **2522** and an end plate **2529**. As described in further detail herein, an encoder drum **2531** of the encoder assembly **2530** is coupled to the end flange **2529** such that at least a portion of the encoder assembly **2530** is disposed within an inner volume **2528** defined by the drum **2525**. The drum **2525** has an outer surface **2526** that defines a set of helical grooves **2527**. The helical grooves **2527** receive a portion of the tether **2505** and define a path along which the tether **2505** can wrap to coil and/or uncoil around the drum **2525**. For example, the motor **2511** can receive a signal from the electronic system **2700** to rotate the output shaft **2512** in the first direction. In this manner, the drum **2525** is rotated in the first direction and the tether **2505** can be, for example, coiled around the drum **2525**. Conversely, the motor **2511** can receive a signal from the electronic system **2700** to rotate the output shaft **2512** in the second direction, thus, the drum is

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rotated in the second direction and the tether **2505** can be, for example, uncoiled from the drum **2525**.

The encoder assembly **2530** includes the encoder drum **2531**, a mounting flange **2532**, a bearing bracket **2533**, a bearing **2535**, a coupler **2536**, an encoder **2537**, and an encoder housing **2538**. As described above, a first end portion of the encoder drum **2531** is coupled to the end flange **2529** of the drum **2525** such that a portion of the encoder assembly **2530** is disposed within the inner volume **2528** of the drum **2525**. The mounting flange **2532** is coupled to a second end portion of the encoder drum **2531** and is further coupled to the bearing bracket **2533**. The bearing bracket **2533** includes an axle **2534** about which the bearing **2535** is disposed. The coupler **2536** is coupled to the axle **2534** of the bearing bracket **2533** and is configured to couple the encoder **2537** to the bearing bracket **2533**. As shown in FIG. **28**, the coupler **2536** and the encoder **2537** are disposed within the encoder housing **2538**. More specifically, the coupler **2536** is movably disposed within the encoder housing **2538** and the encoder **2537** is fixedly coupled to the encoder housing **2538**. Moreover, a first end portion of the encoder housing **2538** is disposed about the bearing **2535** and a second end portion of the encoder housing **2538** is in contact with and fixedly coupled to the recessed portion **2244** of the second side member **2240** of the housing **2240**. In this manner, the encoder drum **2531**, the mounting flange **2532**, the bearing bracket **2533**, and the coupler **2536** are configured to rotate concurrently with the drum **2525**, relative to the encoder **2537** and the encoder housing **2538**. Thus, the encoder **2537** can receive and/or determine information associated with the rotation of the drum **2525**. For example, the encoder **2537** can determine position, rotational velocity, rotational acceleration, feed rate of the tether **2505**, or the like. Furthermore, the encoder **2537** can be in electrical communication (e.g., via a wired communication or a wireless communication) with a portion of the electronic system **2700** and can send information associated with the winch assembly **2510** to the portion of the electronic system **2700**. Upon receiving the information from the encoder **2537**, a portion of the electronic system **2700** can send a signal to any other suitable system associated with performing an action (e.g., increasing or decreasing the power of one or more motors or the like), as described in further detail herein.

Referring back to FIG. **27**, the guide mechanism **2540** of the support mechanism **2500** is at least partially disposed within the guide mechanism opening **2215** of the base **2210** included in the housing **2200**. More specifically, the guide mechanism **2540** includes a set of mounting brackets **2541** that are coupled to the mounting tabs **2216** of the base **2210**. In this manner, at least a portion of the guide mechanism **2540** is suspended within the guide mechanism opening **2215**. As shown in FIG. **31**, the guide mechanism **2540** includes the mounting brackets **2541**, a guide drum assembly **2545**, a stopper bracket **2550**, a stopper **2551**, a roller assembly **2554**, a coupler **2559**, a support bracket **2560**, and an encoder **2561**. As described above, the mounting brackets **2541** are coupled to the mounting tabs **2216** of the base **2210**. The mounting brackets **2541** each include a first mounting portion **2542** that is movably coupled to a portion of the guide drum assembly **2545**, a second mounting portion **2543** that is fixedly coupled to the stopper bracket **2550**, and a pivot portion **2544** that is movably coupled to a portion of the roller assembly **2554**. The stopper bracket **2550** is further coupled to the stopper **2551** and is configured to limit a movement of the guide drum assembly **2545** relative to the mounting brackets **2541**.

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The guide drum assembly **2545** includes a guide drum **2546**, a set of pivot plates **2547**, and a stopper plate **2549**. The guide drum **2546** is movably coupled to the pivot plates **2547**. For example, while not shown in FIG. **31**, the pivot plates **2547** can each include an opening configured to receive an axle about which the guide drum **2546** can rotate. The pivot plates **2547** each include a pivot axle **2548** that can be disposed within an opening (not shown) defined by the first mounting portion **2542** of the mounting brackets **2541**. In this manner, the guide drum assembly **2545** can pivot about the pivot axles **2548** relative to the mounting brackets **2541**. The stopper plate **2549** is coupled to the pivot plates **2547** and is configured to engage a portion of the stopper **2551** to limit the pivoting motion of the guide drum assembly **2545** relative to the mounting brackets **2541**. More specifically, with the stopper bracket **2550** fixedly coupled to the mounting brackets **2541** and to the stopper **2551**, the guide drum assembly **2545** can pivot toward the stopper bracket **2550** (e.g., in response to a force exerted on tether **2505**, as described in further detail herein) such that the stopper plate **2549** is placed in contact with the stopper **2551**. The stopper **2551** can be any suitable shape, size, or configuration. For example, in some embodiments, the stopper **2551** can be an elastomeric member configured to absorb a portion of a force exerted by the guide drum assembly **2545** when the stopper plate **2549** is placed in contact with the stopper **2551**.

The roller assembly **2554** includes a set of swing arms **2555** and a set of rollers **2558**. The swing arms **2555** include a first end portion **2556** and a second end portion **2557**. The first end portion **2556** of the swing arms **2555** are movably coupled to the rollers **2558**. More specifically, the rollers **2558** can be arranged such that a spaced defined between the rollers **2558** can receive a portion of the tether **2505**. Thus, when the tether **2505** is moved relative to the rollers **2558**, the rollers **2558** can rotate relative to the swing arms **2555**. The second end portion **2557** of the swing arms **2555** are coupled to the pivot portion **2543** of the mounting brackets **2541**. For example, as shown in FIG. **31**, the pivot portion **2543** can include a set of axles disposed within a bearing. In this manner, the second end portion **2557** of the swing arms **2555** can couple to the axles such that the roller assembly **2554** and the axles can pivot relative to the mounting brackets **2541** (e.g., in response to a force exerted on tether **2505**, as described in further detail herein).

The coupler **2559** included in the guide mechanism **2540** is coupled to the axle of the pivot portion **2543** of one of the mounting brackets **2541**. The coupler **2559** is further coupled to an input shaft of the encoder **2561**. More specifically, the support bracket **2560** is coupled to the base **2210** of the housing **2200** and is also coupled to a portion of the encoder **2561** to limit the movement of a portion of the encoder **2561** relative to the base **2210**. Thus, the encoder **2561** can receive and/or determine information associated with the pivoting motion of the roller assembly **2554** relative to the mounting brackets **2541**. For example, the encoder **2561** can determine position, rotational velocity, rotational acceleration, feed rate of the tether **2505**, or the like. Furthermore, the encoder **2561** can be in electrical communication (e.g., via a wired communication or a wireless communication) with a portion of the electronic system **2700** and can send information associated with the guide mechanism **2540** to the portion of the electronic system **2700**. Upon receiving the information from the encoder **2561**, a portion of the electronic system **2700** can send a signal to any other suitable system associated with performing an action (e.g., increasing or decreasing the power of one

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or more motors **2311** and **2511**, changing the direction of one or more of the motors **2311** and **2511**, or the like).

As shown in FIG. **32**, the first pulley **2563** and the second pulley **2565** are rotatably coupled to a first pulley bracket **2564** and a second pulley bracket **2565**, respectively. The first pulley bracket **2564** and the second pulley bracket **2565** are further coupled to the base **2210** of the housing **2200**. In this manner, the first pulley **2563**, the second pulley **2565**, and at least a portion of the cam mechanism **2570** can be engaged by the tether **2505** to provide a mechanical advantage to the winch assembly **2510**, as described in further detail herein.

As shown in FIGS. **32** and **33**, the cam mechanism **2570** includes a cam pulley assembly **2571**, a cam **2580**, a coupler **2585**, a coupler housing **2586**, an encoder **2587**, and a bias mechanism **2588**. The cam pulley assembly **2571** includes a cam pulley **2572**, a cam arm **2574**, a cam axle **2575**, and a spacer **2576**. The cam arm **2574** includes a first end portion that is rotatably coupled to the cam pulley **2572** and a second end portion that is rotatably coupled to the cam axle **2575**. The cam axle **2575** extends through the cam pivot opening **2220** (defined by the base **2210**), the spacer **2576**, and the cam **2580** to be coupled to the coupler **2585**. The spacer **2576** is coupled to the base **2210** and is disposed between the second side **2212** of the base **2210** and a surface of the cam **2580**. The spacer **2576** can be formed from a material having a relatively low friction coefficient such as, for example, polyethylene, nylon, or the like to allow the cam **2580** to move relatively easily along a surface of the spacer **2576**. In this manner, the cam **2580** is spaced a sufficient distance from the second side **2212** of the base **2210** to allow a portion of the bias mechanism **2588** to be disposed therebetween, as described in further detail herein.

The cam **2580** of the cam assembly **2570** defines an opening **2581**, and includes a mounting portion **2582** and an engagement surface **2583**. The engagement surface **2583** of the cam **2580** is in contact with a portion of the bias mechanism **2588**, as described in further detail herein. The opening **2581** defined by the cam **2580** receives a bearing **2584**. When disposed within the opening **2581**, the bearing **2584** allows the cam **2580** to rotate about the cam axle **2575**. The mounting portion **2582** of the cam **2580** is at least partially disposed within the cam pulley opening **2219** and is coupled to the cam pulley **2572**. For example, as shown in FIG. **33**, the mounting portion **2582** is a threaded rod extending from a surface of the cam **2580** that can be received by a threaded opening (not shown) defined by the cam pulley **2572**. In this manner, movement of the cam pulley assembly **2571**, in response to a change in force exerted on the tether **2505** (e.g., an increase or a decrease of force), rotates the cam **2580** about the cam axle **2575** (as described above).

The coupler housing **2586** is coupled to a surface of the cam **2580** that is opposite the side adjacent to the spacer **2576**. In other words, the coupler housing **2586** extends away from the base **2210** when coupled to the cam **2580**. The coupler housing **2586** is further coupled to the encoder **2587**. Thus, when the cam **2580** is rotated about the cam axle **2575**, the coupler housing **2586** and the encoder **2587** are also rotated about the cam axle **2575**. The coupler **2585** is disposed within the coupler housing **2586** and is coupled to both the cam axle **2575** and an input portion (not shown) of the encoder **2587**. Therefore, with the coupler **2585** coupled to the cam axle **2575** and the input portion of the encoder **2587**, the rotation of the cam **2580** and the coupler housing **2586** rotates the encoder **2587** about its input portion. In this manner, the encoder **2587** can receive and/or determine

information associated with the pivoting motion of the cam **2580** and/or the cam pulley assembly **2571** relative to the cam axle **2575**. For example, the encoder **2587** can determine position, rotational velocity, rotational acceleration, feed rate of the tether **2505**, or the like. Furthermore, the encoder **2587** can be in electrical communication (e.g., via a wired communication or a wireless communication) with a portion of the electronic system **2700** and can send information associated with the cam mechanism **2570** to the portion of the electronic system **2700**. Upon receiving the information from the encoder **2587**, a portion of the electronic system **2700** can send a signal to any other suitable system associated with performing an action (e.g., increasing or decreasing the power of one or more motors **2311** and **2511**, changing the direction of one or more of the motors **2311** and **2511**, or the like).

The bias mechanism **2588** includes an axle **2589**, a mounting flange **2590**, a first pivot arm **2591**, a second pivot arm **2595**, a guide member **2596**, a bias member **2597**, and a mounting post **2598**. The axle **2589** is movably disposed within the mounting flange **2588** and is configured to extend through the bias mechanism opening **2217** defined by the base **2210** to be fixedly disposed within an axle opening **2592** defined by the second pivot arm **2591**. Expanding further, a portion of the mounting flange **2589** extends through the bias mechanism opening **2217** and beyond the second side **2212** of the base **2210** to be in contact with a surface of the second pivot arm **2591**. In this manner, the surface of the second pivot arm **2591** is offset from the second side **2212** of the base **2210**. Moreover, the arrangement of the spacer **2576** (described above) is such that when the axle **2589** is disposed within the axle opening **2592**, a second surface of the first pivot arm **2591** is offset from a surface of the cam **2580**. Thus, the first pivot arm **2591** can pivot relative to the base **2210** with a relatively low amount of friction. In some embodiments, at least the portion of the mounting flange **2590** that extends through the bias mechanism opening **2217** can be made from a material having a relatively low coefficient of friction such as, for example, polyethylene, nylon, or the like.

The first pivot arm **2591** defines the axle opening **2592** and a guide member opening **2593**, and includes an engagement member **2594**. The guide member opening **2593** is configured to receive a portion of the guide member **2596** to couple the guide member **2596** to the first pivot arm **2591**. The guide member **2596** extends from a surface of the first pivot arm **2591** toward the base **2210** such that a portion of the guide member **2596** extends through the guide member opening **2218** defined by the base **2210**. In some embodiments, the guide member **2596** can include a sleeve or the like configured to engage the base **2210**. In such embodiments, the sleeve can be formed from a material having a relatively low friction coefficient such as, for example, polyethylene, nylon, or the like. Thus, the guide member **2596** can move within the guide member track **2218** when the first pivot arm **2591** is moved relative to the base **2210**.

The engagement member **2594** of the first pivot arm **2591** extends from a surface of the first pivot arm **2591** toward the cam **2580**. In this manner, the engagement member **2594** can be moved along the engagement surface **2583** of the cam **2580** when the cam **2580** is moved relative to the base **2210**, as described in further detail herein. In some embodiments, the engagement member **2594** can be rotatably coupled to the first pivot arm **2591** and can be configured to roll along the engagement surface **2583**. In other embodiments, the engagement member **2594** and/or the engagement surface **2583** can be formed from a material having a relatively low

friction coefficient. In such embodiments, the engagement member **2594** can be slid along the engagement surface **2583**.

The second pivot arm **2595** of the bias mechanism **2588** has a first end portion that is fixedly coupled to the axle **2589** and a second end portion that is coupled to a first end portion of the bias member **2597**. The mounting post **2598** is fixedly coupled to the base **2210** and is further coupled to a second end portion of the bias member **2597**. Therefore, the second pivot arm **2595** can pivot relative to the mounting flange **2590** between a first position, where the bias member **2597** is in a first configuration (undeformed configuration), and a second position, where the bias member **2597** is in a second configuration (deformed configuration). For example, in some embodiments, the bias member **2597** can be a spring that can be moved between an uncompressed configuration (e.g., the first configuration) and a compressed configuration (e.g., the second configuration). In other embodiments, the bias member **2597** can be a spring that can be moved between an unexpanded and an expanded configuration. In other words, the bias member **2597** can be either a compression spring or an expansion spring, respectively. In still other embodiments, the bias member **2597** can be any other suitable biasing mechanism and/or energy storage device such as, for example, a gas strut or the like.

When the cam **2580** is rotated from a first position to a second position in response to a force exerted on the tether **2505** (as described above), the bias member **2597** can exert a reaction force that resists the rotation of the cam **2580**. More specifically, with the engagement member **2594** in contact with the engagement surface **2583** of the cam **2580**, the bias member **2587** exerts the reaction force that resists the movement of the engagement member **2594** along the engagement surface **2583**. Therefore, in some instances, relatively small changes in the force exerted on the tether **2505** may not be sufficiently large to rotate the cam **2580** and the cam pulley assembly **2571**. This arrangement can reduce undesirable changes in the amount of body weight supported by the support system **2000** in response to minor fluctuations of force exerted on the tether **2505**.

FIG. **34** illustrates the patient attachment mechanism **2800**. The patient attachment mechanism **2800** can be mated with the second end portion **2507** of the tether **2505** to couple the patient attachment mechanism **2800** to the trolley **2100**. Moreover, the patient attachment mechanism **2800** can be coupled to a harness or the like, worn by the patient, to couple the patient to the support system **2000**, as described below.

The patient attachment mechanism **2800** has a first coupling portion **2810** and a second coupling portion **2812**. The first coupling portion **2810** includes a coupling mechanism **2811** configured to couple to the second end portion **2507** of the tether, as described above. For example, the coupling mechanism **2811** can be a loop or hook configured to couple to an attachment device of the tether **2505** (not shown in FIGS. **2-34**). The second coupling portion **2821** is movably coupled to a first arm **2820** and a second arm **2840**. As described in further detail herein, the first **2820** and the second arm **2840** can pivot relative to each other to absorb at least a portion of a force exerted by the weight of a patient coupled to the patient attachment mechanism **2800**.

The first arm **2820** of the patient attachment mechanism **2800** includes a pivot portion **2821** and a mount portion **2822**. The pivot portion **2821** is movably coupled to the second coupling portion **2812**. The mount portion **2822** receives a guide rod **2830**, as described in further detail herein. The first arm **2820** defines a slot **2824** that receives

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a portion of the second arm **2840** and an opening **2826** that receives a portion of a harness worn by the patient.

The second arm **2840** has a pivot portion **2841** and a coupling portion **2842**. The pivot portion **2841** is movably coupled to the second coupling portion **2812**. In this manner, both the first arm **2820** and the second arm **2840** can pivot relative to the coupling portion **2812** and relative to each other, as described in further detail herein. The coupling portion **2842** defines an opening **2843** that receives a portion of the harness worn by the patient. The coupling portion **2842** is also movably coupled to a first end portion of a first energy storage member **2844** and a first end portion of a second energy storage member **2851** (collectively referred to as energy storage member **2850**). The energy storage members **2850** can be, for example, gas struts or the like.

As shown in FIG. **34**, the energy storage members **2850** are configured to extend towards the first arm **2820**. More specifically, the second energy storage member **2851** includes a coupling portion **2852** that is movably coupled to the guide rod **2830** of the first arm **2820**. The first energy storage member **2844** also includes a coupling portion (not shown in FIG. **34**) that is movably coupled to an engagement member **2845** and further coupled to the coupling portion **2852** of the second energy storage member **2851**. Similarly stated, the coupling portion of the first energy storage member **2844** extends in a substantially perpendicular direction relative to a longitudinal centerline (not shown) of the first energy storage member **2844**.

The engagement member **2845** is movably coupled to the coupling portion of the first energy storage member **2844** and the coupling portion **2852** of the second coupling portion **2851**. The engagement member **2845** is configured to be placed in contact with an engagement surface **2825** of the first arm **2820** that at least partially defines the slot **2825**. Similarly stated, the engagement member **2845** is disposed within the slot **2824** defined by the first arm **2820** and in contact **2825** with the engagement surface **2825**. Moreover, the arrangement of the engagement member **2845** and the energy storage members **2850** allows the engagement member **2845** to roll along the engagement surface **2825**.

When a force is exerted on the first arm **2820** the second arm **2840** by the patient, the first arm **2820** and the second arm **2840** pivot about the second coupling portion **2812** towards one another. The pivoting of the first arm **2820** and the second arm **2840** moves the engagement member **2845** along the engagement surface **2825** and further moves the energy storage members **2850** for a configuration of lower potential energy to a configuration of higher potential energy (e.g., compresses a gas strut). Thus, the energy storage members **2850** can absorb at least a portion of a force exerted of the patient attachment mechanism **2800**. Moreover, when the force exerted on the patient attachment mechanism **2800** is less than the potential energy of the energy storage members **2850** in the second configuration, the energy storage members **2850** can move towards their first position to pivot the first arm **2820** and the second arm **2840** away from one another.

In use, the patient support system **2000** can be used to actively support at least a portion of the body weight of a patient that is coupled thereto. For example, in some instances, a patient is coupled to the patient attachment mechanism **2800**, which, in turn, is coupled to the second end portion **2507** of the tether **2505**, as described above. In this manner, the support system **2000** (e.g., the tether **2505**, the trolley **2100**, and the support rail **2050**) can support at least a portion of the body weight of the patient.

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In some instances, a user (e.g., a technician, a therapist, a doctor, a physician, or the like) can input a set of system parameters associated with the patient and the support system **2000**. For example, in some embodiments, the user can input a set of system parameters via a remote control device such as, for example, a personal computer, a mobile device, a smart phone, or the like. In other embodiments, the user can input system parameters on, for example, a control panel included in or on the trolley **2100**. The system parameters can include, for example, the body weight of the patient, the height of the patient, a desired amount of body weight to be supported by the support system **2000**, a desired speed of the patient walking during gait therapy, a desired path or distance along the length of the support track **2050**, or the like.

With the system parameters entered, the patient can begin, for example, a gait therapy session. In some instances, the trolley **2100** can move along the support structure **2050** (as described above with reference to FIGS. **23** and **26**) in response to the movement of the patient. Similarly stated, the trolley **2100** can move along the support structure **2050** as the patient walks. In some instances, the trolley **2100** can be configured to remain substantially over-head of the patient. In such instances, the electronic system **2700** can execute a set of instructions associated with controlling the motor **2311** of the drive system **2300** based on information received from, for example, the encoder **2470** of the drive system **2300**, the encoder **2561** of the guide mechanism **2540**, and/or the encoder **2587** of the cam assembly **2570**. For example, the electronic system **2700** can send a signal to the motor **2311** of the drive system **2300** operative in changing the rotational velocity of the drive wheels **2385** based at least in part on information associated with the encoder **2561** of the guide mechanism **2540**. Expanding further, in some instances, the patient may walk faster than the trolley **2100**, thereby changing the angle of the tether **2505** and the guide mechanism **2540** relative to the base **2210**. Thus, the encoder **2561** of the guide mechanism **2540** can send a signal associated with the angle of the guide mechanism **2540** relative to the base **2210** and upon receiving the signal, the electronic system **2700** can send a signal to the motor **2311** of the drive system **2300** to increase the rotational velocity of the drive wheels **2385**. In this manner, the position of the trolley **2100** relative to the patient can be actively controlled based at least in part on a user defined parameter and further based at least in part on information received from the encoder **2470** of the drive system **2300**, the encoder **2561** of the guide mechanism **2540**, and/or the encoder **2587** of the cam assembly **2570**. Although described as being actively controlled to be over-head of the patient, in other instances, the user can define a parameter associated with the trolley **2100** trailing the patient by a desired distance or leading the patient by a desired distance.

In some instances, the amount of force exerted on the tether **2505** by the patient may increase or decrease. By way of example, a patient may stumble, thereby increasing the amount of force exerted on the tether **2505**. In such instances, the increase of force exerted on the tether **2505** can pivot the guide mechanism **2540** and can move the cam pivot arm **2571** in response to the increase in force. The movement of the cam pivot arm **2571** moves the cam assembly **2570** (as described above with reference to FIG. **33**). In this manner, the encoder **2561** of the guide mechanism **2540** and the encoder **2587** of the cam assembly **2570** can send a signal to the electronic system **2700** associated with the changes in the state of the guide mechanism **2540** and the cam assembly **2570**, respectively.

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Upon receiving the signals from the encoders **2561** and **2587**, the processor can execute a set of instructions included in the memory associated with the cam assembly **2570**. For example, the processor can determine the position of the cam **2580** or the guide mechanism **2540**, the velocity and the acceleration of the cam **2580** or the guide mechanism **2540**, or the like. Based on the determining of the changes in the guide mechanism **2540** and the cam assembly **2570** configurations, the processor can send a signal to the motor **2311** of the first drive assembly **2310** and/or the motor **2511** of the winch assembly **2510** to change the current state of the drive system **2300** and/or the patient support mechanism **2500**. In some instances, the magnitude of change in the state of the drive system and/or the patient support mechanism **2500** is based at least in part on a proportional-integral-derivative (PID) control. In such instances, the electronic system **2700** (e.g., the processor or any other electronic device in communication with the processor) can determine the changes of the patient support mechanism **2500** and model the changes based on the PID control. Based on the result of the modeling the processor can determine the suitable magnitude of change in the drive system **2300** and/or the patient support mechanism **2500**.

After a relatively short time period (e.g., much less than a second, for example, after one or a few clock cycles of the processor) the processor can receive a signal from the encoder **2470** of the drive system **2300**, the encoder **2537** of the winch assembly **2510**, the encoder **2561** of the guide mechanism **2540**, and/or the encoder **2587** of the cam assembly **2570** associated with a change in configuration of the drive system **2300**, the winch assembly **2510**, the guide mechanism **2540**, and/or the cam assembly **2570**, respectively. In this manner, one or more of the electronic devices included in the electronic system **2700**, including but not limited to the processor, execute a set of instructions stored in the memory associated with the feedback associated with the encoders **2470**, **2537**, **2561**, and **2587**. Thus, the drive system **2300** and the patient support mechanism **2500** of the trolley **2100** can be actively controlled in response to a change in force exerted on the tether **2505** and based at least in part on the current and/or previous states of the drive system **2300** and the patient support system **2500**. Similarly stated, the support system **2000** can actively reduce the amount a patient falls after stumbling or falling for other reasons.

While the patient support system **2000** is described above with reference to FIGS. 2-34 as actively supporting a portion of the body weight of the patient, in some embodiments, a patient support system can passively (i.e., not actively) support a portion of the body weight of a patient. For example, FIGS. 35 and 36 illustrate a body weight support system **3900** according to an embodiment. The body weight support system **3900** (also referred to herein as “support system”) can be used to support a portion of a patient’s body weight, for example, during gait therapy, gait training, or the like. The support system **3900** can be movably coupled to a support track (not shown) that is configured to support the weight of the support system **3900** and the weight of the patient utilizing the support system **3900**. The support track can be, for example, similar to or the same as the support track **2050** described above.

The support system **3900** includes a first coupling portion **3910** and a second coupling portion **3940**. The first coupling portion **3910** is configured to movably couple to the support track, as described above. The first coupling portion **3910** includes a first side assembly **3911**, a second side assembly **3921**, and a base **3930**. The first side assembly **3911** includes

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a set of drive wheels **3912**, a set of guide wheels **3913**, an outer wall **3914**, an inner wall **3915**, and a set of couplers **3916**. The couplers **3916** are configured to extend between the outer wall **3914** and the inner wall **3915** to couple the outer wall **3914** and the inner wall **3915** together. The outer wall **3914** is further coupled to the base **3930**. The drive wheels **3912** are arranged into an upper set of drive wheels **3912** configured to be disposed on a top surface of the support track, and a lower set of drive wheels **3912** configured to be disposed on a bottom surface of the support track. In this manner, the drive wheels **3912** roll along a horizontal portion of the support track (not shown in FIGS. 35 and 36). The guide wheels **3913** are arranged in a perpendicular orientation relative to the drive wheels **3912** and are configured to roll along a vertical portion of the support track (e.g., as similarly described above with reference to FIG. 23).

The second side assembly **3921** includes a set of drive wheels **3922**, a set of guide wheels **3923**, an outer wall **3924**, an inner wall **3925**, and a set of couplers **3916**. The first side assembly **3911** and the second side assembly **3921** are substantially the same and arranged in a mirrored configuration. Therefore, the second side assembly **3921** is not described in further detail herein and should be considered the same as the first side assembly **3921** unless explicitly described.

As shown in FIG. 36, the second coupling portion **3940** includes a cylinder **3941**, an attachment member **3945**, a piston **3950**, and an energy storage member **3960**. The cylinder **3941** is coupled to the base **3930** and is configured to house the spring **3960** and at least a portion of the piston **3950**. More specifically, the cylinder **3941** defines an opening **3942** at an end portion, opposite the base **3930**, through which at least a first end portion **3951** of the piston **3950** can move. The piston **3950** further has a second end portion **3952** that is in contact with a portion of the energy storage member **3960**. The energy storage member **3960** can be any suitable device configured to move between a first configuration having lower potential energy and a second configuration having a higher potential energy. For example, as shown in FIG. 36, the energy storage member **3960** can be a spring that is compressed when moved to its second configuration.

The attachment mechanism **3945** includes a first coupling portion **3946** that is coupled to the first end portion **3951** of the piston **3950**, and a second coupling portion **3947** that can be coupled to, for example, a harness worn by a patient. As shown in FIGS. 35 and 36, the second end portion **3952** can be an annular protrusion. In this manner, a portion of the harness such as a hook or the like can be at least partially disposed within the opening defined by the second coupling portion **3947** to couple the patient to the support system **3900**.

In use, the patient can be coupled to the support system **3900** (as described above) such that the support system **3900** supports at least a portion of the body weight of the patient. In this manner, the patient can walk along a path associated with the support track (not shown). With the support system **3900** coupled to the patient, the movement of the patient moves the support system **3900** along the support track. Similarly stated, the patient pulls the support system **3900** along the support track. In some instances, a patient may stumble while walking, thereby increasing the amount of force exerted on the support system **3900**. In such instances, the increase in force exerted on the support system **3900** can be sufficient to cause the energy storage member **3960** to move from its first configuration towards its second configuration (e.g., compress). In this manner, the piston **3950**

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can move relative to the cylinder **3941** and the energy storage member **3960** can absorb at least a portion of the increase in the force exerted on the support structure **3900**. Thus, if the patient stumbles the support system **3900** can dampen the impulse experienced by the patient that would otherwise result in known passive support systems **3900**.

Although the support system **3900** is described as including an energy storage member, in other embodiments, the support system **3900** need not include the energy storage member. For example, in some embodiments, the support system **3900** can be coupled to, for example, the attachment mechanism **2800** described above with reference to FIG. **34**. In this manner, the attachment mechanism **2800** can be used to dampen at least a portion of a change in force exerted on the support system **3900**. For example, in some instances a patient coupled to the support system **3900** may stumble, thereby increasing the force exerted on the support system **3900**. In such instances, the increase in force can move the first arm **2820** towards the second arm **2840** (see e.g., FIG. **34**), thereby moving the energy storage member **2850** towards their second configuration. Thus, at least a portion of the increase in force can be absorbed by the attachment mechanism **2800**.

Although not shown in FIG. **2-36**, one or more active support system (e.g., the support system **2000**) and/or one or more passive support system (e.g., the support system **3900**) can be disposed about a similar support track and can be utilized at the same time. For example, FIG. **37** is a schematic illustration of a support system **4000** according to an embodiment. The support system **4000** includes a support track **4050**, a first support member **4100**, and a second support member **4900**. The support system **4000** can be used to support at least a portion of the body weight of one or more patients during, for example, gait therapy (e.g., after injury), gait training (e.g., low gravity simulation), and/or the like. The support track **4050** is configured to support the weight of the first support member **4100** and the second support member **4900** and the weight of the patient utilizing the first support member **4100** and/or the second support member **4900**.

As shown in FIG. **37**, the support track **4050** can form a closed loop track. The support track **4050** can be similar to or the same as the support track **2050**, described above with reference to FIGS. **2** and **3**; the first support member **4100** can be similar to or the same as the trolley **2100**, described above with reference to FIGS. **2-33**; and the second support member **4900** can be similar to or the same as the support system **3900**, described above with reference to FIGS. **35** and **36**. In this manner, the first support member **4100** and the second support member **4900** can be hung from the support track **4050**, as described in detail above.

In some embodiments, a first patient (not shown in FIG. **37**) can be coupled to the first support member **4100** and a second patient (not shown in FIG. **37**) can be coupled to the second support member **4900** with both being suspended from the support track **4050**. As shown in FIG. **37**, the first support member **4100** can move in the direction of the arrow A in response to a movement of the first patient coupled thereto. Similarly, the second support member **4900** can be moved in the direction of the arrow B in response to a movement of the second patient coupled thereto. Expanding further, the first support member **4100** can be an active support member and can be configured to move in accordance with the movement of the first patient, as described in detail above. Conversely, the second support member **4900** can be a passive support member and can be moved by the second patient coupled thereto, as described in detail above.

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Although the support system **4000** is shown and described as including the first support member **4100** and the second support member **4900**, in other embodiments, the support system **4000** can include any suitable number of support members movably coupled to the support track **4050**. Moreover, any combination of active support members and passive support members can be included in the support system **4000**. For example, while shown as including an active support member (e.g., the first support member **4100**) and a passive support member (e.g., the second support member **4900**), in other embodiments, the support system **4000** can include two active support members, two passive support members, two active support members and two passive support members, or any other suitable combination thereof.

Although not shown in FIG. **37** the support system **4000** (i.e., the first support member **4100** and/or the second support member **4900**) can include a collision management system that is configured to prevent and/or mitigate the impact, force, or effect of a collision between the first support member **4100** and the second support member **4900**. For example, in some embodiments, the first support member **4100** can include a sensor (e.g., an ultrasonic proximity sensor or the like) configured to sense the position of the first support member **4100** relative to the second support member **4900**. Thus, when the distance between the first support member **4100** and the second support member **4900** approaches a predetermined threshold (e.g., a minimum distance), an electronic system (e.g., similar to or the same as the electronic system **2700** described above) included in the first support member **4100** can send a signal to a drive system (not shown) to increase or decrease a rotational velocity of one or more drive wheels. Thus, a collision of the first support member **4100** and the second support member **4900** can be avoided. In other embodiments, the collision management system can increase or decrease the velocity of one or more drive wheels to substantially reduce a force associated with a collision between the first support member **4100** and the second support member **4900**.

While the first support member **4100** is described above as including a sensor and/or the like that is configured to sense the position of the first support member **4100** relative to the second support member **4900**, in other embodiments, a support system can include any suitable member, device, mechanism, assembly, and/or the like that is configured to substantially maintain a distance between a first support member and a second support member included therein and/or otherwise reduce a force associated with or a likelihood of a collision. In other embodiments, a support system can include and/or can be coupled to any suitable member, device, mechanism, assembly, and/or the like that is configured to prevent direct contact between a first support member and a second support member (e.g., is disposed and/or coupled therebetween). For example, FIGS. **38-40** illustrate a support system **5000** according to an embodiment. The support system **5000** includes a first support member **5100**, a second support member **5100'**, a collision management assembly **5080**, and a support track **5050**. The support track **5050** can be similar to or the same as the support track **2050** (described above with reference to FIGS. **2** and **3**) and/or the support track **4050** (described above with reference to FIG. **37**). The first support member **5100** and the second support member **5100'** can be substantially similar to each other and can each be substantially similar to or the same as the trolley **2100**, described above with reference to FIGS. **2-33**. As such, the first support member **5100** (e.g., a first trolley) and the second support member **5100'** (e.g., a second trolley) can each be active support systems that are

hung from the support track **5050**. More specifically, as shown in FIG. **38**, the support track **5050** includes a horizontal portion **5051** and a vertical portion **5052** about which a drive mechanism of the support members **5100** and **5100'** can be disposed, thereby allowing the support members **5100** and **5100'** to move along a length of the support track **5050** in response to a motion of a supported patient, as described in detail above. Thus, the form and function of the support members **5100** and **5100'** are not described in further detail herein.

The collision management assembly **5080** of the support system **5000** can be coupled to and/or otherwise disposed between the first support member **5100** and the second support member **5100'**. In some embodiments, the collision management assembly **5080** can be coupled to the first support member **5100** or the second support member **5100'**. For example, as shown in FIG. **38**, the collision management assembly **5080** includes a coupling portion **5090** that is coupled to the first support member **5100** and a trolley portion **5085** that is movably disposed about the support track **5050**. The trolley portion **5085** can be substantially similar in form and/or function as the first coupling portion **3910** of the support system **3900** described above with reference to FIG. **35**. As such, the trolley portion **5085** includes a set of wheels **5086** that are configured to roll along the horizontal portion **5051** or the vertical portion **5052** of the support track **5050**, as described in detail above.

The trolley portion **5085** also includes a set of bumpers **5087** that extend from a surface of the trolley portion **5085**. In some embodiments, the bumpers **5087** can be formed from a relatively elastic material (e.g., rubber, silicone, polyethylene, polypropylene, polyurethane, and/or the like including copolymers and combinations thereof) that can be configured to absorb at least a portion of a force when placed in contact with an object. More specifically, in some instances, a force can be exerted that can move the trolley portion **5085** along the support track **5050** to place the bumpers **5087** in contact with an object (e.g., the second support member **5100'**). The arrangement of the bumpers **5087** can be such that when the bumpers are placed in contact with the object, at least a portion of the force exerted to move the trolley portion **5085** along the support track **5050** is absorbed by the bumpers **5087**, resulting in a deformation (e.g., an elastic or non-permanent deformation) thereof. In some instances, the deformation of the bumpers **5087** can be such that a portion of the force transmitted through the bumpers **5087** and onto the object (e.g., the second support member **5100'**) is reduced, which can reduce damage to and/or fatigue of a portion of the object. Similarly stated, the bumpers **5087** can be formed from and/or can otherwise include a material that can absorb at least a portion of an impact force between the trolley portion **5085** and an object (e.g., a wall, a support member, and/or the like).

As described above, the coupling portion **5090** is coupled to a portion of the first support member **5100**. More particularly, a first end portion **5092** of the coupling portion **5090** is rotatably coupled to the portion of the first support member **5100**. For example, the first end portion **5092** can include a rotatable eyelet or the like that can be coupled to the portion of the first support member **5100** via, for example, a bolt, pin, post, and/or the like, thereby defining an axis about which the first eyelet can rotate. Similarly, a second end portion **5094** of the coupling portion **5090** can be rotatably coupled to a portion of the trolley portion **5085**. Thus, the coupling portion **5090** can couple or otherwise form a linkage between the first support member **5100** and the trolley portion **5085** such that movement of the first

support member **5100** along the support track **5050** moves the trolley portion **5085** along the support track **5050**. For example, the coupling portion **5090** can be configured to transmit, transfer, and/or otherwise exert at least a portion of a force, associated with movement of the first support member **5100** along the support track **5050**, on the trolley portion **5085**. Moreover, the rotatable coupling of the coupling portion **5090** to the first support member **5100** and the trolley portion **5085** can be such that the first support member **5100** can push the trolley portion **5085** along a support track that is substantially nonlinear, as shown in FIG. **38**.

The coupling portion **5090** can be any suitable member, device, and/or mechanism. For example, in some embodiments, the coupling portion **5090** can be a substantially rigid rod or the like that is configured to maintain a substantially fixed distance between the trolley portion **5085** and the first support member **5100**. In other embodiments, the coupling portion **5090** can be substantially non-rigid wherein a distance between the first support member **5100** and the trolley portion **5085** can be varied (i.e., non-fixed). For example, in some embodiments, a first portion **5091** of the coupling portion **5090** can be configured to move relative to a second portion **5093** of the coupling portion **5090**. Moreover, in some embodiments, the coupling portion **5090** can be configured to absorb at least a portion of a force (associated with movement of the first support member **5100** along the support track **5050**) that would otherwise be exerted on the trolley portion **5085**. For example, as shown in FIGS. **38-40**, the coupling portion **5090** can be a piston-cylinder configuration, wherein a region of the first portion **5091** (e.g., a piston) is movably disposed in the second portion **5093** (e.g., a cylinder). Furthermore, an energy storage member **5095** (e.g., a spring or the like) can be disposed in the second portion **5093** of the coupling portion **5090**, as shown in FIG. **40**. In this manner, movement of the first portion **5091** relative to the second portion **5093** can increase a potential energy of the energy storage member **5095**. For example, in some embodiments, the energy storage member **5095** can be a spring that can be transitioned from a substantially non-compressed configuration (i.e., a relatively lower potential energy) to a substantially compressed configuration (i.e., a relatively higher potential energy) when the first portion **5091** is moved relative to the second portion **5093**. The energy storage member **5095** can be configured to allow the first portion **5091** to move relative to the second portion **5093**, for example, up to about 0.5 inches (0.5"), about 1", about 1.5", about 2", about 2.5", about 3", about 4", about 5", about 7", about 10", or any suitable distance or fraction therebetween. Thus, the coupling portion **5090** can be configured to absorb at least a portion of energy and/or force that would otherwise be transferred and/or transmitted between the first support member **5100** and the trolley portion **5085**. Although the energy storage member **5095** is shown and described as being a spring, in other embodiments, the energy storage member **5095** can be any suitable device, member, and/or volume such as, for example, a volume of a compressible gas and/or the like.

In use, the collision management assembly **5080** can be included in the support system **5000** to substantially prevent a collision between the first support member **5100** and the second support member **5100'** (see e.g., FIG. **38**). Similarly stated, the collision management assembly **5080** can be included in the support system to substantially prevent direct contact between the first support member **5100** and the second support member **5100'**. For example, in some instances, it can be desirable to maintain a distance between

the first support member **5100** and the second support member **5100'** that is greater than a predetermined minimum distance and/or a distance threshold. In this manner, the collision management assembly **5080** can be coupled to the first support member **5100** such that when the first support member **5100** and the second support member **5100'** move along the support track **5050** substantially independent from one another, a distance therebetween is maintained that is greater than the predetermined minimum distance and/or distances threshold. For example, in some instances, the first support member **5100** can move relative to the second support member **5100'** such that a distance therebetween is reduced to an extent that places the bumpers **5087** of the trolley portion **5085** in contact with a portion of the second support member **5100'**. Thus, the collision management assembly **5080** can maintain the first support member **5100** and the second support member **5100'** at a distance that is greater than the minimal distance, thereby preventing direct contact (i.e., a direct collision) therebetween. Moreover, the arrangement of the bumpers **5087** and the coupling portion **5090** is such that as the collision management assembly **5080** is brought into contact with the portion of the second support member **5100'** at least a portion of a force associated with the impact is absorbed (e.g., the bumpers **5087** can be transitioned from a non-deformed to a deformed configuration and/or the energy storage member **5095** can be transitioned from a lower potential energy configuration to a higher potential energy configuration). In this manner, an acceleration and/or a jerk (e.g., the rate of change in the acceleration) of the first support member **5100** and/or the second support member **5100'** is not rapidly changed as the collision management assembly **5080** is brought into contact with the second support member **5100'**. In some instances, once the collision management assembly **5080** is placed in contact with the second support member **5100'**, the first support member **5100** and the second support member **5100'** can move along the support track **5050** substantially congruently. In other words, when the collision management assembly **5080** is placed in contact with the second support member **5100'**, the collision management assembly **5080** can push the second support member **5100'** such that the first support member **5100**, the second support member **5100'**, and the collision management assembly **5080** collectively move along the support track **5050** at substantially the same speed.

In some embodiments, the collision management assembly **5080** and/or a portion of the support members **5100** and/or **5100'** can include, for example, one or more sensors or the like that can sense and/or detect one or more parameters associated with the collision management assembly **5080**. For example, in some embodiments, the trolley portion **5085** of the collision management assembly **5080** can include a sensor such as, for example, an accelerometer or the like that can sense and/or otherwise detect and acceleration of the trolley portion **5085** when the bumper **5087** is placed in contact with the second support member **5100'**. In some instances, the sensor can send a signal associated with the acceleration of the trolley portion **5085** to, for example, the electronic system of the first support member **5100**. As such, the electronic system can be configured to control one or more systems (e.g., a drive system or the like) of the first support member **5100** based at least in part on the signal received from the sensor. For example, in some instances, the electronic system can reduce a velocity of the first support member **5100** based at least in part on information received from the sensor of the collision management assembly **5080**.

Although the collision management assembly **5080** is shown and described as being coupled to the first support member **5100** and placed in contact the second support member **5100'** (see e.g., FIG. 38), in other embodiments, the collision management assembly **5080** can be rotatably coupled to the second support member **5100'** and placed in contact with the first support member **5100** in a similar manner as described above. In addition, while the second support member **5100'** is shown and described as being substantially similar to the first support member **5100** (i.e., an active support member), in other embodiments, the second support member **5100** can be a passive support member such as, for example, the support system **3900** described above with reference to FIGS. 35 and 36.

While the support system **5000** is described above as including the collision management assembly **5080** to substantially maintain a distance between the first support member **5100** and the second support member **5100**, in other embodiments, a support system can include any suitable member, device, mechanism, assembly, and/or the like that is configured to absorb at least a portion of energy that is associated with a collision between a support member and another object (e.g., a second support member, a wall, and/or any other obstruction). For example, FIGS. 41-42 illustrate a support system **6000** according to an embodiment. The support system **6000** includes a support member **6900** movably disposed about a support track **6050**. The support track **6050** can be similar to or the same as the support track **2050** (described above with reference to FIGS. 2 and 3) and/or the support track **4050** (described above with reference to FIG. 37). The support member **6900** can be substantially similar to the support system **3900**, described above with reference to FIGS. 35-36. As such, the support member **6900** can be, for example, a passive support system that is hung from the support track **6050**. More specifically, as shown in FIGS. 41 and 42, the support track **6050** includes a horizontal portion **6051** and a vertical portion **6052** about which a drive mechanism **6910** (e.g., similar to or the same as the first coupling portion **3910** of the support system **3900** described above) of the support member **6900** can be disposed, thereby allowing the support member **6900** to move along a length of the support track **6050** in response to a motion of a supported patient, as described in detail above. Thus, the form and function of the support member **6900** is not described in further detail herein.

As shown in FIGS. 41 and 42, the support member **6900** can be coupled to and/or can otherwise include a collision plate **6020**. The collision plate **6020** (e.g., a collision management assembly or member) can be any suitable shape, size, or configuration. For example, although the collision plate **6020** is shown as having a substantially circular perimeter, in other embodiments, a collision plate can be any suitable shape such as, square, rectangular, oblong, elliptical, and/or the like. As shown in FIG. 42, the collision plate **6020** can be coupled to a portion of the support member **6900** such that a surface of the collision plate **6020** in contact with the support member **6900** is substantially parallel to the horizontal portion **6051** of the support track **6050**. Moreover, although not shown in FIGS. 41 and 42, the arrangement of the support member **6900** can be such that the collision plate **6020** is disposed between the drive portion **6910** and a coupling portion (e.g., such as the second coupling portion **3940** included in the support system **3900** described above with reference to FIG. 36).

As shown, the collision plate **6020** is configured to extend beyond a perimeter of the support member **6900**. The collision plate **6020** can be formed from and/or can include

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any suitable material that can be substantially rigid such as, for example, wood, medium density fiber (MDF), plywood, and/or a metal or alloy thereof (e.g., aluminum, aluminum alloy, steel, steel alloy, etc.). In other embodiments, the collision plate **6020** can be formed from and/or can include any suitable material that can be substantially elastic such as, for example, rubber, silicone, polyethylene, polypropylene, polyurethane, nylon, and/or the like including copolymers and/or combinations thereof. The collision plate **6020** includes a bumper **6021** that is coupled to and/or that is otherwise configured to extend from a peripheral surface, as shown in FIGS. **41** and **42**. The bumper **6021** can be any suitable shape, size, and/or configuration. For example, in some embodiments, the bumper **6021** can be formed from and/or can include, for example, expanded foam neoprene, ethylene propylene diene monomer (EPDM) rubber, ethylene-vinyl acetate (EVA) foam, polypropylene (PP) foam, high-density polyethylene (HDPE) foam, low-density polyethylene (LDPE) foam, linear-low-density polyethylene (LLPDE) foam, and/or any other suitable thermoplastic elastomer (TPE) foam, and/or the like. In this manner, the bumper **6021** can be configured to absorb at least a portion of energy that is associated with, for example, an impact. By way of example, in some instances, the support member **6900** can move along the support track **6050** relative to another support member and/or other object until the bumper **6021** of the collision plate **6020** is placed in contact with the other support member and/or other object. More specifically, the support member **6900** can be moved along the support track **6050** with a force resulting from a patient, coupled thereto, dragging or towing the support member **6900** (as described above). In some instances, the support member **6900** can be moved relative to another object on or supported by the support track **6050** in such a manner that the support member **6900** and the other object (e.g., a second support member or the like) collide. Thus, with the collision plate **6020** coupled to the support member **6900** and the bumper **6021** extending beyond the support member **6900**, the bumper **6021** is placed in contact with the other object, resulting in an elastic deformation of the bumper **6021** in response to at least a portion of a force associated with the collision. As such, the bumper **6021** can absorb at least a portion of the energy associated with the collision to, for example, protect and/or otherwise minimize damage to the support member **6900** and/or other object that can otherwise result from the collision.

Although the support track **4050** is shown and described above as being a substantially closed-loop track, in other embodiments, a support track can be an open-loop track. By way of example, in some embodiments, a support track can have a first end portion that is substantially discrete from a second end portion (i.e., an open-loop configuration). In some embodiments, such a support track can include, for example, an end stop or the like that can be configured to substantially limit movement of a support member, support system, trolley, etc., prior to reaching the end of the support track. For example, FIGS. **43** and **44** illustrate a support track **7050** including a track stop **7060**, according to an embodiment. The support track **7050** can be substantially similar to the support track **2050** described above. As such, the support track **7050** can include a horizontal portion **7051** and a vertical portion **7052** and can be configured to support a support system such as, for example, the trolley **2100** and/or the support system **3900**.

The track stop **7060** includes a trolley portion **7065** and a coupling portion **7070**. The trolley portion **7065** can be substantially similar in form and/or function as the trolley

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portion **5085** included in the collision management assembly **5080** described above with reference to FIGS. **38-40**. As such, the trolley portion **7065** includes a set of wheels **7066** that are configured to roll along the horizontal portion **7051** or the vertical portion **7062** of the support track **7050**, as described in detail above. The trolley portion **7065** also include at least one bumper **7067** that extends from a surface of the trolley portion **7065** (e.g., away from an end surface of the support track **7050**). In some embodiments, the bumper **7067** can be formed from a relatively elastic material (e.g., rubber, silicone, polyethylene, polypropylene, polyurethane, and/or the like including copolymers and combinations thereof) that can be configured to absorb at least a portion of a force when placed in contact with an object, as described in detail above. The arrangement of the bumper **7067** can be such that when placed in contact with, for example, a support member, at least a portion of the force exerted to move the support member along the support track **7050** is absorbed by the bumper **7067**, resulting in a deformation (e.g., an elastic or non-permanent deformation) thereof, which can reduce damage to and/or fatigue of a portion of the support member, as described in detail above.

The coupling portion **7070** is coupled to the end portion of the support track **750** and a portion of the trolley portion **7065**, as shown in FIG. **43**. More particularly, a mounting bracket **7075** is coupled to the end portion of the support track **7050** and is configured to couple and/or otherwise mount the coupling portion **7070** to the support track **7050**. The coupling portion **7070** can be any suitable member, device, and/or mechanism. For example, in some embodiments, the coupling portion **7070** can be a piston-cylinder device, a strut, and/or the like. As such, the coupling portion **7070** includes a first member **7071** (e.g., a piston) that can be moved relative to a second member **7073** (e.g., a cylinder). For example, at least a portion of the first member **7071** can be movably disposed in the second member **7073**. More particularly, an attachment member **7072** of the first member **7071** is rotatably coupled to the trolley portion **7065** (as described above) and in turn, the first member **7071** is configured to move substantially concurrently with the trolley portion **7065**. Similarly stated, the attachment member **7072** rotatably couples the first member **7071** to the trolley portion **7065** such that as the trolley portion **7065** is moved along the support track **7050**, the first member **7071** is moved in an axial direction. The second member **7073** of the coupling portion **7070** is fixedly coupled to the mounting bracket **7075**, which is configured to maintain the second portion **7073** in a substantially fixed position relative to the support track **7050**. Thus, movement of the trolley portion **7065** along the support track **7050** moves the first member **7071** of the coupling portion **7070** relative to the second member **7073**, as described in further detail herein.

As shown in FIG. **44**, an energy storage member **7074** (e.g., a spring or the like) is disposed in the second portion **7093** of the coupling portion **7070** and is configured to engage and/or be in contact with at least a surface of the first member **7071**. In this manner, movement of the first member **7071** relative to the second member **7073** can increase a potential energy of the energy storage member **7074**. For example, in some embodiments, the energy storage member **7074** can be a spring (as shown in FIG. **44**) that can be transitioned from a substantially non-compressed configuration (i.e., a relatively lower potential energy) to a substantially compressed configuration (i.e., a relatively higher potential energy) when the first member **7071** is moved relative to the second member **7073**. The energy storage member **7074** can be configured to allow the first member

7071 to move relative to the second member **7073**, for example, up to about 0.5 inches (**0.5"**), about 1", about 1.5", about 2", about 2.5", about 3", about 4", about 5", about 7", about 10", or any suitable distance or fraction therebetween. Thus, the coupling portion **7070** can be configured to absorb at least a portion of energy and/or force, as described in further detail herein. Although the energy storage member **7074** is shown and described as being a spring, in other embodiments, the energy storage member **7074** can be any suitable device, member, and/or volume such as, for example, a volume of a compressible gas and/or the like.

In use, the track stop **7060** can be included in the support system **7000** to substantially prevent a support member and/or trolley (not shown in FIGS. **43** and **44**) from reaching an end of a support track **7050** when moving along a length thereof. For example, a support member can move along the support track **7050** and towards the end portion to a position in which a portion of the support member is placed in contact with the bumper **7067** of the trolley portion **7065**. Thus, the support member exerts a force on the bumper **7067** that can transition the bumper **7067** from a non-deformed configuration to a deformed configuration, thereby absorbing at least a portion of the force and/or kinetic energy. Moreover, the force exerted by the support member can move the trolley portion **7065** along the support track **7050**, which in turn, moves the first member **7071** of the coupling portion **7070** relative to the second member **7073** of the coupling portion **7070**. Accordingly, with the first member **7071** in contact with the energy storage member **7074**, the movement of the first member **7071** relative to the second portion **7072** can transition the energy storage member **7074** from a lower potential energy configuration to a higher potential energy configuration. In this manner, an acceleration and/or a jerk (e.g., the rate of change in the acceleration) of the support member is not rapidly changed as the track stop **7060** limits further movement of the support member along the support track **7050**. Furthermore, by absorbing at least a portion of the kinetic energy and/or force exerted by the support member, damage to the support member that can otherwise result from the support member hitting a "hard stop" (e.g., a stop mechanism with little or no energy absorption).

Although the trolley **2100** is described above as including the encoder **2470** of the drive system **2300**, the encoder **2561** of the guide mechanism **2540**, and the encoder **2587** of the cam assembly **2570**, which are collectively used to determine one or more system parameters (e.g., position, velocity, acceleration, etc.), in other embodiments, a trolley and/or the like can include any suitable device, mechanism, and/or system configured to determine one or more system parameters. For example, FIGS. **45-47** are schematic illustrations of a trolley **8100** including an optical tracking system **8720**, according to an embodiment. The trolley **8100** (e.g., a support member) can be substantially similar to or the same as the trolley **2100**, described above with reference to FIGS. **2-33**. As such, the trolley **8100** is an active support system that is hung from a support track (not shown in FIGS. **45-47**). The trolley **8100** can differ from the trolley **2100**, however, with the inclusion of the optical tracking system **8720**, as described in further detail herein.

The optical tracking system **8720** includes at least an imaging device **8725** and a tracking member **8860**. As shown in FIG. **45**, the tracking member **8860** can be coupled to and/or included in a patient attachment mechanism **8800**, which can otherwise be substantially similar to the patient attachment mechanism **2800** described above with reference to FIG. **34**. The patient attachment mechanism **8800** is

operably coupled to the trolley **8100** by a tether **8505**. The tether **8505** can be substantially similar to or the same as the tether **2505** included in the support system **2500** described above with reference to FIGS. **27-33**. The tracking member **8860** can be any suitable shape, size, and/or configuration. For example, in some embodiments, the tracking member **8860** can be a substantially spherical or oblong ball. Although not shown in FIGS. **45-47**, the tracking member **8860** can include a surface finish that can facilitate an optical tracking. For example, in some embodiments, the tracking member **8860** can include a surface having a color and/or pattern that can be used to identify, for example, position information such as relative linear position, relative angular position, absolute position, etc. Moreover, information associated with the color, the pattern, the size, the shape, and/or the like of the tracking member **8860** can be stored, for example, in a memory included in an electronic system (e.g., substantially similar to the electronic system **2700** of the trolley **2100** (not shown in FIGS. **45-47**)) of the trolley **8100**.

The imaging device **8725** of the optical tracking system **8720** can be any suitable imaging device. For example, in some embodiments, the imaging device **8725** can be a camera and/or the like that can capture discrete pictures and/or can continuously record a video stream. The imaging device **8725** is coupled to the trolley **8100** and is maintained in a fixed position relative thereto. Although not shown in FIGS. **45-47**, the imaging device **8725** is operably coupled to the electronic system of the trolley **8100**. Thus, the imaging device **8725** can be configured to send a signal representing data associated with captured images and/or video streams and, upon receipt, the electronic system can store the data in, for example, the memory and/or the like. Furthermore, the memory of the electronic system can store data associated with the position of the imaging device **8725** or a portion of the imaging device **8725** (e.g., a lens, aperture, focal point, charge-coupled device (CCD) sensor, a complementary metal-oxide-semiconductor (CMOS) sensor, and/or the like), relative to a portion of the trolley **8100**. As such, the electronic system of the trolley **8100**, and more specifically, a processor and/or module can determine, for example, a reference coordinate system relative to the imaging device **8725** and/or a portion of the trolley **8100**.

In some instances, the imaging device **8725** can be used to capture one or more images and/or video streams of the tracking member **8860** while in use during, for example, gait training and/or the like. For example, as shown in FIGS. **46** and **47**, the optical tracking system **8720** can be used to determine a first position **P** and a second position **P'** of the tracking member **8860** and thus, the patient attachment mechanism **8800**. More specifically, in some instances, a patient (not shown) can be coupled to the patient attachment mechanism **8800** (e.g., via a harness or the like, as described above) and can perform a gait training therapy session, thereby moving the patient attachment mechanism **8800** relative to the trolley **8100** and the trolley along the support track (not shown in FIGS. **45-47**). During use, the imaging device **8725** can capture one or more images and/or video streams of the tracking member **8860** to determine, for example, the first position **P** and the second position **P'** of the tracking member **8860**. More specifically, as shown in FIG. **46**, the imaging device **8725** can capture one or more images and/or video streams and can send a signal representing data associated with the one or more images and/or video streams to the processor and/or to a module (e.g., a processing module) included in the electronic system. The processor and/or module can, for example, analyze the image and can calculate a distance **D** of the image of the tracking member

8860 from a reference plane **R** and a size **S** of the image of the tracking member **8860**. Based at least in part on the calculated distance **D** and the calculated size **S**, the processor and/or module can determine and/or calculate an angle **A** of the tether **8505**, a length **L** of the tether **8505**, and a distance **H** of the tracking member **8860** from the trolley **8100** (FIG. 47), thereby determining the first position **P** of the tracking member **8860** and the patient attachment mechanism **8800**. Similarly, when the patient moves from the first position **P**, the imaging device **8725** can capture one or more images and/or video streams and can send a signal representing data associated with the new images and/or video streams to the processor and/or module. As such the processor and/or module can, for example, analyze the image and can calculate a second distance **D'** of the image of the tracking member **8860'** from the reference plane **R** and a second size **S'** of the image of the tracking member **8860'**. Based at least in part on the calculated second distance **D'** and the calculated second size **S'**, the processor and/or module can determine and/or calculate a second angle **A'** of the tether **8505'**, a second length **L'** of the tether **8505'**, and a second distance **H'** of the tracking member **8860'** from the trolley **8100** (FIG. 47), thereby determining the second position **P'** of the tracking member **8860'** and the patient attachment mechanism **8800'**.

Although the trolley **2100** is described above as including the encoder **2470** of the drive system **2300**, the encoder **2561** of the guide mechanism **2540**, and the encoder **2587** of the cam assembly **2570**, which are collectively used to determine one or more system parameters (e.g., position, velocity, acceleration, etc.), and the trolley **8100** is described above as including the optical tracking system **8720** to determine the one or more system parameters, in other embodiments, a trolley and/or support system can use any suitable combination of an encoder system and an optical tracking system. For example, in some embodiments, a trolley can use data from any number of encoders (e.g., of a drive system, guide mechanism, and/or cam assembly) and an optical tracking system.

While the trolleys **2100** and **8100** are described above as including an electronic system (e.g., the electronic system **2700**) that actively controls the operating condition of the trolleys **2100** and **8100** to support at least a portion of the weight of the patient, in some embodiments, a trolley can include an electronic system, which, in addition to controlling the operating condition of the trolley, can determine one or more characteristics associated with the patient's gait during use. By way of example, a trolley such as the trolley **2100** and/or **8100** can include a set of encoders, sensors, and/or the like that can determine a set of operating conditions associated with a portion of the trolley. Specifically, in some embodiments, the trolley can include a drive system similar to the drive system **2300** in FIGS. 12-26, a patient support mechanism similar to the patient support mechanism **2500** in FIGS. 27-33, and an electronic system similar to the electronic system **2700** in FIGS. 10 and 11, which can be used collectively to determine the set of operating conditions associated with the trolley. In turn, the electronic system can determine, based on the set of operating conditions, the one or more characteristics associated with the patient's gait during use.

By way of example, in some embodiments, the patient support mechanism can include, inter alia, a winch assembly coupled to a tether, a guide mechanism, a cam assembly. The winch assembly can have an encoder (e.g., similar to the encoder **2537**), the guide mechanism can have an encoder (e.g., similar to the encoder **2561**), and the cam assembly can

have an encoder (e.g., similar to the encoder **2587**). Similarly, the drive system can have an encoder (e.g., similar to the encoder **2470**). The electronic system can include at least a processor and a memory configured to receive one or more signals from the encoders of the drive mechanism and the patient support mechanism. In some embodiments, the electronic system can also include an imaging device (e.g., similar to the imaging device **8725** in FIGS. 46 and 47) configured to capture and image or video stream of a tracking member (e.g., similar to the tracking member **8860**).

As described in detail above, when a patient using the patient support system begins to walk, the drive mechanism can move the trolley along the support track in response to his or her movement. The encoder of the drive mechanism can, in turn, sense one or more characteristics associated with the operation of the drive mechanism. For example, the encoder can sense a position of the drive mechanism relative to the support track, a translational velocity of the drive mechanism along the support track, a translational acceleration of the drive mechanism along the support track, a rotational velocity of one or more wheels, a rotational acceleration of one or more wheels, an angular orientation of one or more wheels, a motor speed and/or direction, a voltage associated with at least a portion of the motor, and/or the like. The encoder can then send a signal associated with the one or more characteristics of the drive mechanism to the electronic system, which in response, can cause the processor to determine and/or update an operating condition of the drive mechanism based at least in part on a change in the one or more characteristics of the drive mechanism relative to a previously defined operating condition of the drive mechanism (e.g., stored in a memory or the like), as described in detail above with reference to the trolley **2100**.

Similarly, in response to the walking of the patient, the encoder of the winch assembly, the guide mechanism, and/or the cam assembly (as well as the imaging device if included therein) can sense and/or determine one or more characteristics associated with the operation of the patient support mechanism. For example, in some instances, the patient may walk faster than the trolley, thereby changing the angle of the tether and the guide mechanism relative to the trolley. The encoder of the guide mechanism can sense the angular deflection of the guide mechanism and can send a signal associated with the angle of the guide mechanism to the electronic system. Upon receipt, the electronic system can cause the processor to determine and/or update an operating condition of the guide mechanism.

In some instances, the movement of the patient may, for example, increase a length of a portion of the tether. As such, a portion of the tether can be unspooled from a drum or the like included in the winch assembly. More specifically, at least a portion of a force exerted by the patient on the tether can rotate the drum or the like, which in turn, results in an unspooling of the tether (i.e., an increase in a length of a portion of the tether between the patient and the winch assembly). The encoder of the winch assembly can sense one or more characteristics associated with the operation of the winch assembly. For example, the encoder can sense an angular position of the drum, a rotational velocity of the drum, an acceleration of the drum, a speed and/or direction of a motor included in the winch assembly, a voltage associated with at least a portion of the motor of the winch assembly, and/or the like. The encoder can then send a signal associated with the one or more characteristics of the winch assembly to the electronic system, which in response, can cause the processor to determine and/or update an oper-

ating condition of the winch assembly based at least in part on a change in the one or more characteristics of the winch assembly relative to a previously defined operating condition of the winch assembly (e.g., stored in a memory or the like), as described in detail above with reference to the trolley **2100**. In some instances, based at least in part on the updated operating condition of the winch assembly, the processor can determine a length of the portion of the tether disposed between the patient and the winch assembly. In some embodiments, the tether can be coupled to a load cell or the like configured to sense a force exerted by the patient on the tether (e.g., by measuring a stress, tension, strain, and/or the like along and/or within a portion of the tether). The load cell can be configured to send a signal to the electronic system associated with a load (e.g., force) exerted on the tether, which in turn, can cause the processor to determine a force exerted by the patient.

In some instances, an amount of force exerted on the tether by the patient may increase or decrease in a substantially sudden manner. For example, if a patient stumbles, an amount of force exerted on the tether may increase relatively suddenly. In such instances, the increase of force exerted on the tether may pivot the guide mechanism and/or increase a length of a portion of the tether (as described above), as well as rotate a cam and/or cam arm included in the cam assembly (e.g., as described with reference to the cam assembly **2570** in FIGS. **32** and **33**). In other words, at least a portion of the cam assembly can be configured to rotate in response to a relatively fast movement and/or deflection of the tether. The encoder of the cam assembly can sense one or more characteristics associated with a movement of the cam and/or cam arm such as, for example, position, velocity, acceleration, jerk, orientation, alignment, force, and/or the like. The encoder of the cam assembly can then send a signal associated with the one or more characteristics of the cam assembly to the electronic system, which in response, can cause the processor to determine and/or update an operating condition of the cam assembly based at least in part on a change in the one or more characteristics of the cam assembly relative to a previously defined operating condition of the cam assembly (e.g., stored in memory), as described above with reference to the trolley **2100**.

By defining, determining, and/or updating one or more operating conditions of the drive mechanism and/or the patient support mechanism, the electronic system (e.g., at least the processor of the electronic system) can actively control the trolley to support at least a portion of a weight of the patient using the patient support system. As described above, in some instances, the magnitude of change in the operating condition of the drive system and/or the patient support mechanism is based at least in part on a proportional-integral-derivative (PID) control. In such instances, the electronic system (e.g., the processor or any other electronic device in communication with the processor) can determine the changes of the patient support mechanism and model the changes based on the PID control. Based on the result of the modeling the processor can determine the suitable magnitude of change in the operating condition of the drive system and/or the patient support mechanism.

For example, FIG. **48** is a schematic illustration of a control diagram according to an embodiment. In this embodiment, the electronic system (described above) can be configured to control the drive system and/or the patient support mechanism based at least in part on a tension within and/or along a portion of the tether. Specifically, a nurse, technician, therapist, doctor, physician, etc. can define a predetermined value associated with a target tether tension

T^* (e.g., commanded tether tension). With the commanded tether tension T^* stored, for example, in memory, the processor of the electronic system can compare an actual tension T within and/or along the portion of the tether against the commanded tether tension T^* to determine a tension error. In some instances, the processor can then perform a derivative control operation **101** on the tension error, the output of which can be added to one or more proportional control operation outputs (described in further detail below) to determine, for example, a motor speed command ω_M^* for controlling motor and drive dynamics **102** associated with a motor included in the drive system and/or the patient support mechanism.

As shown in FIG. **48**, a proportional control operation **103** can be performed on a value associated with an actual motor speed ω_M of the motor included in the drive system and/or patient support mechanism. In addition the actual motor speed ω_M can be evaluated with a value Z associated with a downward motion of the tether (e.g., in response to a force exerted by a patient) for controlling spring mechanism dynamics **104** associated with, for example, the cam assembly of the patient support mechanism. As a result, the processor can define (1) an updated value of the actual tension T within and/or along the portion of the tether, and (2) a cam unloading rotation speed ω_C . An equivalent motor speed can be determined by evaluating a rotational speed associated with a portion of the cam and a rotational speed associated with, for example, the drum of the winch assembly (represented in FIG. **48** by the reference numeral **105**). A proportional control operation **106** can be performed on the equivalent motor speed, an output of which can then be added to an output of the proportional control operation **103**. As described above, the sum of the proportional control operations **103** and **106** can be added to the output of the derivative control operation **101** to define the motor speed command ω_M^* . Thus, in this embodiment and as described above, the electronic system (e.g., or at least the processor included therein) can control the trolley, in response to movement of a patient, based at least in part on a PID control feedback loop and/or the like.

In some instances, the electronic system can determine one or more characteristic associated with a patient's gait based at least in part on an operating condition and/or a change in operating condition of the drive mechanism and/or the patient support mechanism. For example, FIG. **49** is a graph **200** illustrating a displacement of a center of mass of a patient according to an embodiment. As shown, a patient's center of mass shifts during a gait cycle (e.g., up to about 5 centimeters (cm)), which in turn, results in a shifting and/or changing force exerted on the tether when the patient is using the patient support system. For example, the center of mass of the patient can be at a lowest point (i.e., closest to a surface on which the patient is walking) at about 5% and about 55% of the gait cycle, which corresponds to a termination of a swing phase of the gait cycle. The center of mass of the patient can be at a highest point (i.e., furthest away from the surface on which the patient is walking) at about 30% and about 80% of the gait cycle, which corresponds to the patient's center of mass passing over his or her weight bearing leg. Similarly, the center of mass of the patient can shift in a lateral direction during the gait cycle, as shown in FIG. **49**. With at least a portion of the weight of the patient supported by the patient support mechanism, the shifting of the center of mass of the patient results in a corresponding shift and/or change in the force exerted on the tether by the weight of the patient. Therefore, based on one or more operating conditions associated with the drive system and/or

the patient support mechanism, the processor can determine a set of characteristics associated with the patient's gait.

By way of example, FIGS. 50-53 are graphs illustrating operating conditions associated with the patient support mechanism in response to a patient's movement. In this instance, the operating conditions associated with the patient support mechanism relate to a tether position and a cam angle of the cam included in the cam assembly, which in turn, can be used to determine one or more characteristics associated with the patient's gait. More specifically, the processor of the electronic system can determine the tether position based on a signal received from one or more encoders (e.g., the encoder of the winch assembly, the guide member, and/or any other suitable encoder) and can determine the cam angle based on, for example, the encoder of the cam assembly.

As shown in FIG. 50, the tether position and cam angle are graphed in response to a relatively slow movement of a normal or healthy patient's gait. Specifically, graph 301 illustrates a position of a portion of the tether, with and without factoring in a position associated with the cam, in response to the patient's gait; graph 302 illustrates a cam angle of the cam in response to the patient's gait; graph 303 illustrates a change in the tether position plus a change in the cam angle in response to the patient's gait; and graph 304 illustrates the speed and acceleration associated with the tether in response to the patient's gait. In some instances, the position of the portion of the tether, as shown in graph 301, can change in response to a relatively slow, gradual, and/or substantial change in the patient's movement, while the cam angle of the cam, as shown in graph 302, can change in response to a relatively fast, sudden, and/or abrupt movement of the tether. In some instances, the change in cam angle in response to the relatively fast movement of the tether can, for example, reduce noise or the like that might otherwise alter a determination of the tether position. As shown in graph 303, the change in the tether position and the change in the cam angle can be determined, which in turn, can be used to determine a speed and acceleration associated with the tether position, as shown in graph 304. Moreover, by determining the tether position, velocity, and acceleration, the processor of the electronic system can determine one or more characteristics associated with the patient's gait. For example, in some instances, the gait of a healthy patient may have and/or define a substantially symmetric characteristic when comparing movement of the patient's left leg to movement of the patient's right leg. Thus, by determining the position, velocity, and acceleration of the tether, the processor can determine gait characteristics such as, for example, a number of steps, a distance traveled, a stride length, a velocity, a difference between gait characteristics associated with the left leg and the right leg, and/or any other suitable characteristic.

In a similar manner, FIG. 51 illustrates graphs showing the tether position and cam angle in response to a relatively fast movement of the normal or healthy patient's gait. Specifically, graph 401 illustrates a position of a portion of the tether, with and without factoring in a position associated with the cam, in response to the patient's gait; graph 402 illustrates a cam angle of the cam in response to the patient's gait; graph 403 illustrates a change in the tether position plus a change in the cam angle in response to the patient's gait; and graph 404 illustrates the speed and acceleration associated with the tether in response to the patient's gait. As can be seen in FIGS. 50 and 51, the speed associated with the patient's movement can result in a different response of the tether position and the cam angle. Thus, the processor of the

electronic system can determine any suitable gait characteristic associated with the patient's relatively fast gait, which can be different from a corresponding gait characteristics associated with the patient's relatively slow gait.

While the graphs in FIGS. 50 and 51 illustrate the tether position and the cam angle relative to a normal or healthy patient's gait, FIGS. 52 and 53 illustrate a tether position and cam angle relative to an impaired patient's gait and more specifically, to the gait of a patient with an impairment resulting in a dragging of one of his or her legs. For example, in FIG. 52, graph 501 illustrates a position of a portion of the tether, with and without factoring in a position associated with the cam relative to the impaired patient's gait; graph 502 illustrates a cam angle of the cam relative to the impaired patient's gait; graph 503 illustrates a change in the tether position plus a change in the cam angle relative to the impaired patient's gait; and graph 504 illustrates the speed and acceleration associated with the tether relative to the impaired patient's gait. Similarly, in FIG. 53, graph 601 illustrates a position of a portion of the tether, with and without factoring in a position associated with the cam relative to circumduction movement of the impaired patient's gait; graph 602 illustrates a cam angle of the cam relative to circumduction movement of the impaired patient's gait; graph 603 illustrates a change in the tether position plus a change in the cam angle relative to circumduction movement of the impaired patient's gait; and graph 604 illustrates the speed and acceleration associated with the tether relative to circumduction movement of the impaired patient's gait.

As can be seen in FIGS. 52 and 53, the impairment causing the patient to drag one leg during his or her gait results in a response of the tether position and the cam angle that is more erratic, abrupt, and/or otherwise more irregular relative to the response of the tether position and the cam angle resulting from a non-impaired patient's gait. In some instances, the position, velocity, and/or acceleration of the tether position resulting from the impaired patient's gait can be compared to the position, velocity, and/or acceleration of the tether position resulting from the non-impaired patient's gait. As such, the processor of the electronic system can determine, predict, and/or otherwise analyze the characteristics of the impaired patient's gait, which in turn, can be used to define a therapeutic treatment plan, a therapeutic progress report, a diagnostic method, and/or the like.

In some instances, the patient support system (and/or any of the patient support systems described herein) can be used in conjunction with any other suitable device configured to determine, provide, and/or define characteristics associated with a patient's gait. In some instances, the analysis of the one or more operating conditions of the drive mechanism and/or patient support mechanism can be used in conjunction with an analysis of data associated with an electric stimulator configured, for example, to improve an impaired patient's gait. For example, the patient support system can be used to support a patient donning an electric stimulator, configured to facilitate the gait of a patient experiencing drop foot or the like, such as those described in U.S. Patent Publication No. 2014/0303705 entitled, "Orthosis for a Gait Modulation System," filed Apr. 4, 2014, the disclosure of which is incorporated herein by reference in its entirety. As shown in FIG. 54, the electric stimulator can define one or more operating conditions associated with the electric stimulator and/or the impaired patient's gait. For example, the electric stimulator can sense and/or determine an anterior or posterior motion, a lateral motion, a total motion (e.g., a combination of the lateral motion and the anterior or pos-

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terior motion), and/or a pressure associated with a heel on or heel off event, as shown in FIG. 54. In this instance, graph 701 illustrates an acceleration associated with the operation of the electric stimulator; graph 702 illustrates a speed associated with the operation of the electric stimulator; graph 703 illustrates a rotation associated with the operation of the electric stimulator; and graph 704 illustrates an angle associated with the operation of the electric stimulator.

In some embodiments, the electric stimulator can send a signal associated with one or more of its operating conditions to the electronic system of the patient support system. As such, the processor can determine one or more gait characteristics of the impaired patient based on data received from the drive system and/or patient support mechanism as well as the electric stimulator. By way of example, FIG. 55 illustrates graphical representations of a set of gait characteristics of a patient, which were determined based at least in part on data associated with the patient support system and the electric stimulator (as described in detail above). Specifically, graph 801 illustrates a swing and stance duration of the patient's gait; graph 802 illustrates a swing to stance ratio of the patient's gait; graph 803 illustrates a cadence of the patient's gait; graph 804 illustrates an anterior and lateral range of motion (ROM) associated with one or both of the patient's legs; graph 805 illustrates an anterior to lateral ratio associated with one or both of the patient's legs; and graph 806 illustrates a stride length and height of the patient's gait. Thus, the operating conditions associated with the patient support system and any other suitable device can be used to determine one or more characteristics of the patient's gait. Moreover, the electronic system can be configured to send a signal to any suitable output device (e.g., a monitor, a laptop, a personal computer, a hand held controller, a smartphone, and/or the like) that is indicative of an instruction to output data associated with the one or more characteristics of the patient's gait.

As described above, any of the patient support systems and/or body weight support systems described herein can be used to and/or can otherwise facilitate an analysis of a patient's gait while using that system. For example, in some embodiments, the patient support systems can be used with an electronic device (e.g., a personal computer, laptop, tablet, smartphone, controller, remote display, workstation, server, and/or the like) to determine data associated with the patient's gait and graphically and/or alpha-numerically represent that data on a display. The patient support system can include, for example, a trolley tracking and dynamic body weight engine, module, process, compute device, etc. to determine data such as trolley speed, travelled distance, tether length, CAM angle, body weight unloading, elapsed time, and/or any other suitable data set.

In addition, when a patient support system such as those described herein is used with, for example, an electric stimulator system or with any other suitable electric and/or electronic data collection system, the patient support system can be configured to receive signals from and/or send signals to such electric or electronic systems associated with, for example, heel on or off events and/or other gait phases. Thus, in some instances, the patient support systems described herein can calculate and/or determine a step duration, a step length, a walking speed, a symmetry level of gait patterns (left/right), and/or any other suitable gait characteristic. Moreover, the patient support systems described herein can send one or more signals (e.g., via a wired or wireless connection) to, for example, the electronic device to cause a graphical representation, a numeric representation, and/or an alpha-numeric representation of the calculated

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and/or determined gait characteristics to be presented on a display. In other instances, the patient support system can send data associated with one or more operating conditions of the patient support system to the electronic device. In such instances, the electronic device can calculate and/or define the gait characteristics, based at least in part on the data received from the patient support system. In addition, the electric stimulator can send data associated with the patient's gait, substantially concurrently with the patient support system, to the electric device. In other instances, the electric stimulator can send data associated with the patient's gait to the patient support system and the patient support system (e.g., a processor, module, or compute device included therein) can aggregate the data associated with the patient support system and the data associated with the electric stimulator and, in turn, can send an aggregated data set to the electronic device.

In some embodiments, the patient support system and/or an electronic device in communication therewith can include memory and/or at least one module that stores data associated with one or more predetermined exercises, routines, tests, and/or the like. For example, the memory and/or module can include data associated with a set of exercises to analyze the patient's current and/or previous gait tests or analysis to track and help improve the patient's ability to walk. In some instances, the patient support system and/or the electronic device in communication therewith can graphically represent data associated with the exercises, routines, tests, and/or the like.

For example, FIG. 56 is a screenshot 901 illustrating a graphical representation of data associated with an asymmetry exercise. The screenshot 901 of the asymmetry exercise visually shows a patient's vertical asymmetry (leaning more on one side than on the other side) and his or her horizontal asymmetry (difference between step durations). As shown, the symmetry can be displayed in position symmetry bar graphs as well as radio dials, which can be complemented by real time graphs showing a history of, for example, changing tether positions and walking speeds. During and after the asymmetry test, the patient support system and/or the electronic device can cause data associated with an average, minimum, and/or maximum walking speed, a vertical and/or horizontal symmetry, and/or the like to be graphically represented on the display.

By way of another example, FIG. 57 is a screenshot 902 illustrating a graphical representation of data associated with a timed-up-and-go (TUG) exercise. The screenshot 902 of the TUG exercise can graphically represent data defined by the patient support system and/or the electronic device associated with the time it takes a patient to stand up from a seated position, walk a predetermined distance, and then sit down. During and after the TUG exercise, the patient support system and/or the electronic device can cause data associated with an average, minimum, and/or maximum speed during the TUG training exercises. The patient support system and/or the electronic device can cause data to be graphically represented on the display such as real time graphs showing the history of the stand-up, walking, and sit down process, tether positions (included in a patient support mechanism of the patient support system, as described in detail above), and/or time durations as well as the walking speeds during the exercise. Based at least in part on the time duration results, a fall risk (e.g., high or low) can be determined for the patient. Moreover, the data associated with the TUG exercise can be compared to historical data (e.g., stored in memory) from that patient's previous TUG

exercises, thereby allowing a clinician or therapist to keep track of improvements in patient's gait.

As another example, FIG. 58 is a screenshot 903 illustrating a graphical representation of data associated with a timed-distance exercise. For example, a user (e.g., clinician and/or patient) can select either a fixed distance (e.g., 10 meters) or a fixed time (e.g., 2 minutes). The patient then walks for that distance or that time the patient support system and/or the electronic device can determine and/or define the patient's performance. For a fixed distance, the timed-distance exercise can determine a gait speed and duration. For a fixed time, the timed-distance exercise can determine a total travelled distance and/or a gait speed. The patient support system and/or the electronic device can cause data to be graphically represented on the display such as real time graphs showing the distance travelled and the walking speed, an average, minimum, and/or maximum walking speed, and/or the like.

As described above, any data associated with the exercises, routines, tests, etc. can be saved, for example, in memory, to replay it back for post exercise analysis. In addition, data associated with any given exercise can be saved as a baseline so it can be used to compare against future exercises to show the improvements in patient's gait. Moreover, in some instances, a report can be defined (e.g., by the patient support system and/or the electronic device) and graphically represented on the display to provide details of a given exercise, including the gait speed, distance, time, time to stand, time to sit, cadence, symmetry indexes, or the like, as well as a Perry Ambulatory Category, a Functional Ambulation Category, and/or fall risk.

The patient support mechanism and/or the electronic device (or a processor, module, compute device, etc. included therein) can be configured to perform the exercises, routines, test, or the like, based on data associated with, for example, a tether position, a cam angle, a walking speed, a motor speed, a heel on or off event (and/or other gait phases), and/or the like. In some instances, the patient support mechanism and/or the electronic device can determine, for example, a change in the position of the tether (i.e., included in a patient support mechanism, as described in detail above) between two heel events to determine a vertical symmetry of the patient's gait. In some instances, the data can be based on both linear tether positions and/or cam angles (e.g., a linear graph) and a derivative thereof (e.g., slope or rate of change) of the tether position and/or cam angles (converted to linear length) to determine a gait pattern and/or characteristic.

Based on a determined gait pattern, the patient support mechanism and/or the electronic device can determine peaks and/or valleys associated with the gait events, which can be graphically represented as a linear graph or a derivative graph. In some instances, the patient support mechanism and/or the electronic device can use, for example, a midpoint logic to normalize the linear graph and/or derivative graph (e.g., remove a graph offset, or the like). In some instances, the peaks and valleys of the graphs (e.g., local minima and/or local maxima of the data) can be used determine the heel on or off events. Based on different predetermined gait patterns (e.g., a first category for normal walkers and a second category for pathological walkers) the peaks and valleys can be defined and/or determined differently. For example, for a normal walker, a valley (e.g., locally the shortest tether position) can be about mid stance (double support) of the gait. Conversely, for a pathological walker, a valley can be during a step.

Once the peaks and valleys are associated with the respective heel on or off events, the difference between the previous and current step tether positions can be determined to define the changes in the tether positions (e.g., determine vertical symmetry difference between the right and the left steps or the difference between the two subsequent steps). The previous and current step elapsed times can also be determined to define changes in the step duration (e.g., determine horizontal symmetry).

Although not shown herein, in some embodiments, the patient support systems and/or the body weight support systems can be used while a patient walks, for example, on a treadmill. As such, a patient support system can receive data associated with one or more operating conditions of the treadmill. In turn, the patient support system can use the data associated with the treadmill and data associated with the operating conditions of the patient support system to define one or more gait characteristics of the patient.

Any of the patient support systems and/or body weight support systems can be used in conjunction with any other suitable device configured to be used during a patient's gait. For example, a patient support system can include camera, infrared emitter and receiver, a visual light source and sensor, magnetic sensor, a force and/or pressure plate and sensor, and/or the like. In some embodiments, a patient support system can include, for example, a projector configured to project a graphical representation of data associated with a predetermined track or path along which the patient is to walk. In some instances, such a projector can project images such as stop signs, turn signs, obstacles to walk around, etc.). Moreover, in some instances, a patient reaching a target location projected onto a surface by the projector can be associated with a value or the like (e.g., a relatively high value) used to determine a patient performance score. Similarly, failing to avoid an obstacle projected onto a surface by the projector can be associated with a value or the like (e.g., a relatively low value). In some instances, such a projector can project a hologram of the patient walking so that they may see themselves walking either from the front or behind.

Any of the patient support systems and/or body weight support systems can be used with any suitable track and/or power rail such as those described herein. In some embodiments, a patient support system can include a track and/or power rail configured to allow for switching, diverting, and/or redirecting of a trolley movably coupled thereto. For example, FIG. 59 illustrates a first track portion 9620A and a second track portion 9620B, and a first power rail portion 9050A and a second power rail portion 9050B. In this embodiment, the first track portion 9620A and the second track portion 9620B are disposed perpendicular to each other. Similarly, the first power rail portion 9050A and the second power rail portion 9050B are disposed perpendicular to each other.

As shown in FIG. 59, a turntable 9625 includes a third track portion 9620C and a third power rail portion 9050C. The turntable 9625 is configured to be rotated relative to the track portions 9620A and 9620B and the power rails 9050A and 9050B, as indicated by the arrow AA. For example, in some embodiments, the turntable 9625 can be manually turned (e.g., a user exerts a force on a portion of the turntable 9625 such as a handle or the like (not shown in FIG. 59)). In other embodiments, the turntable 9625 can include a motor or the like (not shown in FIG. 59) that can receive a signal from a controller or the like and based on that signal, can rotate the turntable 9625. Therefore, in use, the turntable 9625 can rotate to a position relative to the track portions

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9620A and 9620B and the power rails 9050A and 9050B to place the third track portion 9620C in line with the first track portion 9620A, and to place the third power rail portion 9050C in line with the first power rail portion 9050A, as shown in FIG. 59. More particularly, when the third track portion 9620C is placed in line with the first track portion 9620A, the first track portion 9620A and the third track portion 9620C collectively form a substantially continuous track along which a trolley can move.

Similarly, the first power rail portion 9050A and the third power rail portion 9050B can collectively form a substantially continuous power rail configured to power the trolley suspended from the track, collectively formed by the first track portion 9620A and the third track portion 9620C. Specifically, in this embodiment, the turntable 9625 can be disposed in a position such that the first power rail portion 9050A and the third power rail 9050C are in electric communication. Thus, an electric current can flow from a power source (not shown), along a first length of the first power rail portion 9050A, along the third power rail portion 9050C, and along a second length of the first power rail portion 9050A. Moreover, in some embodiments, the ends of the power rail portions 9050A, 9050B, and 9050C can include a transfer section or the like (e.g., a flared or flanged end) that can allow for a given amount of misalignment between the first power rail portion 9050A or the second power rail portion 9050B and the third power rail portion 9050C.

In use, a user (e.g., a patient, a therapist, a technician, a doctor, etc.) may want to redirect a trolley disposed along, for example, a length of the first track portion 9620A. As such, the user can cause the trolley to move from a position along the first track portion 9620A to a position along the third track portion 9620C. With the trolley suspended from the third track portion 9620C and with the trolley in electrical communication with the third power rail 9050C, the user can rotate (e.g., either manually or electrically) the turntable 9625 to a position in which the third track portion 9620C is substantially in line with the second track portion 9620B and in which the third power rail portion 9050C is in line with the second power rail portion 9050B. When the third track portion 9620C is substantially aligned with the second track portion 9620B and the third power rail portion 9050C is substantially aligned with the second power rail portion 9050B, the user can cause the trolley to move from the position along the third track portion 9620C to a position along the second track portion 9620B. In this manner, the trolley can be turned, switched, rotated, and/or otherwise redirected. Similarly stated, the turntable can be rotated from a first position to a second position to rotate, switch, turn, and/or otherwise redirect the trolley.

Some embodiments described herein relate to a computer storage product with a non-transitory computer-readable medium (also can be referred to as a non-transitory processor-readable medium) having instructions or computer code thereon for performing various computer-implemented operations. The computer-readable medium (or processor-readable medium) is non-transitory in the sense that it does not include transitory propagating signals (e.g., propagating electromagnetic wave carrying information on a transmission medium such as space or a cable). The media and computer code (also referred to herein as code) may be those designed and constructed for the specific purpose or purposes. Examples of non-transitory computer-readable media include, but are not limited to: magnetic storage media such as hard disks, optical storage media such as Compact Disc/Digital Video Discs (CD/DVDs), Compact Disc-Read

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Only Memories (CD-ROMs), magneto-optical storage media such as optical disks, carrier wave signal processing modules, and hardware devices that are specially configured to store and execute program code, such as Application-Specific Integrated Circuits (ASICs), Programmable Logic Devices (PLDs), Read-Only Memory (ROM) and Random-Access Memory (RAM) devices. Other embodiments described herein relate to a computer program product, which can include, for example, the instructions and/or computer code discussed herein.

Examples of computer code include, but are not limited to, micro-code or micro-instructions, machine instructions, such as produced by a compiler, code used to produce a web service, and files containing higher-level instructions that are executed by a computer using an interpreter. For example, embodiments may be implemented using imperative programming languages (e.g., C, FORTRAN, etc.), functional programming languages (Haskell, Erlang, etc.), logical programming languages (e.g., Prolog), object-oriented programming languages (e.g., Java, C++, etc.), or other programming languages and/or other development tools. Additional examples of computer code include, but are not limited to, control signals, encrypted code, and compressed code.

While various embodiments have been described above, it should be understood that they have been presented by way of example only, and not limitation, and as such, various changes in form and/or detail may be made. For example, while the attachment mechanism 2800 is described above with reference to FIG. 34 as including energy storage members 2850, in other embodiments, an attachment mechanism need not include an energy storage member. In such embodiments, the attachment mechanism can be coupled to, for example, the trolley 2100 and the further coupled to a harness or the like worn by a patient. In such embodiments, the trolley 2100 can function in a substantially similar manner as described above.

Although the trolley 2100 is described above with reference to FIGS. 2-33 as including a motorized drive system 2300 and an active support mechanism 2500, in other embodiments, a trolley can include either a motorized drive system or an active support mechanism. Similarly stated, the drive system 2300 and the support mechanism 2500 can be mutually exclusive and can independently function in a similar manner to those described above.

Any portion of the apparatus and/or methods described herein may be combined in any suitable combination, unless explicitly expressed otherwise. For example, in some embodiments, the patient support mechanism 2500 of the trolley 2100 included in the support system 2000 can be replaced with a system similar to the support system 3900. In such embodiments, a cylinder, a piston, and an energy storage member can extend, for example, from the base 2210 of the housing 2200 of the trolley 2100. Expanding further, the kinetic and potential energy of the energy storage member (e.g., storage member 3960) could be actively controlled via a feedback system similar to the system described above with reference to the trolley 2100. For example, the energy storage member 3960 could be compressed air, the pressure of which could be controlled in response to a force exerted on the piston.

Where methods and/or schematics described above indicate certain events and/or flow patterns occurring in certain order, the ordering of certain events and/or flow patterns may be modified. Additionally certain events may be performed concurrently in parallel processes when possible, as well as performed sequentially.

What is claimed is:

1. A method, comprising:

receiving, at an active trolley, electrical current from a rigid power conductor, the active trolley including (1) a drive mechanism having a motor and a set of wheels configured to movably suspend the active trolley from a support track and (2) a patient support mechanism having a motor and a tether configured to be coupled to a patient harness such that the patient support mechanism supports a patient, the rigid power conductor being fixedly coupled adjacent to and offset from the support track;

receiving a signal associated with a first operating condition of at least one of the drive mechanism or the patient support mechanism;

providing a portion of the electrical current to at least one of the motor of the drive mechanism or the motor of the patient support mechanism operable to transition at least one of the drive mechanism or the patient support mechanism, respectively, from the first operating condition to a second operating condition in response to movement of the patient such that (1) the motor of the drive mechanism rotates the set of wheels to move the active trolley along the support track or (2) the motor of the patient support mechanism moves the tether relative to the active trolley, respectively;

receiving a signal associated with the second operating condition of at least one of the drive mechanism or the patient support mechanism;

determining a difference between the first operating condition and the second operating condition;

determining, based at least in part on the difference between the first operating condition and the second operating condition, a change in a position associated with the patient harness; and

defining, based at least in part on the change in the position associated with the patient harness, a gait characteristic of the patient supported by the patient support mechanism.

2. The method of claim 1, wherein the first operating condition is a first operating condition of the patient support mechanism and the second operating condition is a second operating condition of the patient support mechanism, the method further comprising:

receiving a first operating condition associated with the drive mechanism;

receiving a second operating condition associated with the drive mechanism; and

determining a difference between the first operating condition of the drive mechanism and the second operating condition of the drive mechanism, the determining of the change in the position associated with the patient harness includes determining the change in the position associated with the patient harness based at least in part on the difference between the first operating condition of the patient support mechanism and the second operating condition of the patient support mechanism and the difference between the first operating condition of the drive mechanism and the second operating condition of the drive mechanism.

3. The method of claim 1, wherein the at least one of the drive mechanism or the patient support mechanism is in the first operating condition when the patient is in a first position relative to the support track, the at least one of the drive mechanism or the patient support mechanism is in the second operating condition when the patient moves to a

second position relative to the support track, the second position being different from the first position.

4. The method of claim 1, the first operating condition is a first operating condition of the patient support mechanism and the second operating condition is a second operating condition of the patient support mechanism, the receiving of the signal associated with the first operating condition includes receiving the signal associated with the first operating condition from a sensor included in the patient support mechanism, the receiving of the signal associated with the second operating condition includes receiving the signal associated with the second operating condition from the sensor included in the patient support mechanism.

5. The method of claim 1, wherein the first operating condition is a first operating condition of the drive mechanism and the second operating condition is a second operating condition of the drive mechanism, the receiving of the signal associated with the first operating condition includes receiving the signal associated with the first operating condition from a sensor included in the drive mechanism, the receiving of the signal associated with the second operating condition includes receiving the signal associated with the second operating condition from the sensor included in the drive mechanism.

6. The method of claim 1, further comprising:

sending a signal to an electronic device having a display, the signal indicative of an instruction to output data associated with the gait characteristic via the display.

7. A method, comprising:

receiving, at an active trolley, electrical current from a rigid power conductor, the active trolley including (1) a drive mechanism having a motor and a set of wheels configured to movably suspend the active trolley from a support track and (2) a patient support mechanism having a motor and a tether configured to tether a patient to the patient support mechanism to support at least a portion of a weight of the patient, the rigid power conductor being fixedly coupled adjacent to and offset from the support track;

providing a first flow of the electrical current to the motor of the patient support mechanism in response to movement of the patient such that the motor of the patient support mechanism moves a portion of the tether relative to the patient;

providing a second flow of the electrical current to the motor of the drive mechanism in response to the movement of the patient such that the motor of the drive mechanism rotates the set of wheels to move the active trolley along the support track;

receiving a first signal from a first sensor, the first signal being associated with an operating condition of the patient support mechanism after being sent the first flow of the electrical current;

receiving a second signal from a second sensor, the second signal being associated with an operating condition of the drive mechanism after being sent the second flow of the electrical current;

defining at least one gait characteristic associated with the movement of the patient based at least in part on the operating condition of the patient support mechanism and the operating condition of the drive mechanism; and

sending, to an electronic device having a display, a third signal, the third signal indicative of an instruction to output data associated with the at least one gait characteristic via the display.

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8. The method of claim 7, wherein the operating condition of the drive mechanism is associated with a rotational velocity or a rotational acceleration of the set of wheels,

the receiving of the second signal from the second sensor includes receiving data associated with at least one of the rotational velocity of the set of wheels or the acceleration of the set of wheels.

9. The method of claim 7, wherein the operating condition of the patient support mechanism is associated with at least one of a length of a portion of the tether, an angle of the portion of the tether relative to the support track, a tension within a portion of the tether, or a feed rate of the tether.

10. The method of claim 7, wherein the movement of the patient is associated with the patient walking, the motor of the drive mechanism configured to rotate the set of wheels to move the active trolley along the support track in response to the patient walking.

11. The method of claim 7, wherein the determining of the at least one gait characteristic associated with the patient includes determining at least one of a step duration, a swing to stance duration, a swing to stance ratio, a cadence, a stride length of height, a range of motion in an anterior and posterior direction, a range of motion in a lateral direction, and ratio between the range of motion in the anterior and posterior direction and the range of motion in the lateral direction.

12. The method of claim 7, wherein the sending of the third signal includes sending the third signal to cause at least one of a graphical representation, a numeric representation, or an alpha-numeric representation of data associated with the gait characteristic to be presented on the display of the electronic device.

13. The method of claim 7, wherein the operating condition of the patient support mechanism is a first operating condition of the patient support mechanism, and the operating condition of the drive mechanism is a first operating condition of the drive mechanism, the method further comprising:

defining, based at least in part on the determining of the at least one gait characteristic, a second operating condition associated with the patient support mechanism and a second operating condition associated with the drive mechanism;

providing a third flow of the electrical current to the patient support mechanism, the third flow of the electrical current operable to move at least the portion of the tether relative to the patient to place the patient support mechanism in its second operating condition; and

providing a fourth flow of the electrical current to the drive mechanism, the fourth flow of the electrical current operable to rotate the set of wheels of the drive mechanism to place the drive mechanism in its second operating condition.

14. A method, comprising:

receiving, at an active trolley, electrical current from a rigid power conductor, the active trolley including (1) a drive mechanism having a motor and a set of wheels configured to movably suspend the active trolley from a support track and (2) a patient support mechanism having a motor and a tether configured to tether a patient to the patient support mechanism to support at least a portion of a weight of the patient, the rigid power conductor being fixedly coupled adjacent to and offset from the support track such that each of the support track and the drive mechanism are separated from the rigid power conductor;

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receiving, at a processor of the active trolley, a signal associated with a first operating condition of the active trolley;

providing a flow of electrical current to at least one of the drive mechanism or the patient support mechanism to transition the active trolley from the first operating condition to a second operating condition in response to a change in force exerted by the patient on the tether such that (1) the motor of the drive mechanism rotates the set of wheels to move the active trolley along the support track or (2) the motor of the patient support mechanism moves a portion of the tether relative to the patient, respectively;

defining, at the processor, at least one gait characteristic of the patient based at least in part on a difference between the first operating condition and the second operating condition of the active trolley; and

displaying data associated with the at least one gait characteristic of the patient on a display of an electronic device in communication with the processor.

15. The method of claim 14, wherein the first operating condition of the active trolley corresponds to a first operating condition of the patient support mechanism and the second operating condition of the active trolley corresponds to a second operating condition of the patient support mechanism,

the difference between the first operating condition of the patient support mechanism and the second operating condition of the patient support mechanism is associated with a difference between at least one of a length of a portion of the tether, an angle of a guide member included in the patient support mechanism and engaged with the tether, a tension within a portion of the tether, or a feed rate of the tether.

16. The method of claim 15, wherein the patient support mechanism includes a cam configured to move in response to movement of the portion of the tether, the difference between the first operating condition of the patient support mechanism and the second operating condition of the patient support mechanism is associated with (1) the difference between at least one of the length of the portion of the tether, the angle of the guide member, the tension within the portion of the tether, or the feed rate of the tether, and (2) a difference between at least one of a cam position, a cam angle, a cam velocity, or a cam acceleration.

17. The method of claim 14, wherein the active trolley includes an electronic system, the electronic system includes the processor and at least one sensor, the at least one sensor configured to send the signal to the processor.

18. The method of claim 14, wherein the change in force exerted by the patient on the tether is associated with a change in a portion of the weight of the patient supported by the patient support mechanism.

19. The method of claim 14, wherein the determining of the at least one gait characteristic associated with the patient includes determining at least one of a step duration, a swing to stance duration, a swing to stance ratio, a cadence, a stride length of height, a range of motion in an anterior and posterior direction, a range of motion in a lateral direction, and ratio between the range of motion in the anterior and posterior direction and the range of motion in the lateral direction.

20. The method of claim 14, wherein the first operating condition of the active trolley corresponds to a first operating condition of the drive mechanism and the second operating condition of the active trolley corresponds to a second operating condition of the drive mechanism,

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the difference between the first operating condition of the drive mechanism and the second operating condition of the drive mechanism is associated with a difference between at least one of a position of at least one wheel from the set of wheels relative to the support track, a 5 velocity of at least one wheel from the set of wheels, or an acceleration of at least one wheel from the set of wheels.

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